



VARSKIN 6

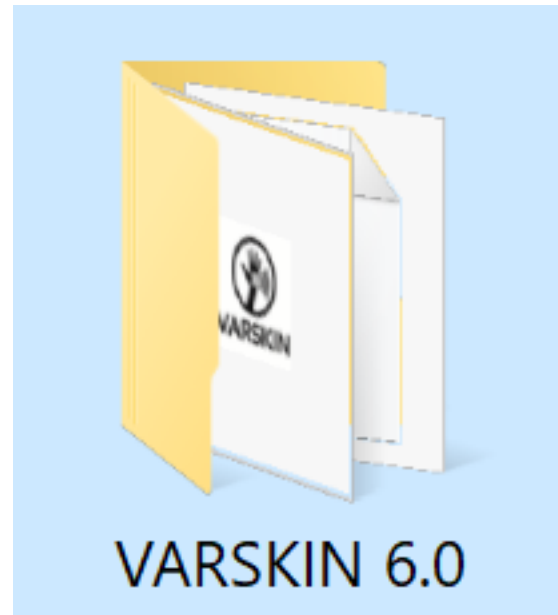


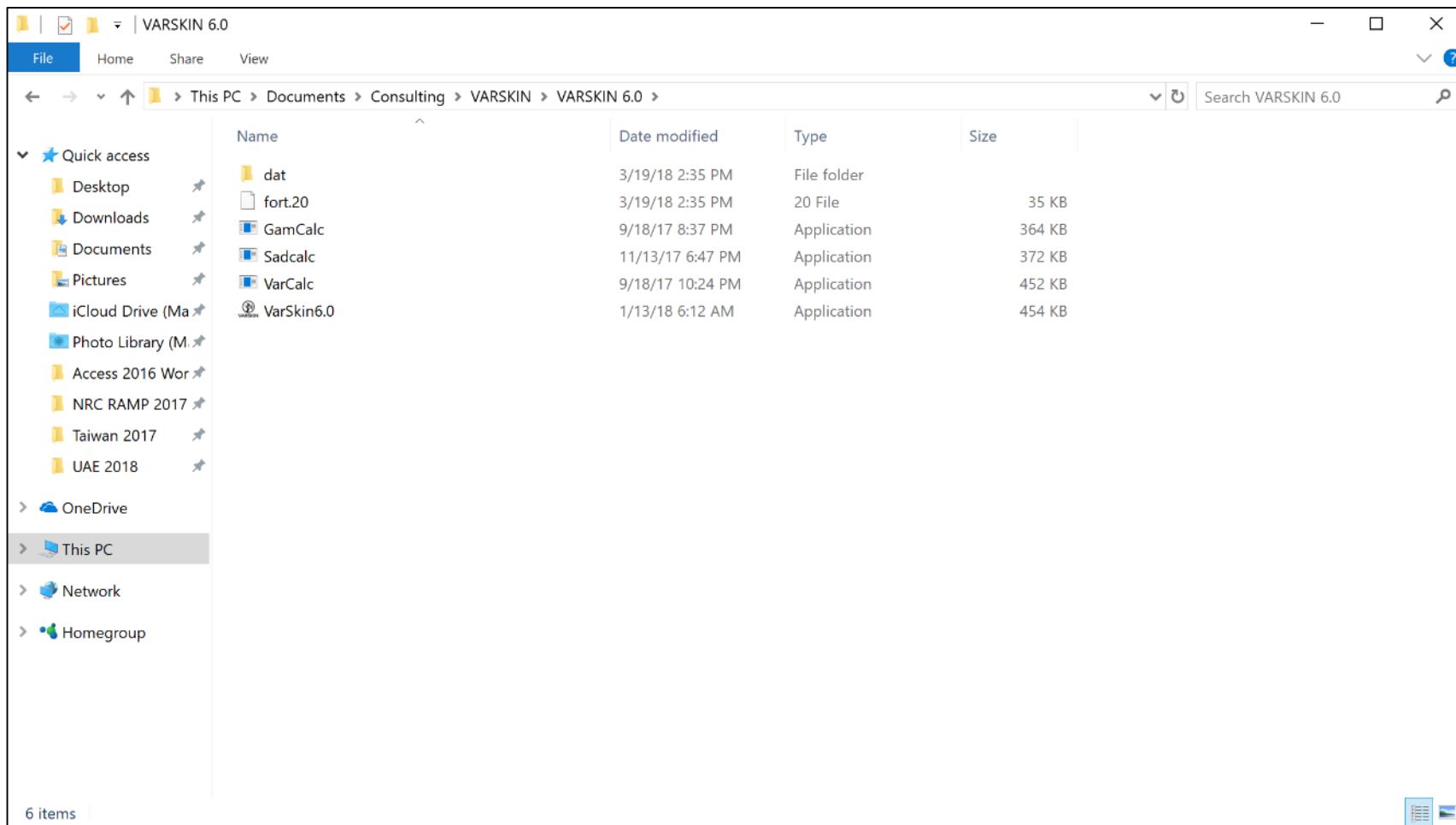
Intro to VARSKIN and Dose Calcs

USING VARSKIN

CODING structure

- GUI written in C#
 - controls I/O functions and executables
- Three modules written in FORTRAN
 - SadCalc.exe; VarCalc.exe; GamCalc.exe
- GamCalc.exe file written to execute photon dose model
- No need to “install” the code
 - simply double-click the VARSKIN 6 executable file





V6 Varskin 6.0

File Help

Source Geometry

- ☐ Point
- ☐ Disk
- ☐ Cylinder

Open
Save
Save AS
Reset
Save Default State
Load Default State
Exit

Special

- ☐ Exclude
- ☐ Exclude Electron Dose
- ☐ Perform Volume Averaging
- ☐ Offset Particle Model

Skin Averaging Area

10 cm²

Exposure Time

60 min

Radionuclide Library [Zeff]

[42] 38
[7.42] 107
[7.42] 107D
[7.42] 38
Ce-144 [7.42] 38D
Co-60 [25.5] 38
Pr-144 [7.42] 107
Pr-144 [7.42] 38
Pr-144m [7.42] 38
Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

Selected Radionuclides

Edit

Remove

Remove All

Point Source Irradiation Geometry

Skin Thickness or Skin Density Thickness: 7 mg/cm²

Air Gap Thickness 0 mm

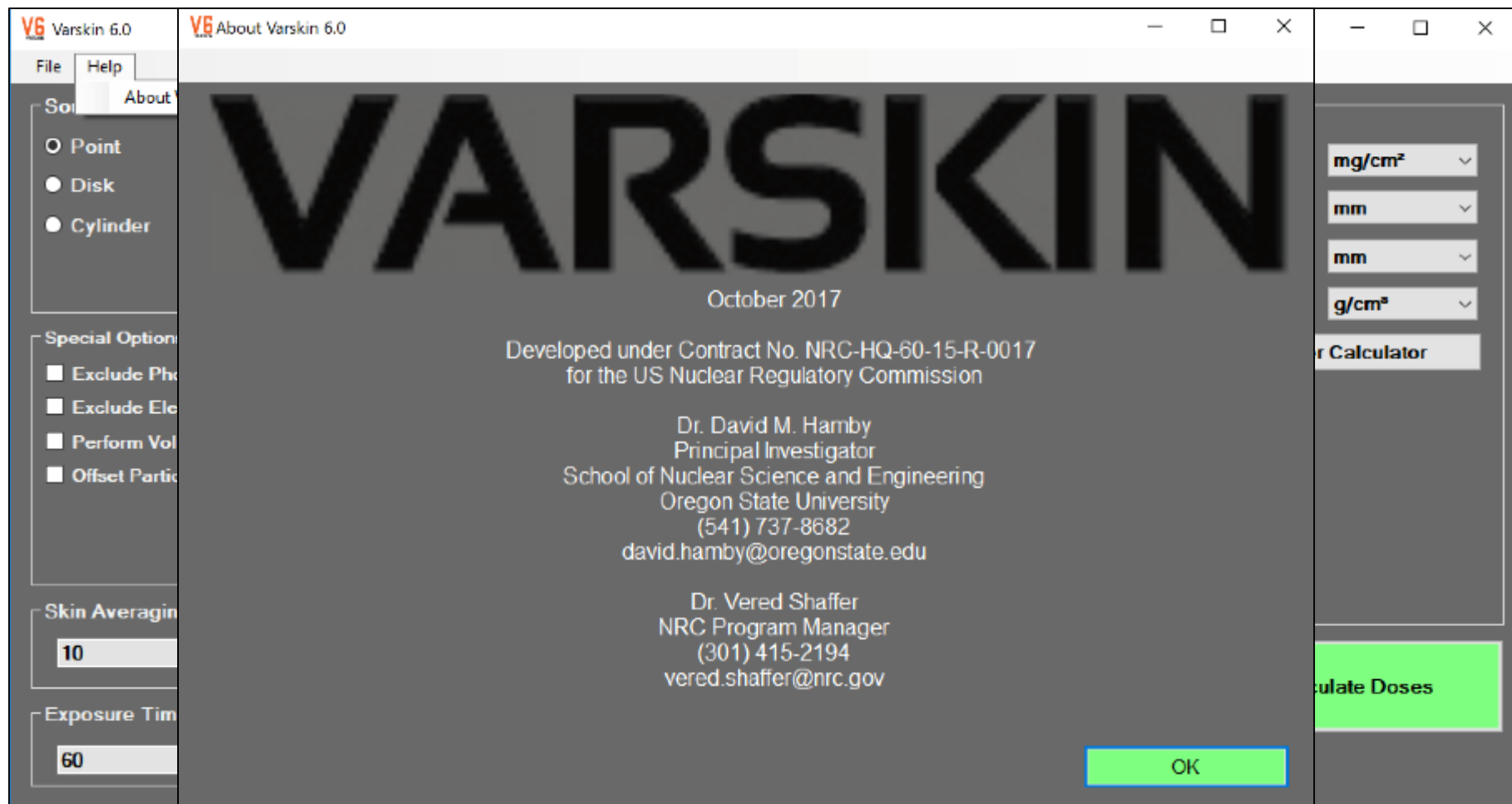
Cover Thickness 0 mm

Cover Density 0 g/cm³

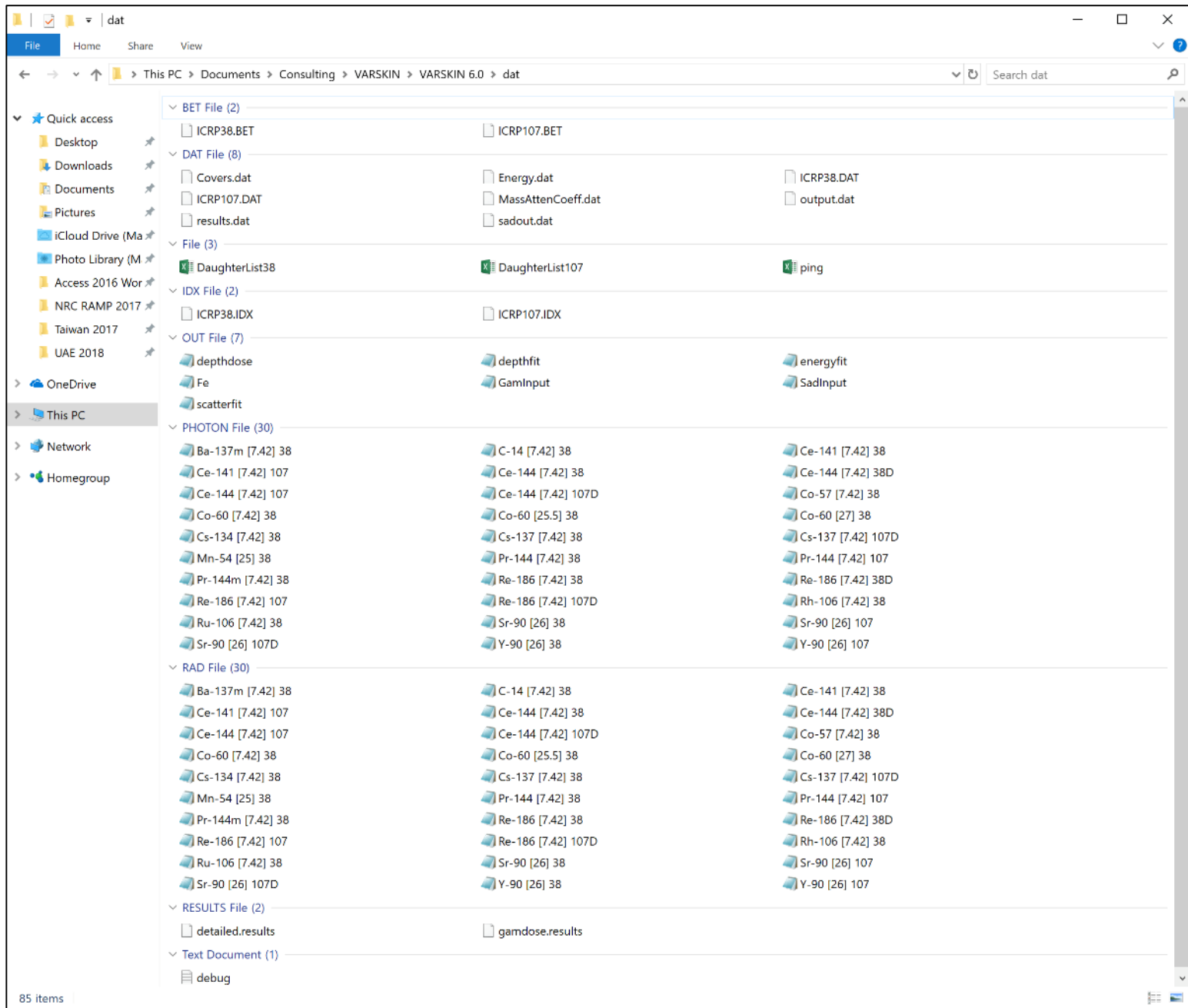
Multiple Cover Calculator

VARSKIN

Calculate Doses



Dat folder



.rad and .photon dat files

```
Co-60 [7.42] 38 - Notepad
File Edit Format View Help
7.42      $ sngZsrc
False     $ Include daughter products
False     $ Use ICRP107 instead of 38
0.09690186 $ sngEavg
0.03300993 $ sngX90
1.00245    $ sngYield
46205.6    $ sngHalfLife
2.69586    $ sngFit[0]
2.50338    $ sngFit[1]
2.3109     $ sngFit[2]
2.1198     $ sngFit[3]
2.02026    $ sngFit[4]
1.93571    $ sngFit[5]
1.66705    $ sngFit[6]
1.48796    $ sngFit[7]
1.34653    $ sngFit[8]
1.22533    $ sngFit[9]
1.11706    $ sngFit[10]
1.01971    $ sngFit[11]
0.931275   $ sngFit[12]
0.850585   $ sngFit[13]
0.77645    $ sngFit[14]
0.707951   $ sngFit[15]
0.644495   $ sngFit[16]
0.585654   $ sngFit[17]
0.531001   $ sngFit[18]
0.480307   $ sngFit[19]
0.433249   $ sngFit[20]
0.349151   $ sngFit[21]
0.277386   $ sngFit[22]
0.216911   $ sngFit[23]
0.166672   $ sngFit[24]
0.09268598 $ sngFit[25]
0.04692546 $ sngFit[26]
0.02115152 $ sngFit[27]
0.001329488 $ sngFit[28]
0.0008001831 $ sngFit[29]
2.38415    $ sngFit[30]
2.25939    $ sngFit[31]
2.13463    $ sngFit[32]
2.01047    $ sngFit[33]
1.92601    $ sngFit[34]
1.85219    $ sngFit[35]
```

```
Co-60 [7.42] 38 - Notepad
File Edit Format View Help
Co-60 [7.42] 38
1 99.9 1.17321
1 99.9824 1.33247
```


How is Beta Dose Determined?



VARSKIN 6



Electron Interactions

Electron Interactions

- As energetic electrons pass through material, they transfer energy
 - primarily via “soft collisions”, i.e., Coulombic interactions
 - or, “hard” collisions with orbital electrons
- Energy loss is a function of KE & charge density
- Energy loss can result in:
 - excitation – characteristic X-rays
 - ionization – scattered energetic electrons
 - Bremsstrahlung (>1 MeV electrons) – low-energy photons
- Scattered electrons may produce additional ion pairs
 - e.g., clusters, delta rays, further excitation/ionization

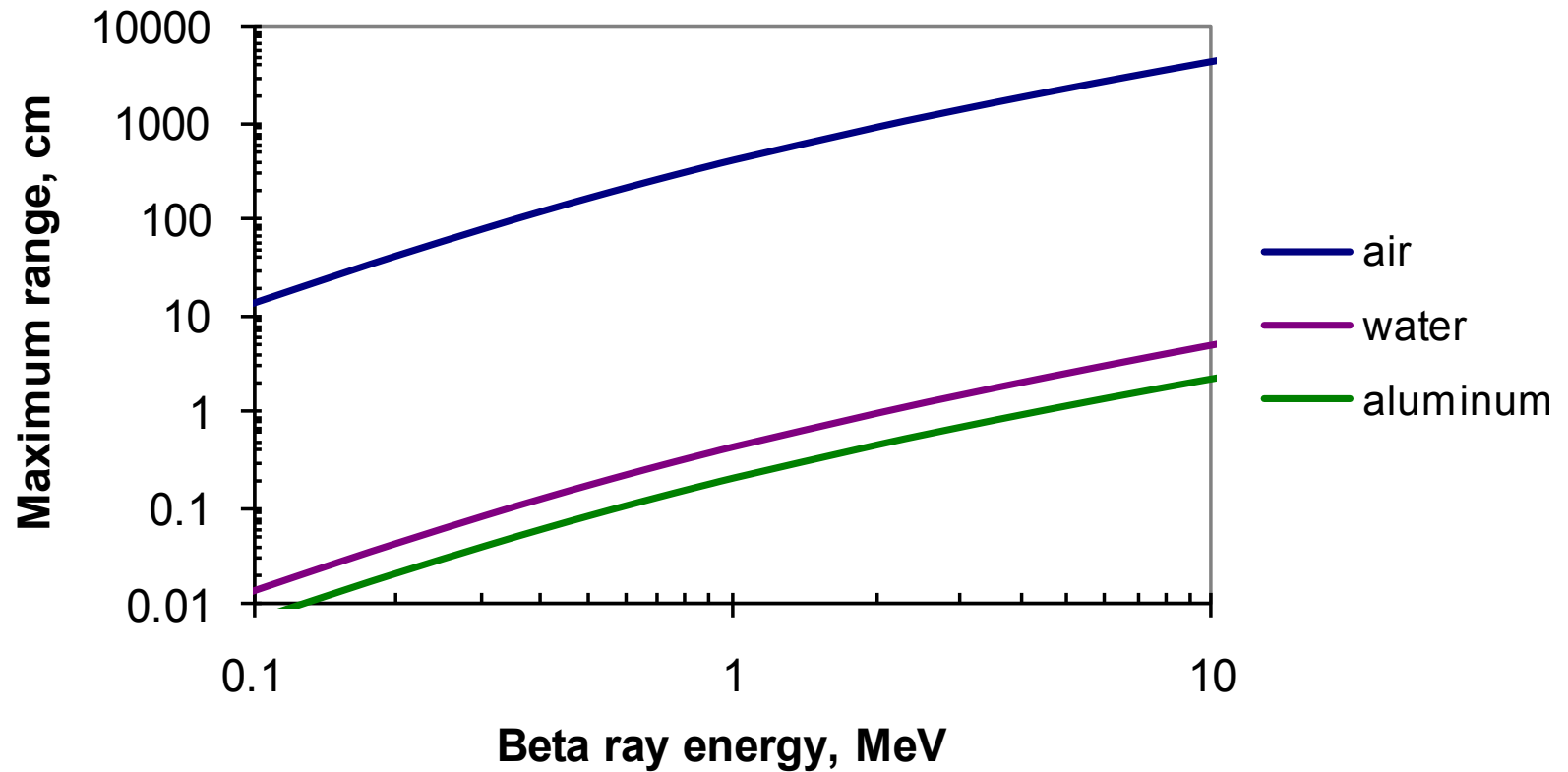
Characteristics Important for Dosimetry

- The depth at which electrons penetrate in tissue
 - Range and “Attenuation”
- The rate at which electron energy is lost
 - Stopping Power
- Relative to the primary electron location, the proximity to which energy is absorbed
 - Bremsstrahlung
- The fraction of electrons scattering without ever entering the dose material
 - Backscatter

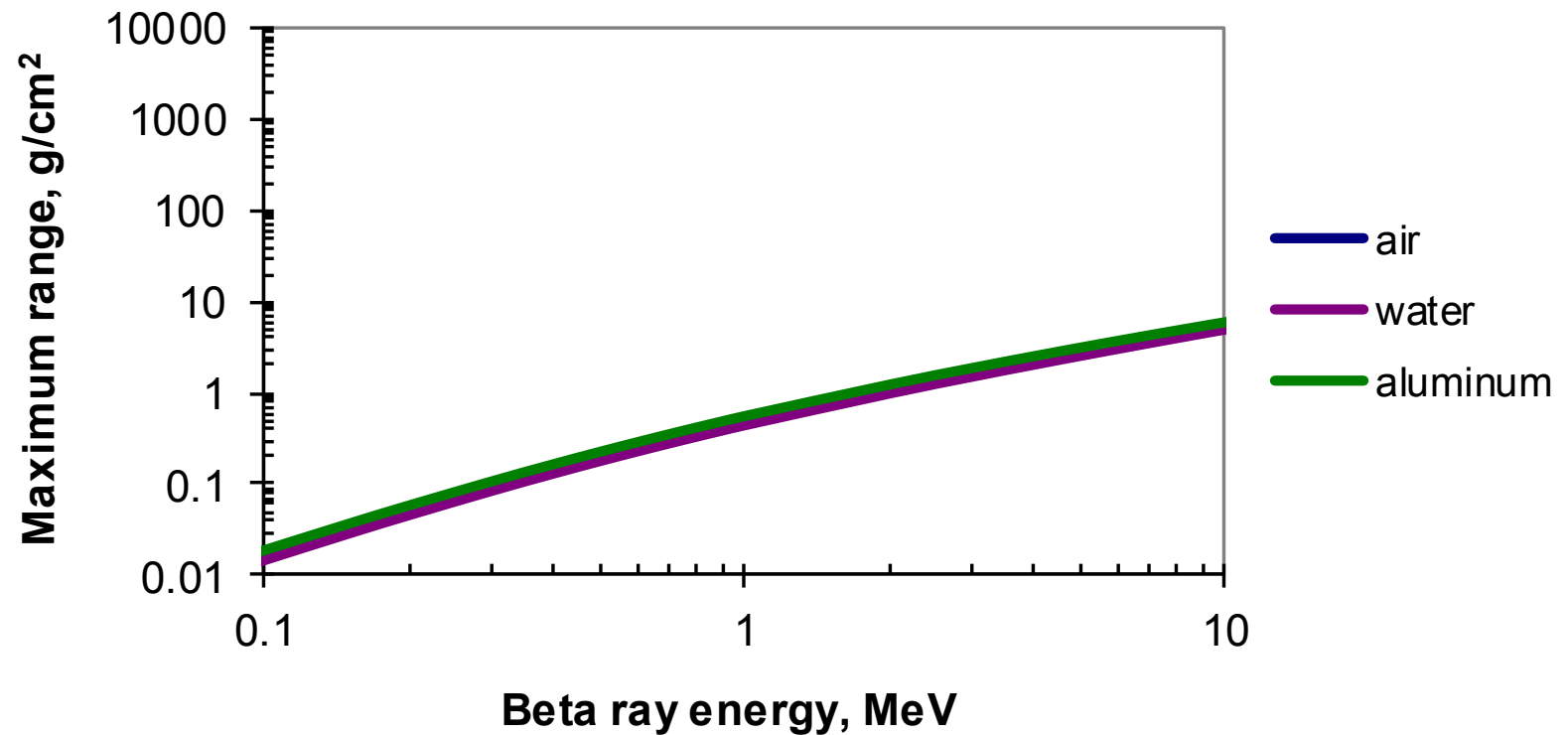
Range-Energy Observations

- Electrons lose energy via tortuous paths
- Electron range (penetration depth) increases with increasing energy
- Linear range is largely dependent on electron density of the absorber atoms
- And, to a lesser degree, range is a function of Z
 - result has practical implications for shielding
 - *density thickness* (mg/cm^2) is best indicator of electron range
 - important tissue depths \rightarrow 7, 100, 300, 1000 mg/cm^2

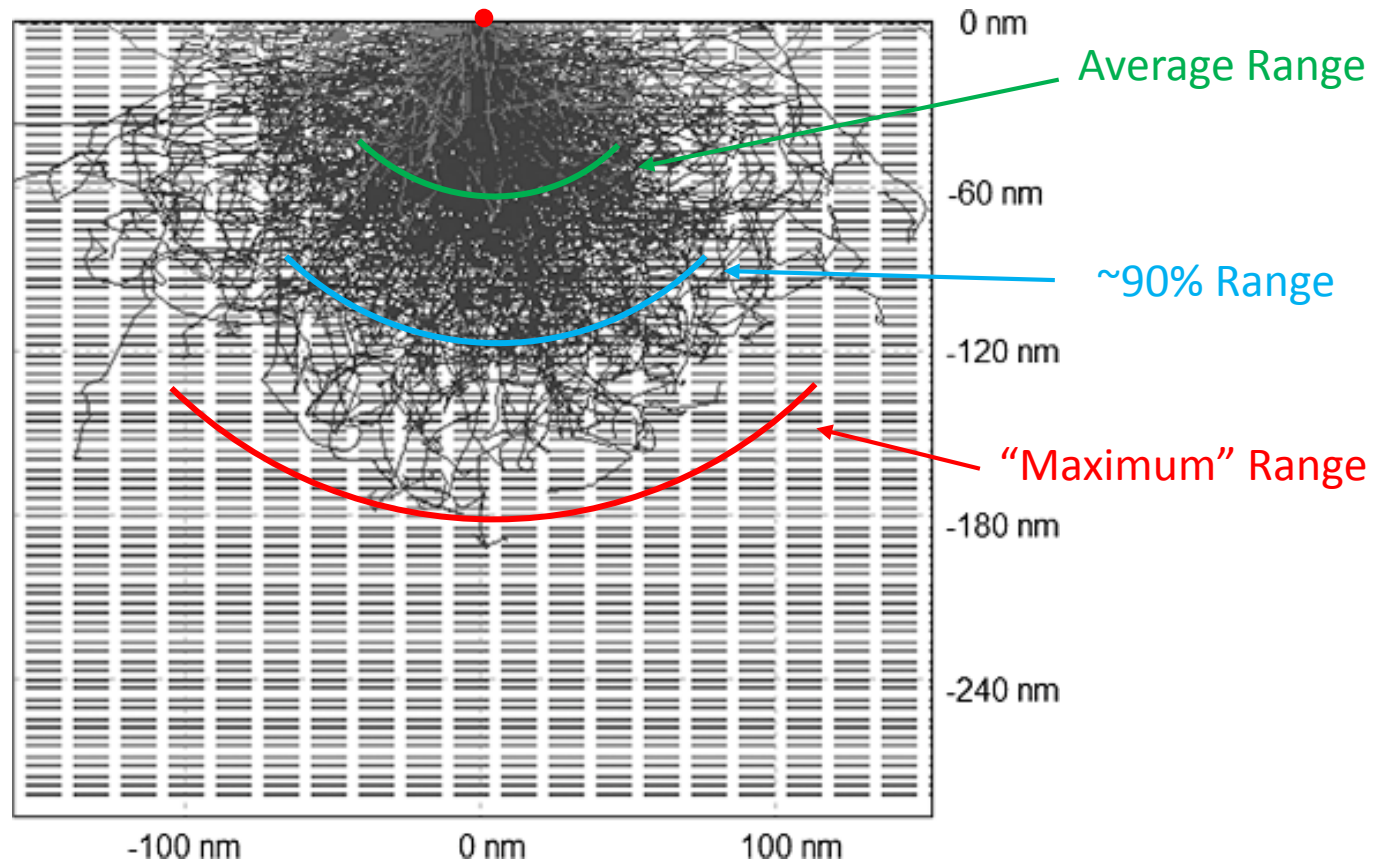
Range-Energy Relationship for Electrons



Advantage of Density Thickness



Electron Track Simulation



Electron “Attenuation”

Method assumes that electrons attenuate similar to photons:

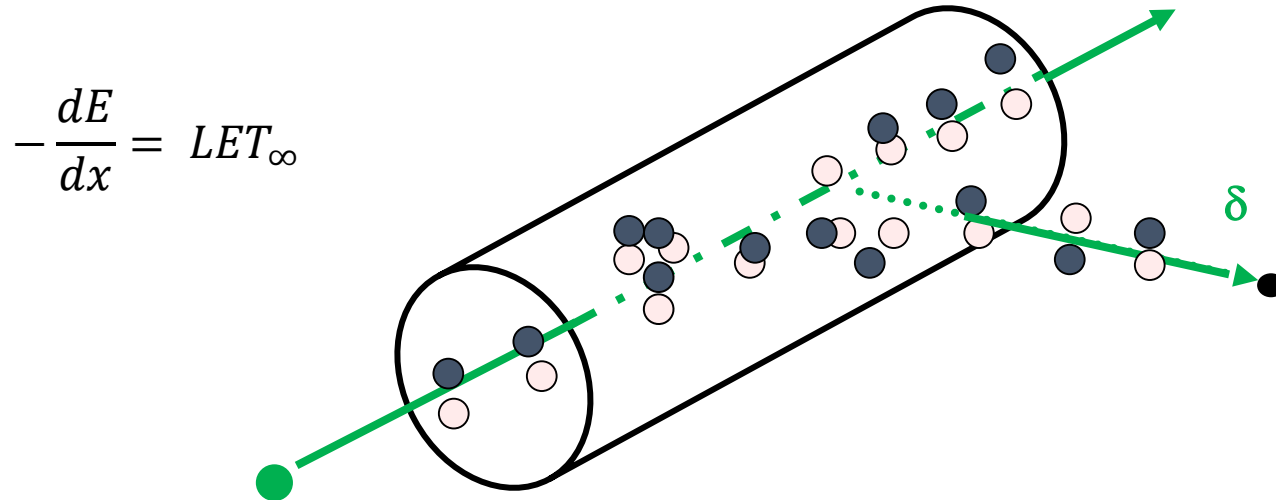
$$\phi_{\beta}(x) = \phi_{\beta,0}(x) \cdot e^{-\mu_{\beta}(\rho x)}$$

then,

$$D_{\beta} \left[\frac{\text{Gy}}{\text{sec}} \right] = \phi_{\beta} \left[\frac{\beta}{\text{sec} \cdot \text{cm}^2} \right] \cdot \bar{E}_{\beta} \left[\frac{\text{J}}{\beta} \right] \cdot \mu_{\beta} \left[\frac{\text{cm}^2}{\text{kg}} \right]$$

“Beta absorption coefficient”

Energy Transfer vs Absorption



$$-\frac{dE}{dx} = LET_{\infty}$$

- “Stopping Power” ($-dE/dx$) is a measure of energy loss
- “LET” is a measure of energy deposited locally
- Not all energy lost (transferred) is absorbed locally
 - due to delta rays or bremsstrahlung
 - “local” is defined by the radius of a cylinder within which energy is deposited, e.g., $LET_{0.1}$

Mass Stopping Power

- Stopping power is often expressed relative to the absorber density (i.e., “mass stopping power”)

$$\frac{S}{\rho} = \left(-\frac{dE}{dx} \right) / \rho$$

- With units of energy per density thickness, it is a very useful parameter in charged-particle dosimetry

$$\left[\frac{S}{\rho} \right] = \frac{\text{MeV} \cdot \text{cm}^2}{\text{g}}$$

Total Mass Stopping Power

$$\frac{S_{total}}{\rho} = \frac{1}{\rho} \left(\frac{-dE}{dx} \right)_c + \frac{1}{\rho} \left(\frac{-dE}{dx} \right)_r$$

- Total energy loss as the electron moves through a medium
- Considers both collisional and radiative energy losses
- Generally, for dosimetry we assume that transfer = absorption
 - i.e., energy loss (per unit density) is used to calculate dose
 - a 3 MeV electron in water loses only 1% of its energy via bremsstrahlung

Electron Backscatter

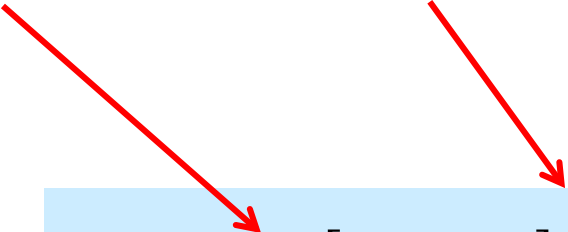
- ✗ Because electrons are interacting with other electrons, the phenomenon of “backscatter” is an important issue
- ✗ In thin foils, backscatter isn’t significant to dosimetry
- ✗ In thick materials, however, some portion of the electron energy flux is redirected in the reverse direction and the average absorbed dose throughout the material is less than expected
- ✗ Empirical relationships appear in many different forms for estimating the backscatter effect
- ✗ Backscatter for particles on skin introduces additional difficulties in electron skin dosimetry

Backscatter Considerations

- × Energy loss functions are often developed with the initial assumption that the absorbing medium is homogeneous (i.e., 4π water)
- × But, there are significant dose implications for scattered electrons when the medium is heterogeneous
 - × source in air, with a tissue interface
 - × volumetric high-Z source on skin
 - × either into, or out of, the dose receptor
- × Most significant for situations with:
 - × low-energy electrons
 - × thick, high-Z targets
- × If dose calculations are based on homogeneous emission/absorption, backscatter must be considered

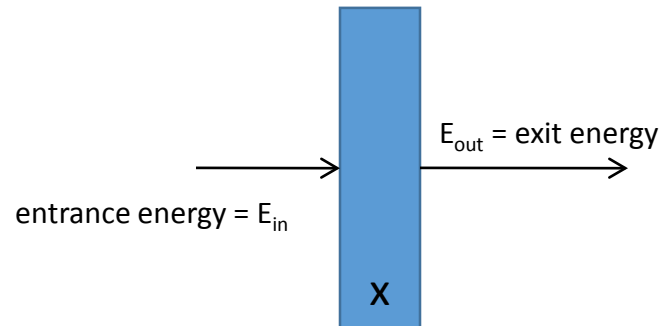
Simplified Electron Dosimetry

In thin slices that are uniformly exposed, the dose rate from charged particles can be expressed simply as the product of particle flux and mass stopping power:


$$\dot{D} \left[\frac{Gy}{sec} \right] = \phi \left[\frac{particles}{sec \cdot cm^2} \right] \cdot \frac{\frac{dE}{dx} \left[\frac{J}{cm} \right]}{\rho \left[\frac{kg}{cm^3} \right]}$$

Simplified Electron Dosimetry

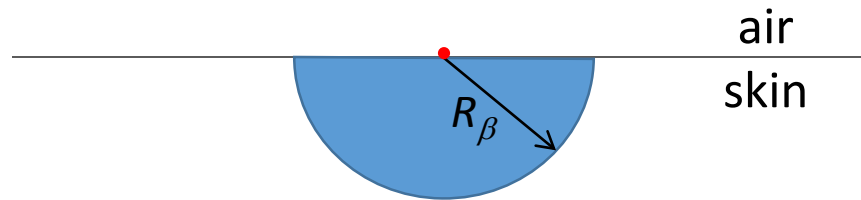
And, in thick materials (uniformly exposed), the average dose rate from charged particles can be determined from estimates of the particle range and related energy loss:



$$D \left[\frac{\text{Gy}}{\text{sec}} \right] = \frac{\phi \left[\frac{\text{particles}}{\text{sec} \cdot \text{cm}^2} \right] (E_{in} - E_{out}) [\text{J}]}{\rho \left[\frac{\text{kg}}{\text{cm}^3} \right] x [\text{cm}]}$$

Simple Hot-Particle Dosimetry

Given an isotropic source, and assuming that all energy is deposited within a hemisphere of skin that has a radius equal to the maximum range (or some percentage thereof):

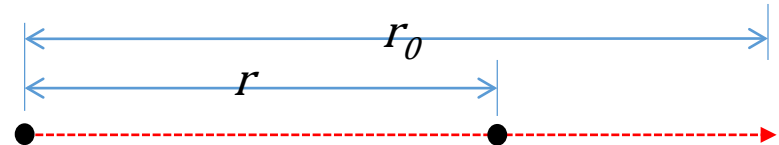


$$D_\beta \left[\frac{\text{Gy}}{\text{sec}} \right] = \frac{\frac{1}{2} \cdot A \left[\frac{\text{dis}}{\text{sec}} \right] \cdot Y \left[\frac{\beta}{\text{dis}} \right] \cdot \bar{E}_\beta \left[\frac{\text{J}}{\beta} \right]}{\frac{1}{2} \cdot \frac{4}{3} \pi \cdot R_\beta^3 \left[\text{cm}^3 \right] \cdot \rho \left[\frac{\text{kg}}{\text{cm}^3} \right]}$$

Electron Point-Kernel Dosimetry

As with photons, the point-kernel method can be used for mono-energetic electron dosimetry in which dose is integrated over all source and receptor points:

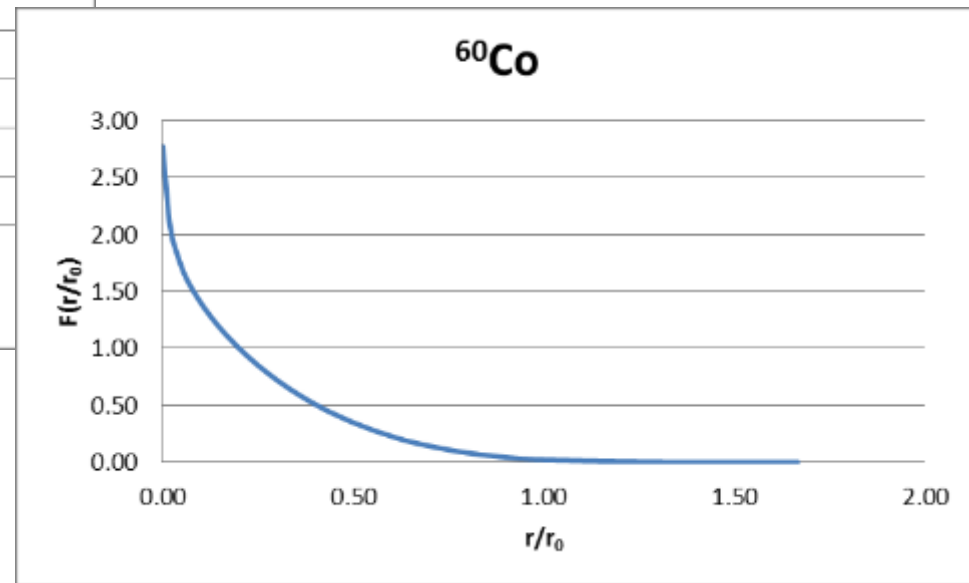
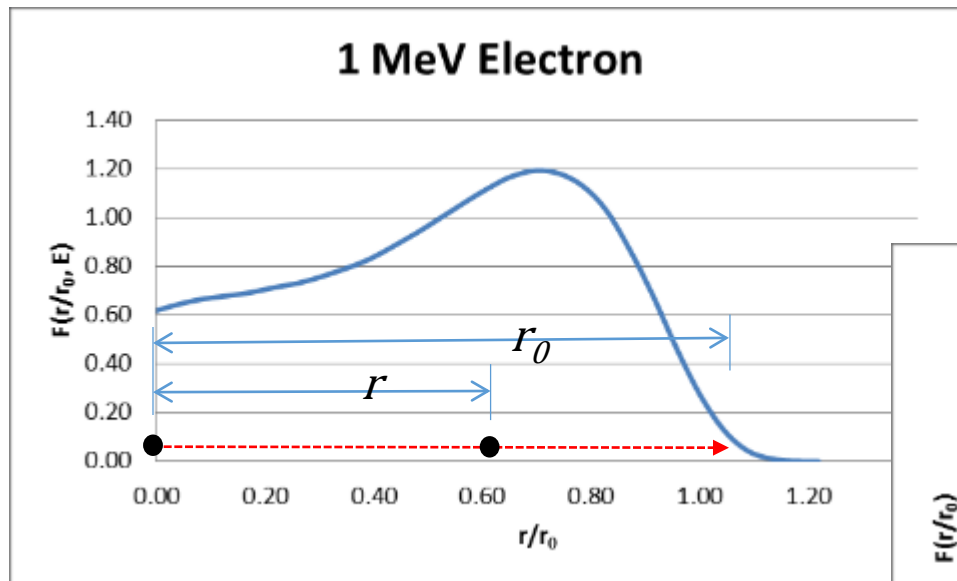
$$G(r, E) = \frac{E}{4\pi r^2 \rho r_0} F(r/r_0, E)$$



The function $F(r/r_0, E)$ is a “scaled absorbed dose distribution” (essentially a normalized Bragg curve) that is dependent on the electron initial energy and the fraction of *maximum* range (r/r_0) that the electron has achieved by the time it reaches the dose location.

Scaled Absorbed Dose Distributions

The factor $F(r/r_0, E)$ is shown for electrons of energy E , and for beta particles of distributed E , normalized over their *maximum* range, r_0





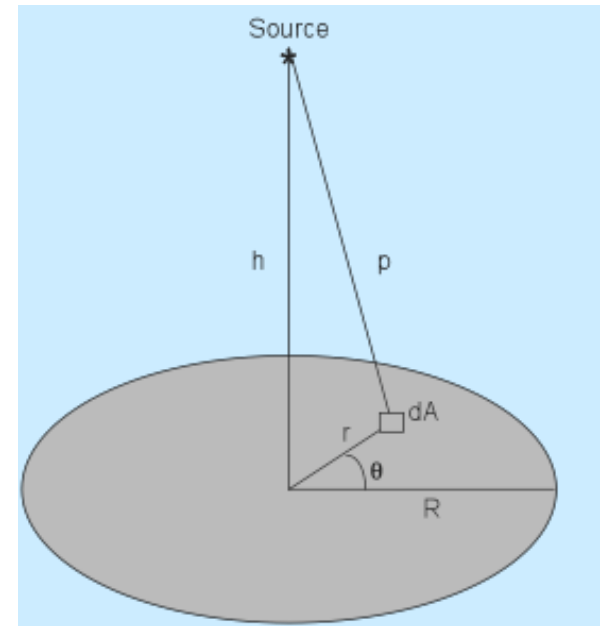
VARSKIN 6



A Brief Review of the Original VARSKIN Beta Dosimetry

Fundamentally ...

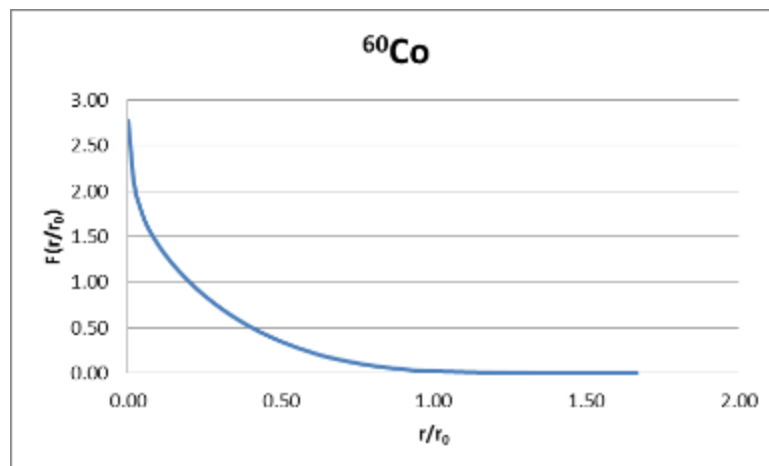
- Point-kernel method employed
- Source on skin surface
- Dose calculated to a given averaging area at the user-specified depth
- Energy absorption based on calculated stopping power at depth



Previous Beta Dosimetry Model

- Using Berger dose point-kernel, $B(r)$ (*MIRD Pamphlet No. 7, 1971*)
- Numerically integrated over source and dose volumes
- r_1 is a *modified* path length based on a density ratio
- r_0 represents the *maximum* path length, in Berger's case the X_{90}

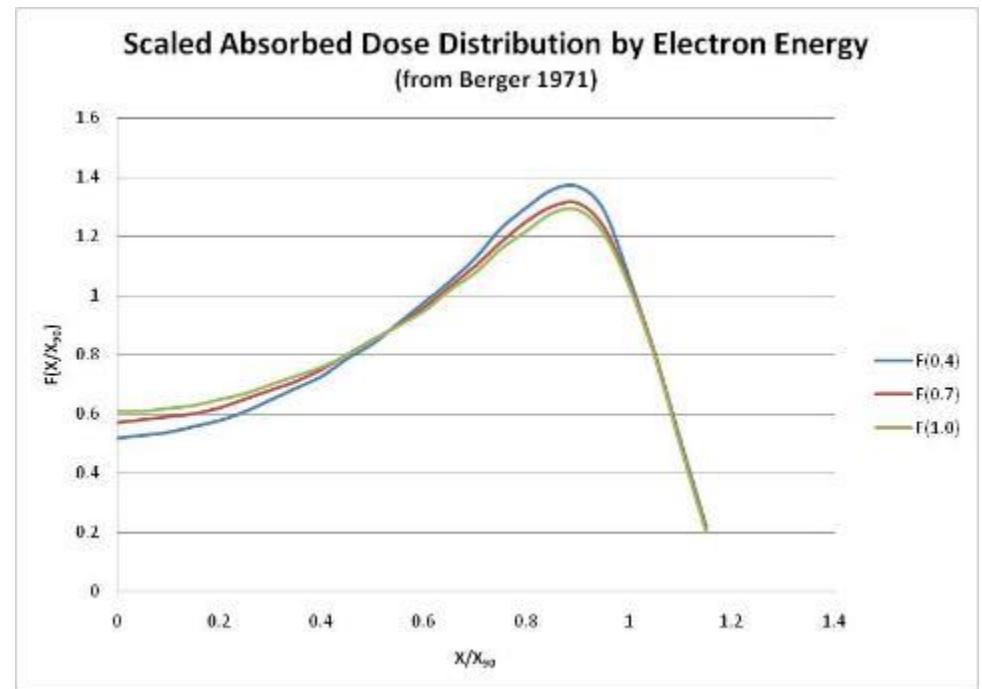
$$B(r) = \frac{kY\bar{E}F_{\beta}(r_1/r_0)}{\pi r^2 \rho r_0}$$



Scaled Absorbed Dose Distribution

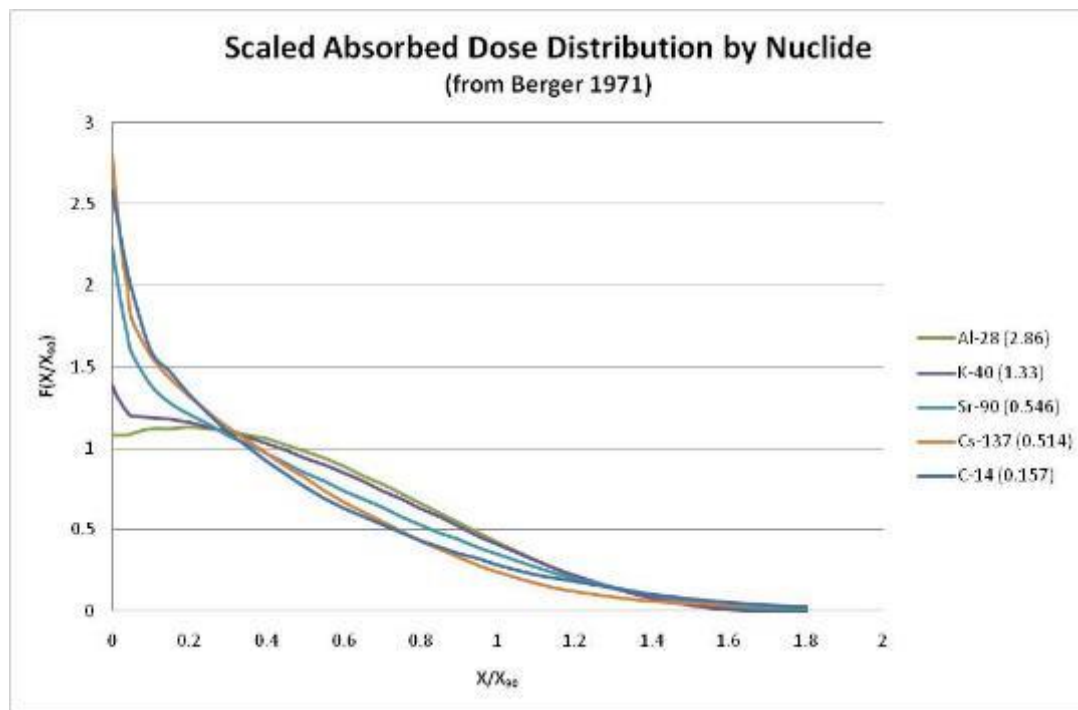
Berger determined the absorbed dose distribution for electrons of a given energy and depth of penetration (X); this is essentially a Bragg curve for monoenergetic electrons traveling through the absorber (water in this case).

When depth of penetration is normalized by the depth required to absorb 90% of its original energy (X_{90}), a Scaled Absorbed Dose Distribution is generated. The SADD is referred to by Berger as $F(X/X_{90})$.



SADD - By Nuclide

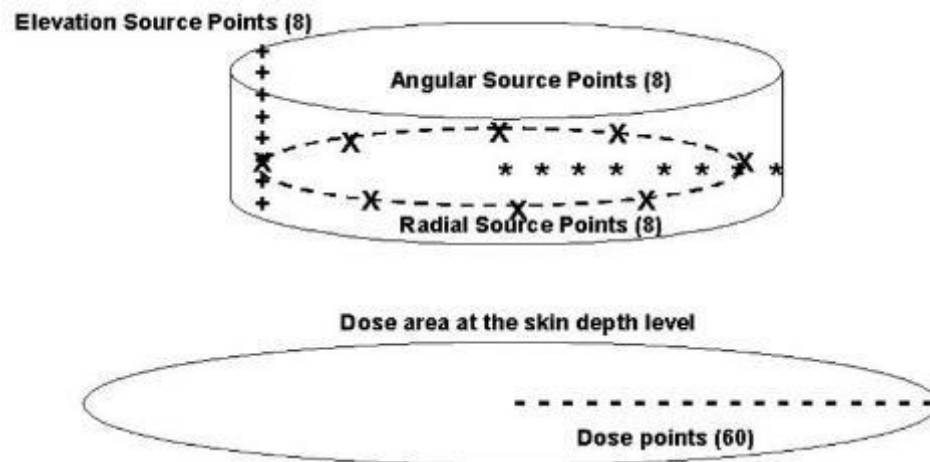
The beta energy emission spectra is folded with the energy-dependent scaled absorbed dose distribution to derive the nuclide-specific SADD.



Berger (1971) provides $F(X/X_{90})$ values for 75 beta emitters.

Symmetric-Source Dose Calculation

- Original VARSKIN begins at the center dose point of the irradiation area
- The code divides the source into very small sub-volumes (source points)
- The number of source points chosen is sufficient for convergence (checked along the way)



Varskin 3/4 Beta Dosimetry

- The dose rate at the next dose point along the radius is calculated until values are obtained at all sixty dose points
- If the dose profile defined by these sixty points as a function of target radius r is denoted by $D(r)$, then the skin dose, averaged over area of the disk, is given by:

$$\bar{D} = \frac{2\pi \int_0^R D(r) \cdot r \, dr}{\pi R^2}$$

Density Correction Model

- The original VARSKIN uses a *modified* path length to determine the energy lost in air or cover material(s) prior to entering the skin
- For small-diameter sources, the electron path from the source point to the dose point may pass through the side of the source (e.g., the path may exit the source and pass through air before penetrating the skin)
- The actual path length within the source is multiplied by the source density, and the path length outside the source and above the cover material is multiplied by the density of the material outside the source (air)
- The point-kernel distance is therefore “density modified”

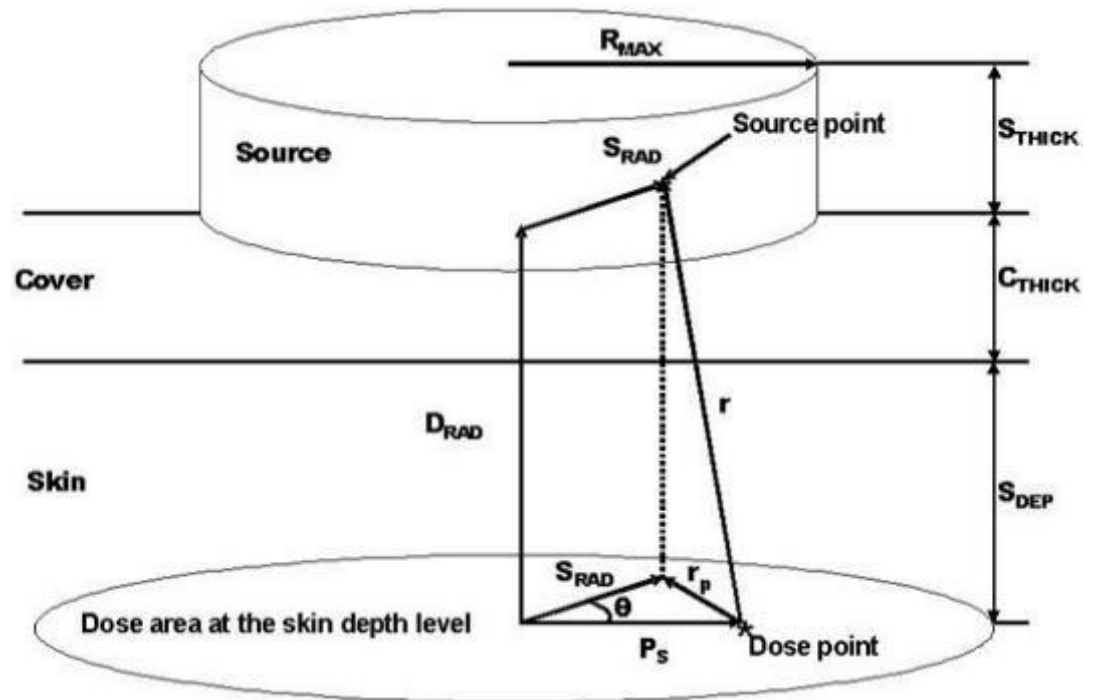
Density Correction Model

$$r_c = C_{thick} \cdot \left(r / D_{rad} \right)$$

$$r_t = S_{dep} \cdot \left(r / D_{rad} \right)$$

$$r_s = (D_{rad} - C_{thick} - S_{dep}) \cdot \left(r / D_{rad} \right)$$

$$r_1 = \frac{(r_s \rho_s + r_c \rho_c + r_t \rho_t)}{\rho_t}$$



How is Gamma Dose Determined?



VARSKIN 6

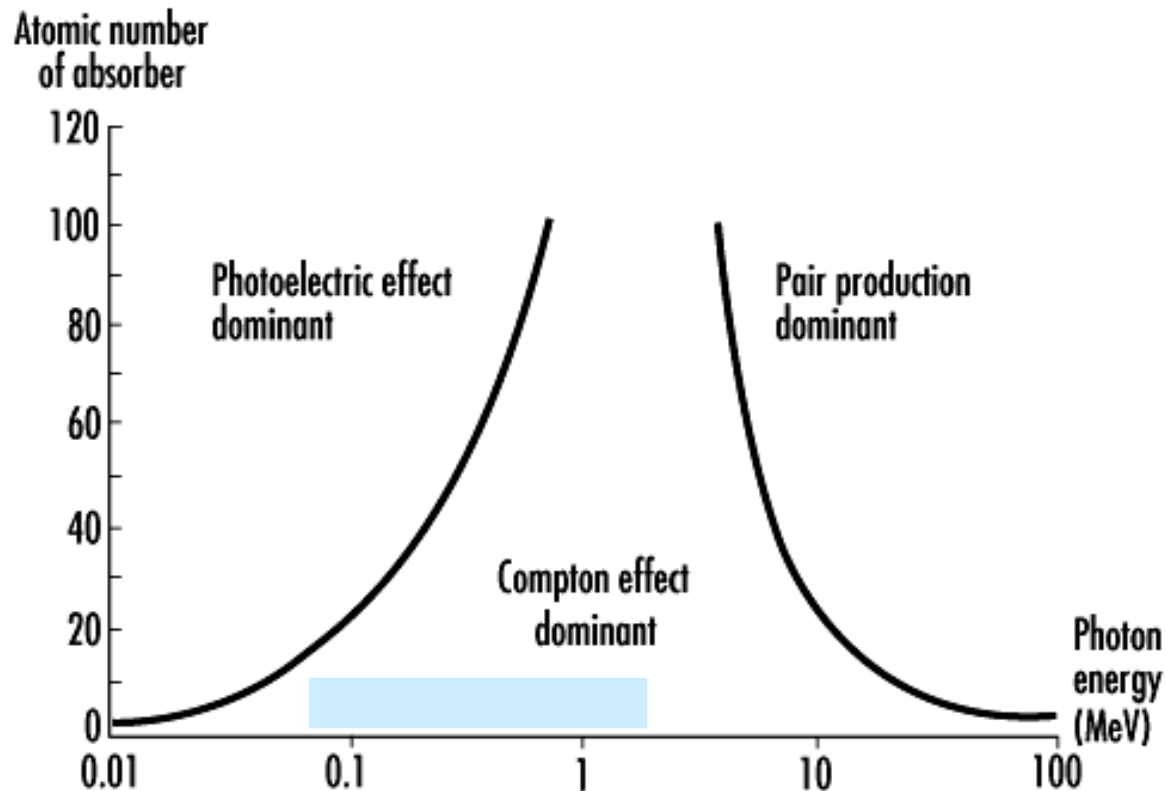


Photon Interactions and Dosimetry

Interaction Fundamentals

- Photon interactions are 'semi-random' events
- Photons generally interact with orbital electrons
- Interaction probability is governed by:
 - material (Z, electron density)
 - photon energy (E)
- ... and is described by an interaction coefficient
- Principal mechanisms of interaction include (by increasing energy):
 - Thomson/Rayleigh scatter (no E transfer)
 - photoelectric
 - Compton scatter
 - pair production
 - photo-disintegration (very high E)

Relative Importance by Interaction Type



Attenuation

- Attenuation is exponential and governed by the Beer-Lambert law
- Photon intensity *never* reaches zero
- Photon attenuation can be described by:

$$I = I_o e^{-\mu x}$$

- I_o = photon intensity (flux) prior to material
 - I = photon intensity after material
 - x = material thickness
 - μ = interaction coefficient (probability of interaction by any mechanism)
-
- For dosimetry considerations, coefficients are often necessary to describe the probability of interaction resulting in energy absorption
 - referred to as *mass absorption coefficient*, with units of area per unit mass

Energy Transfer - KERMA

- Kinetic Energy Relaxed in Matter
- Has units of energy per unit mass of material (J/kg, but not Gy)
- KERMA is directly related to:
 - the average energy transferred to material as a result of that interaction;
 - uncollided photon fluence; and
 - the probability (per unit density thickness) of a photon interaction.

$$K = \bar{E}_{tr} \cdot \Phi_0 \cdot \frac{\mu}{\rho}$$

Energy Absorption - Dose

- “Absorbed Dose” also has units of energy per unit mass (J/kg or Gy)
- Different from KERMA in that the energy is absorbed (rather than simply transferred)
- DOSE is directly related to:
 - the average energy absorbed in material as a result of that interaction;
 - uncollided photon fluence; and
 - the probability (per unit density thickness) of a photon interaction.

$$D = \bar{E}_{en} \cdot \Phi_0 \cdot \frac{\mu}{\rho}$$

Relationship Between KERMA and Dose

$$K = \bar{E}_{tr} \cdot \Phi_0 \cdot \frac{\mu}{\rho} = E_0 \cdot \Phi_0 \cdot \frac{\mu_{tr}}{\rho}$$

$$D = \bar{E}_{en} \cdot \Phi_0 \cdot \frac{\mu}{\rho} = E_0 \cdot \Phi_0 \cdot \frac{\mu_{en}}{\rho}$$

- $\frac{\mu_{tr}}{\rho}$ = probability per unit mass that energy is transferred to charged particles
- $\frac{\mu_{en}}{\rho}$ = probability per unit mass that energy is absorbed locally
- For low-energy photons, nearly all of energy transferred is deposited locally, therefore, KERMA is insignificantly different than absorbed dose

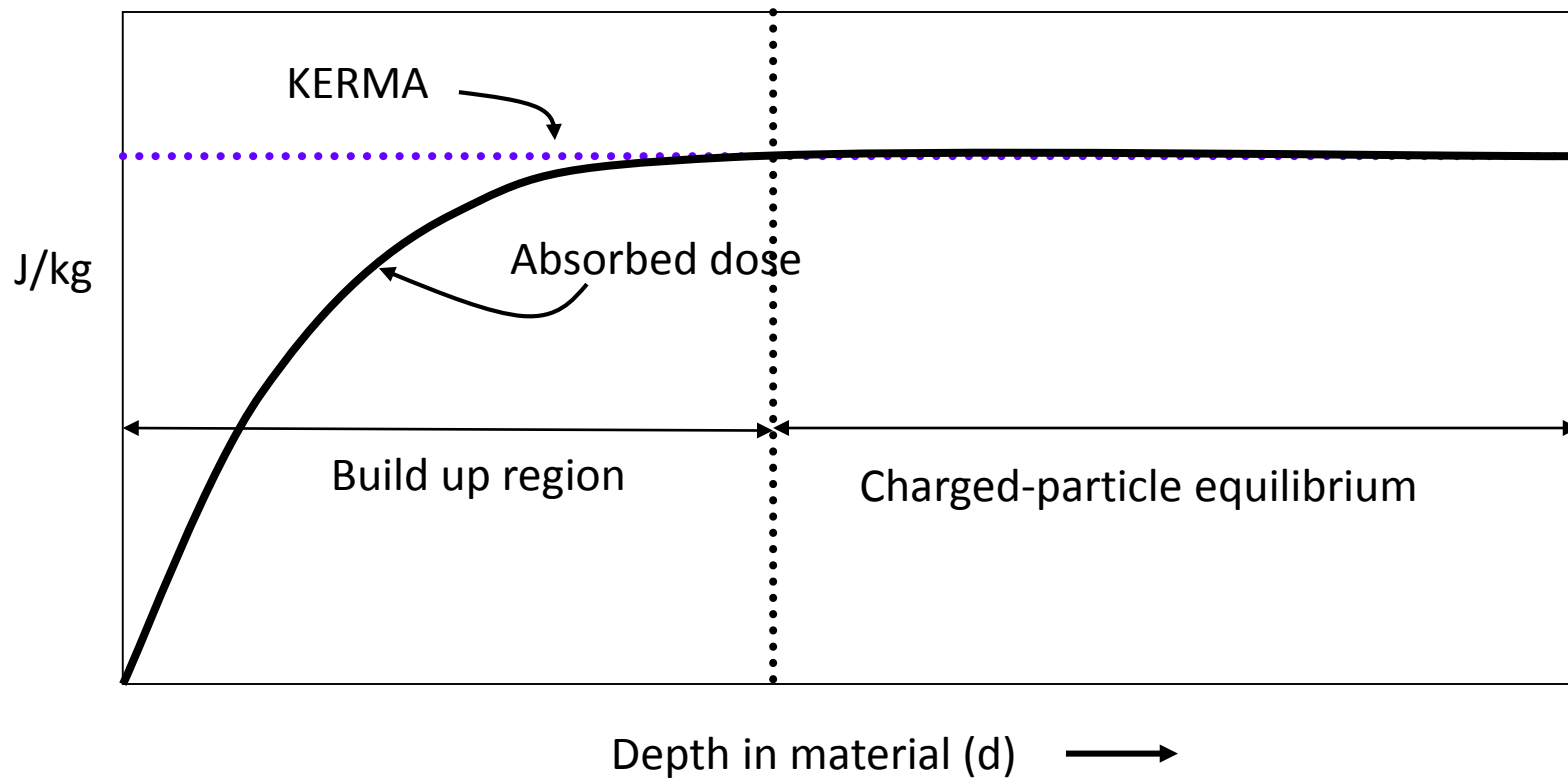
$$D = K \cdot \frac{\mu_{en}}{\mu_{tr}}$$

- For a given photon energy, and once “charged-particle equilibrium” is established:

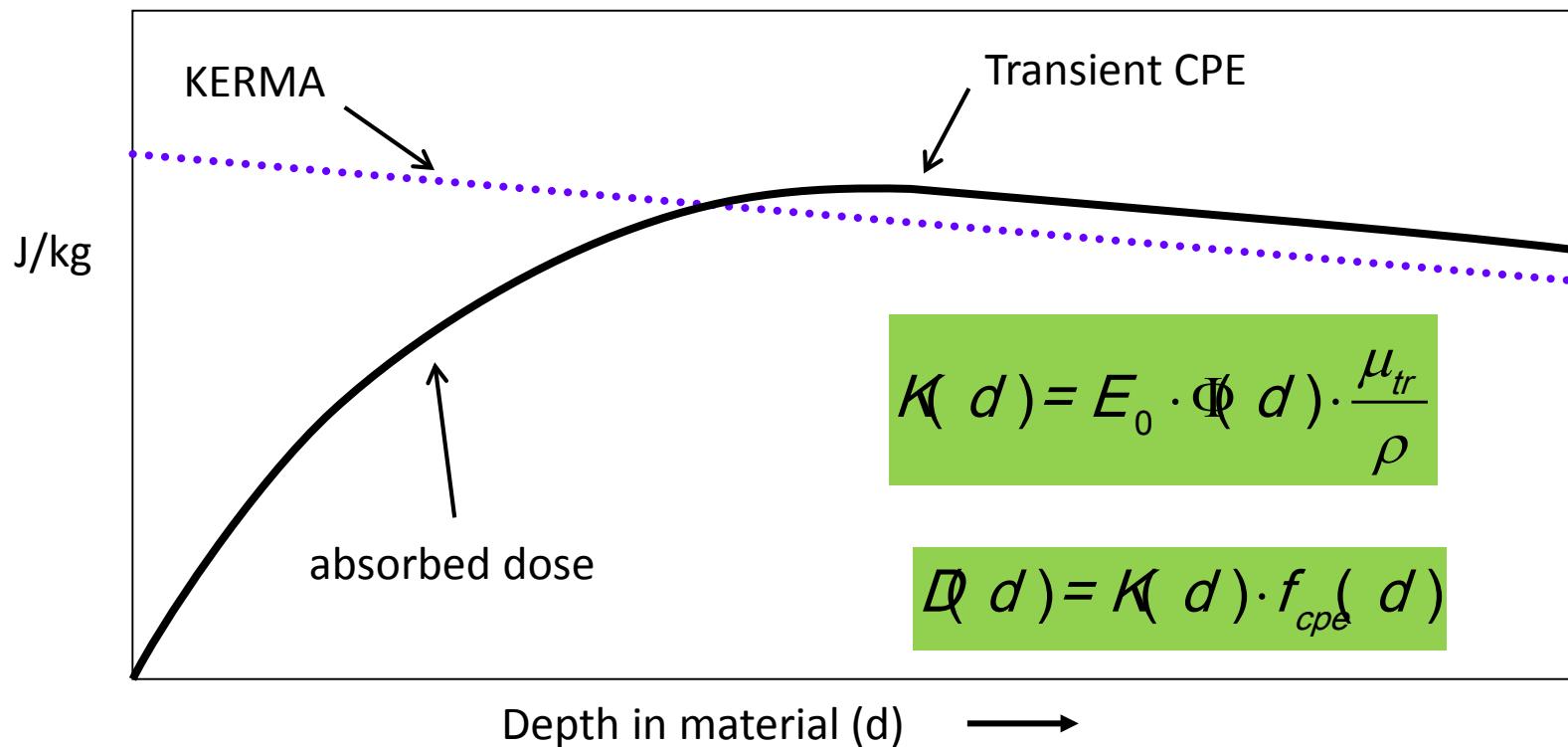
Charged-Particle Equilibrium

- Using a transfer coefficient, KERMA is easily estimated from photon flux
- Dose, as a function of depth, must then be determined from a conversion of KERMA based on the *buildup* of electronic charge, also as a function of depth
- *Charged-Particle Equilibrium* (cpe) is established once this charge buildup is complete

KERMA and Dose Buildup w/o Attenuation

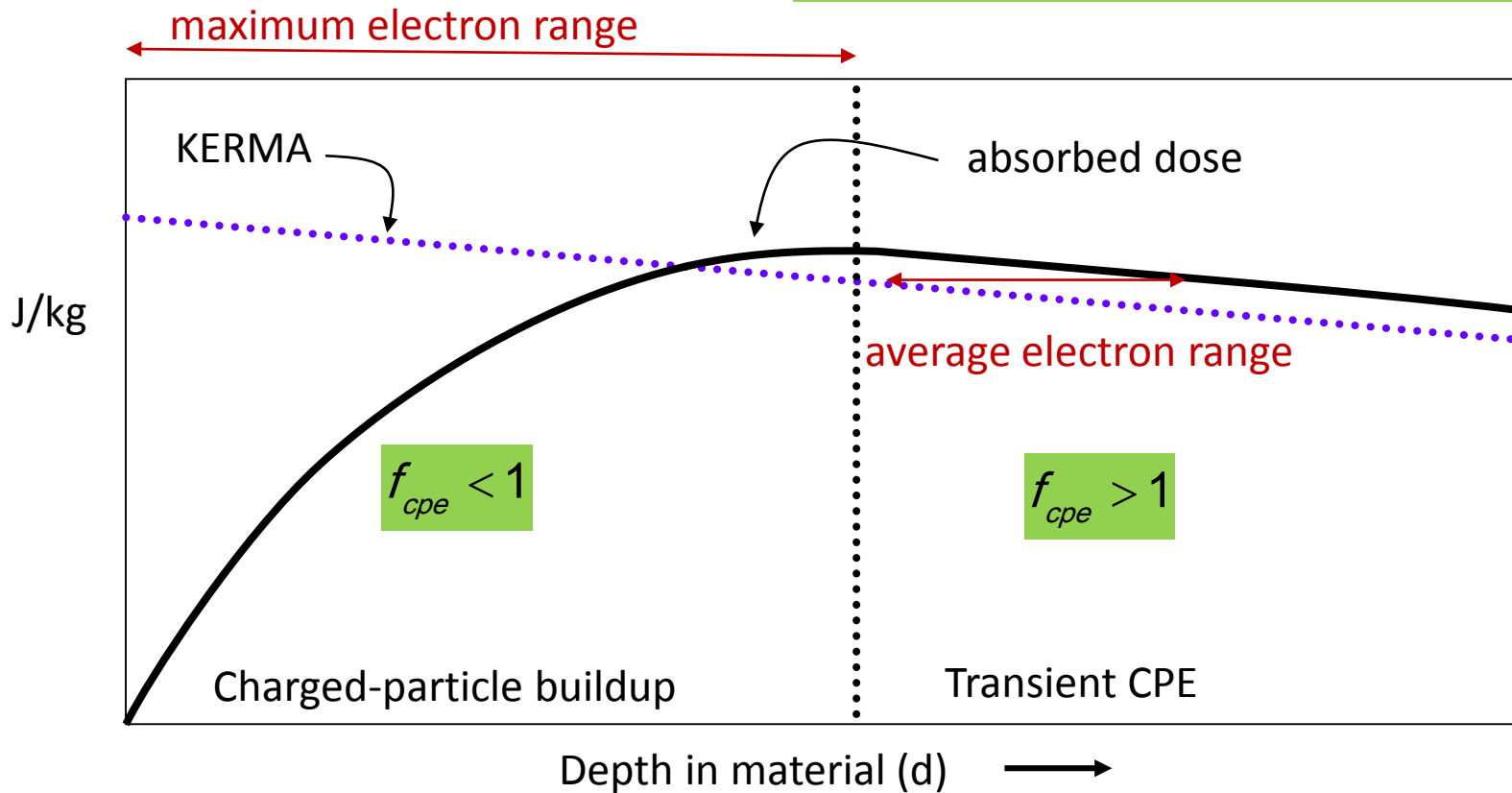


KERMA and Dose Buildup



details ...

$$D(d) = E_0 \cdot \Phi_0 e^{-\mu d} \cdot \frac{\mu_{tr}}{\rho} \cdot f_{cpe}(d)$$



Photon Dose at Shallow Depths

- Thus, with the flux attenuated by material and geometry, and charged particle buildup taken into account, the dose rate at depth d , is determined using:

$$\dot{D}(d) = E_0 \cdot \frac{S \cdot e^{-\mu d}}{4\pi d^2} \cdot \left(\frac{\mu_{tr}}{\rho} \right)_{tissue} \cdot f_{cpe}(d)$$

Photon Flux at Depth

Energy Transfer Probability

Photon Energy

Buildup Factor at Depth

VARSKIN Photon dosimetry

Varskin 3 Photon Dosimetry Model

- Expanded version of a method developed by Lantz and Lambert (1990)
- A point source is assumed (point at bottom center of all volumetric sources)
- All material between the source and target is considered *tissue*
- Estimated depth at which CPE is established is based on highest-energy photon
- Skin attenuation is not included, therefore low-E photons contribute to dose at all depths
 - low-E cutoff is offered as a way to account for this
- Dose calculated assuming 1 rad in tissue is equivalent to 1 R:

$$\Gamma \left[\frac{\text{rad cm}^2}{\text{hr mCi}} \right] = 1938 \left[\frac{\text{rad kg cm}^2}{\text{MeV mCi m}^2 \text{ hr}} \right] \cdot \left[\sum_{i=1}^n f_i \cdot E_i [\text{MeV}] \cdot \left(\frac{\mu_{en}}{\rho} \right)_{E_i, \text{tissue}} \left[\frac{\text{m}^2}{\text{kg}} \right] \right]$$

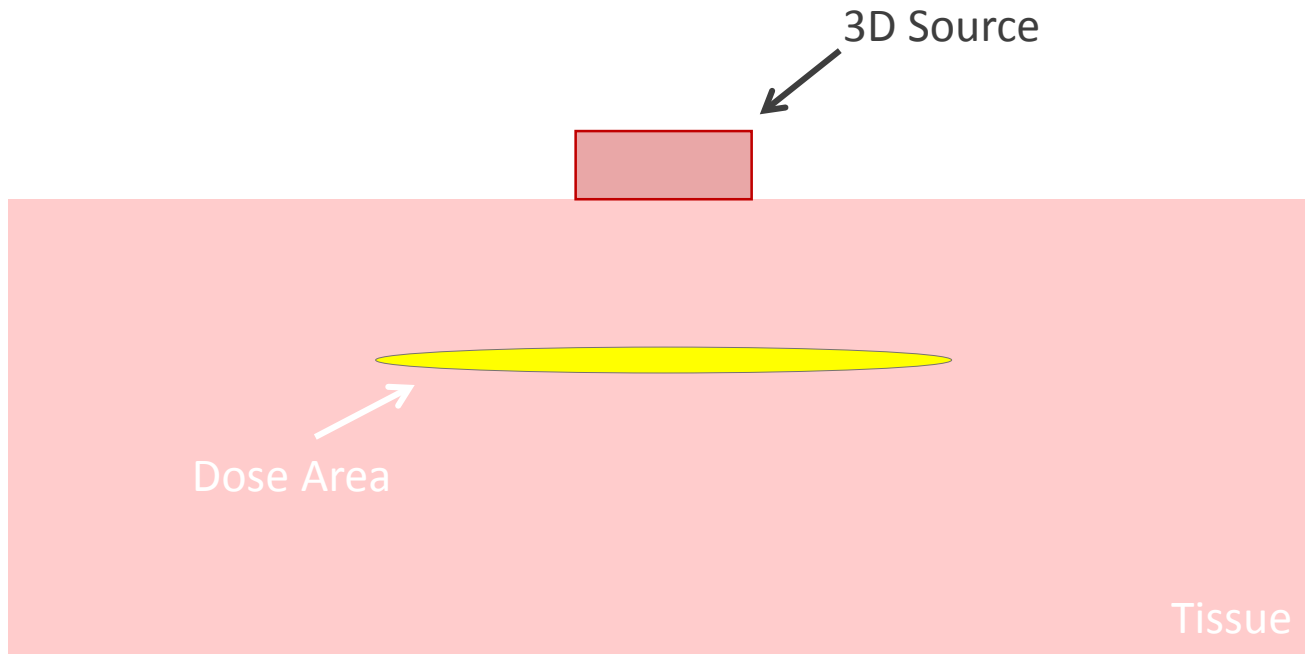
- Relevant data obtained from NIST, ICRU-44, and NUCDECAY files

VARSKIN 4/5/6 Photon Dosimetry

- The new VARSKIN photon dosimetry model introduced in VARSKIN 4 considers:
 - photon point-kernel methodology
 - charge-particle buildup; attenuation; off-axis scatter
 - numerical integration of 300 dose points for each source point
- Employs many of the same assumptions from the electron model:
 - multiple geometries (point, disk, cylinder, sphere, slab)
 - dose calculated to averaging disk (0.01 to 100 cm²) beneath skin at user specified depth
 - variable dose averaging
 - 2D averaging areas (regulatory compliance)
 - 3D averaging volumes (detector simulation)

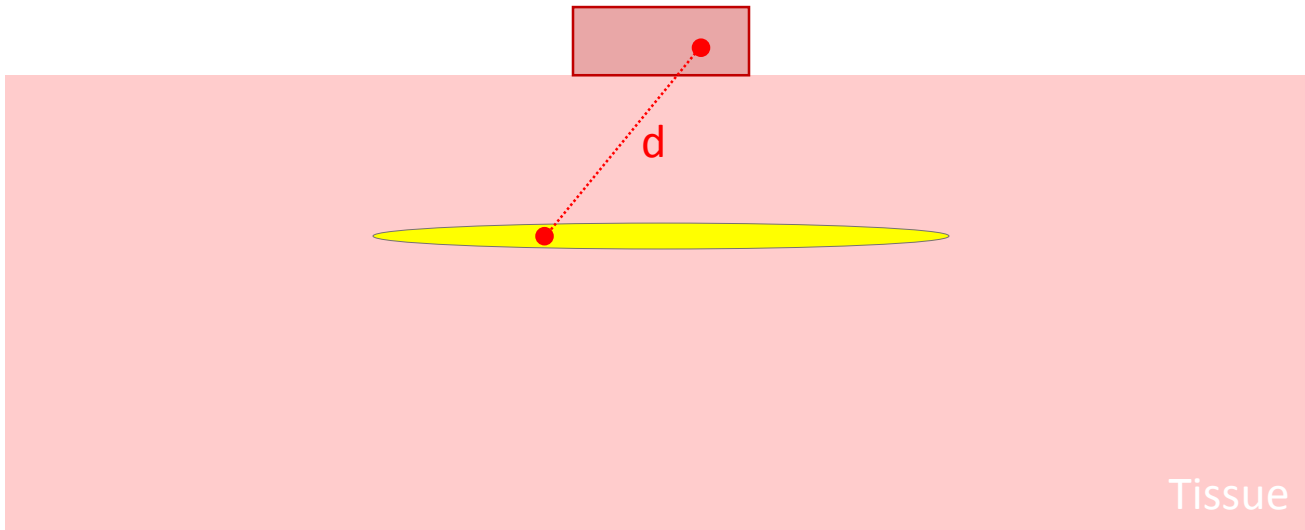
“Point Kernel” Concept

Now, let's put the dose equation to use ...



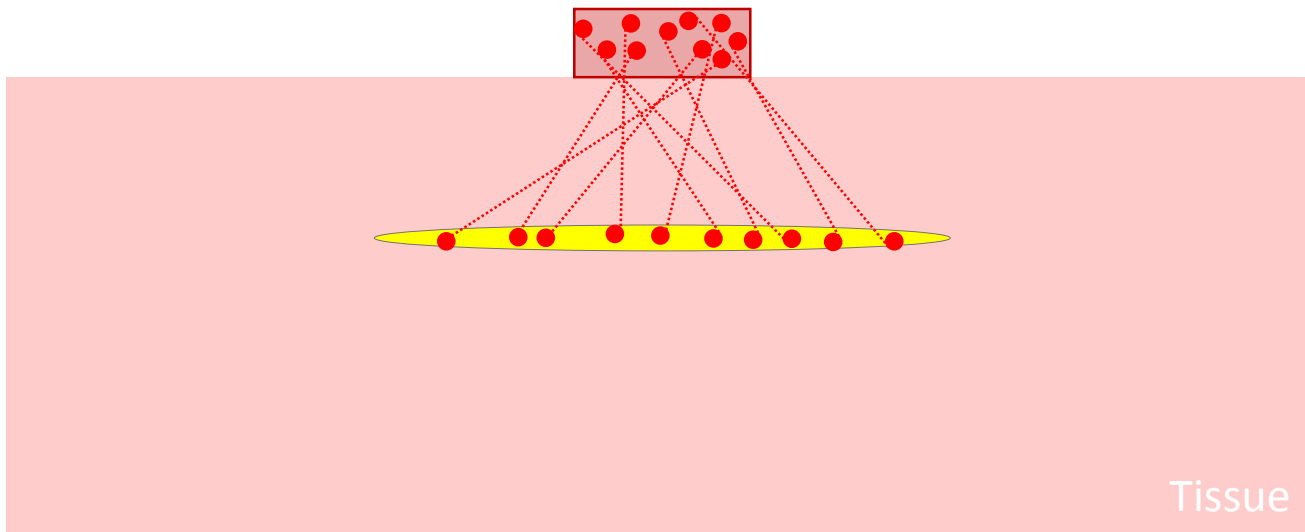
“Point Kernel” Concept

$$\frac{\dot{D}(d)}{S} = E_0 \cdot \frac{e^{-\mu d}}{4\pi d^2} \cdot \frac{\mu_{tr}}{\rho} \cdot f_{cpe}(d)$$



Integrate Point Kernels Over Source/Dose Volume

$$D(r, h) = \sum_i w_i \cdot D(r, d, \theta) = \sum_i w_i \cdot E_0 \cdot \frac{S}{4\pi d^2} e^{-\mu d} \cdot \frac{\mu_{tr}}{\rho} \cdot f_{cpe}(d)$$



Estimating Tissue Mass Attenuation Coefficients

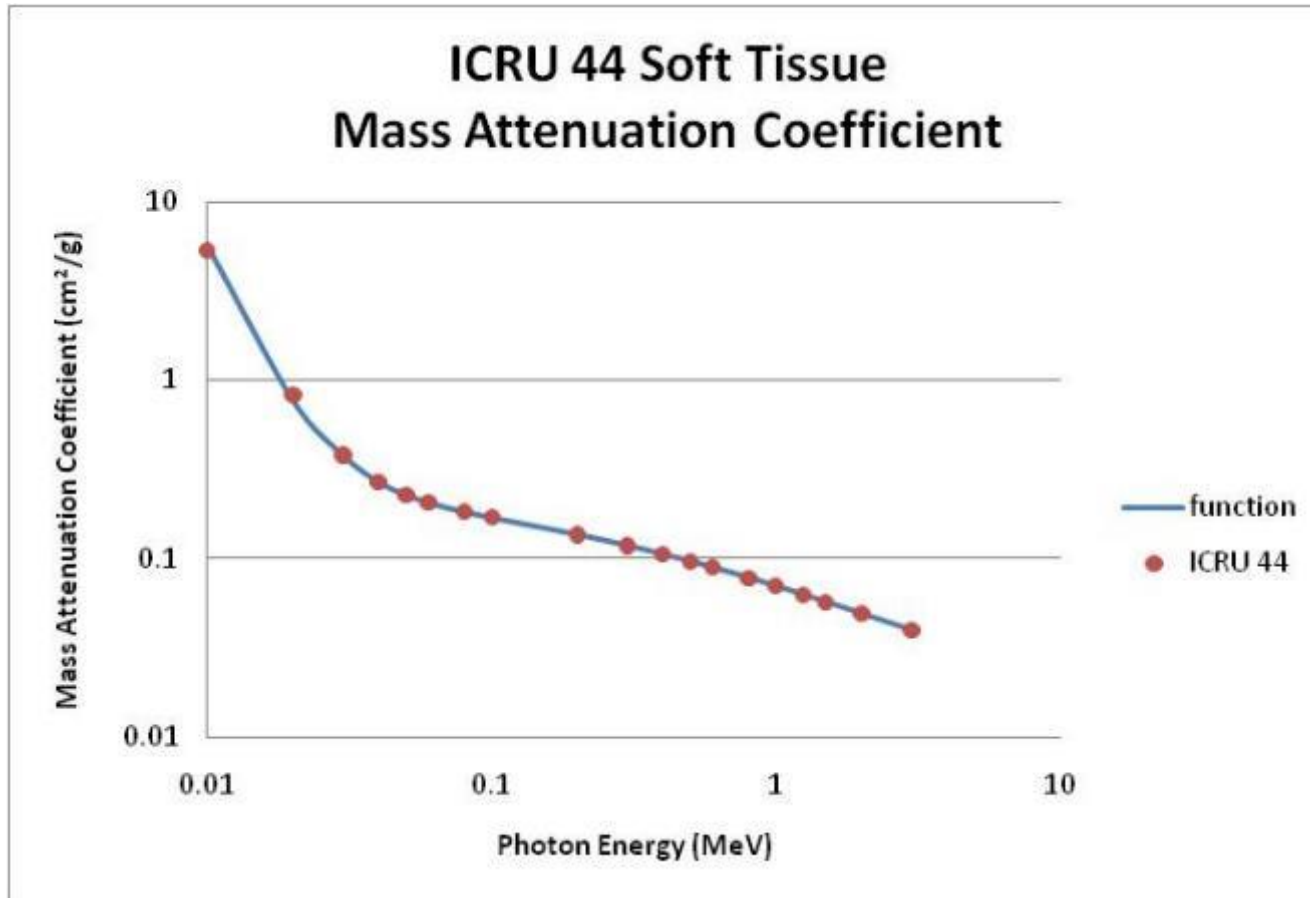
- As used in VARSKIN 4/5, an empirical relationship to estimate μ/ρ for tissue as a function of incident photon energy (in MeV) is given below.
- For energies less than or equal to 20 keV,

$$\frac{\mu}{\rho}(E) = \frac{1}{0.0000145 + 3810E^{2.5} + 134400E^3}$$

- and for energies greater than 20 keV,

$$\frac{\mu}{\rho}(E) = e^{\left[-3.22 - 0.11(\ln E)^2 + 0.5566\sqrt{E} - 0.7713 \ln E + \left(0.000721/E^2\right)\right]}$$

ICRU 44 soft tissue mass attenuation coefficients



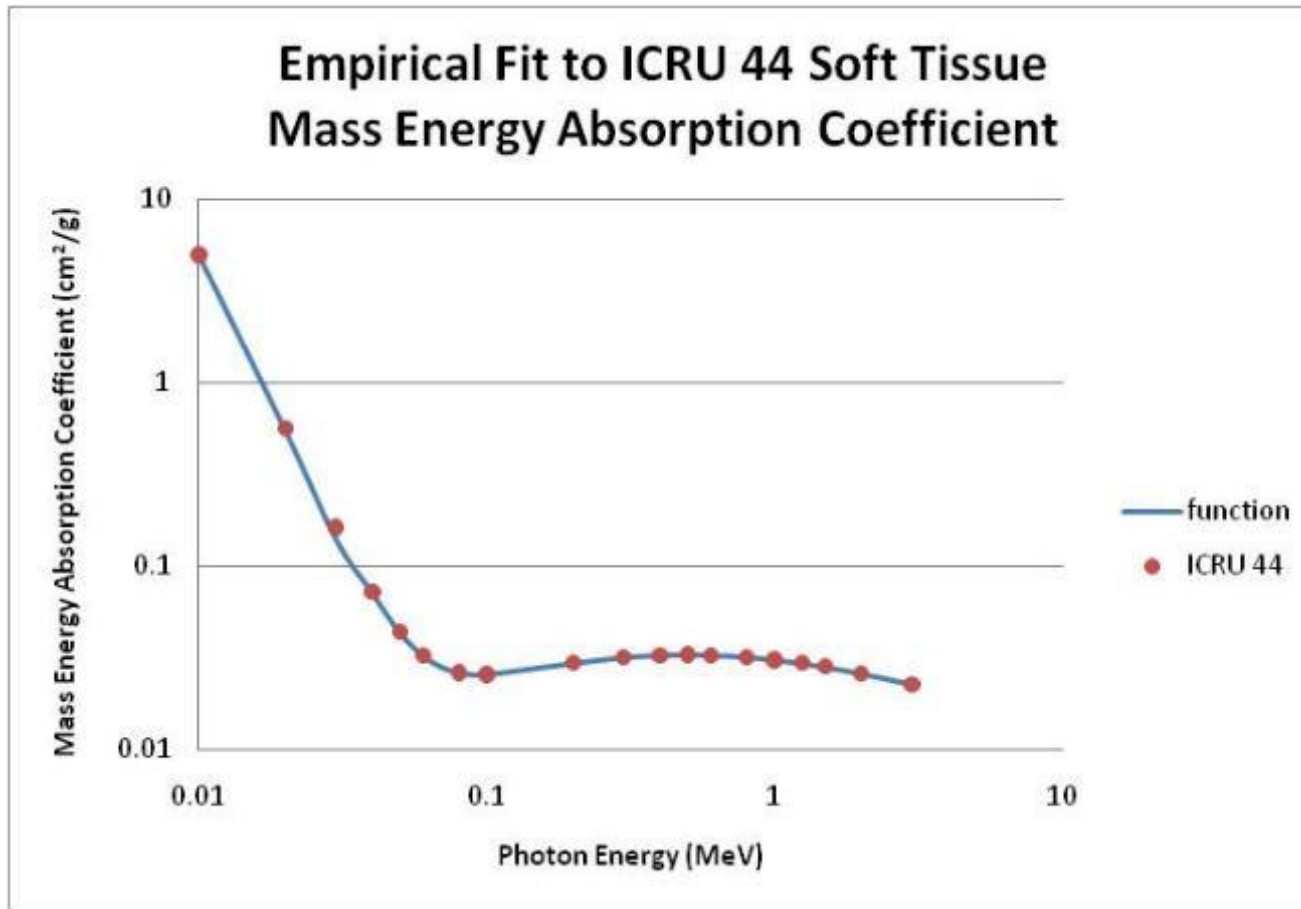
Estimating Tissue Energy Absorption Coefficients

- A function was developed to approximate the energy-dependent value of μ_{en}/ρ for tissue:

$$\frac{\mu_{en}}{\rho}(E) = \frac{a + c \ln E + e(\ln E)^2 + g(\ln E)^3 + i(\ln E)^4}{1 + b \ln E + d(\ln E)^2 + f(\ln E)^3 + h(\ln E)^4 + j(\ln E)^5}$$

- This function has a different set of coefficients for energies less than or equal to 30 keV and energies greater than 30 keV.

ICRU 44 soft tissue mass energy absorption coefficients



Accounting for CPE

CPE buildup correction factors, f_{CPE} , is defined as:

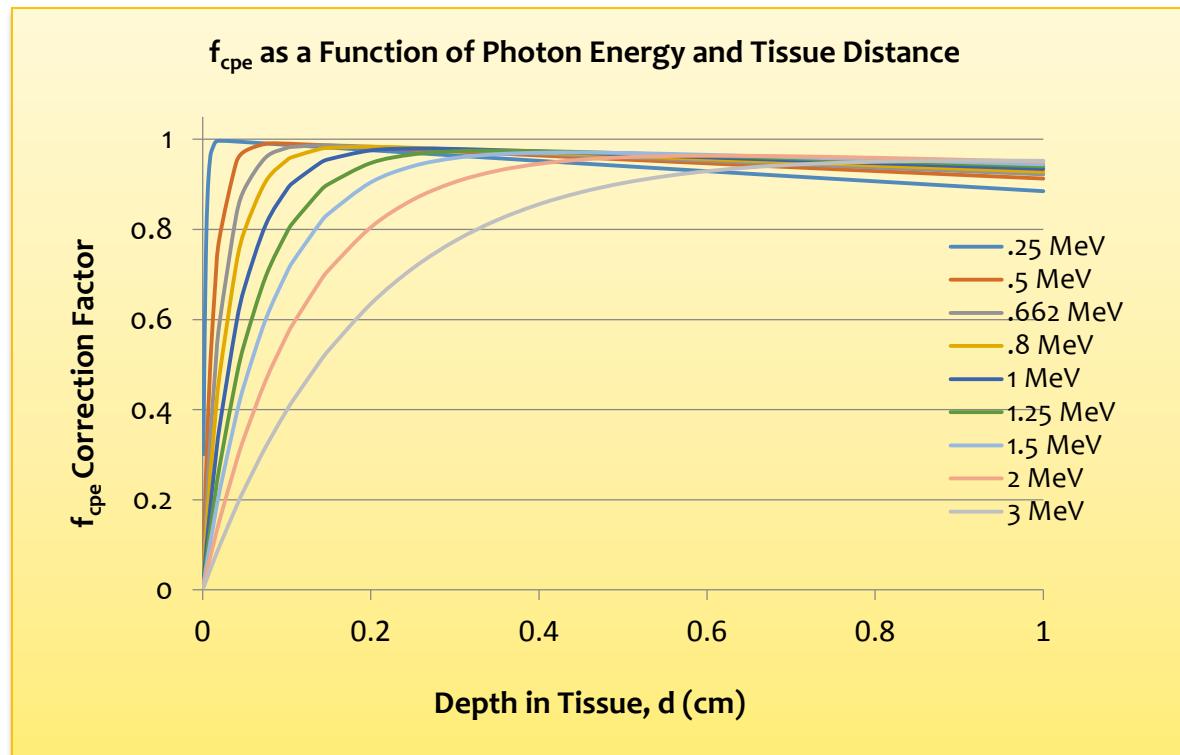
$$D(x) = K(x) \cdot f_{CPE}(x)$$

$$f_{CPE}(x) = \frac{D(x)}{K(x)} \rightarrow \frac{\sum^* f_8(x)}{f_6(x)}$$

Charged-Particle Buildup

- Using Monte Carlo simulation, the buildup correction factors were found to fit the general form:

$$\frac{1}{f_{cpe}(d, E)} = a + b \ln(d) + \frac{c}{\sqrt{d}}$$



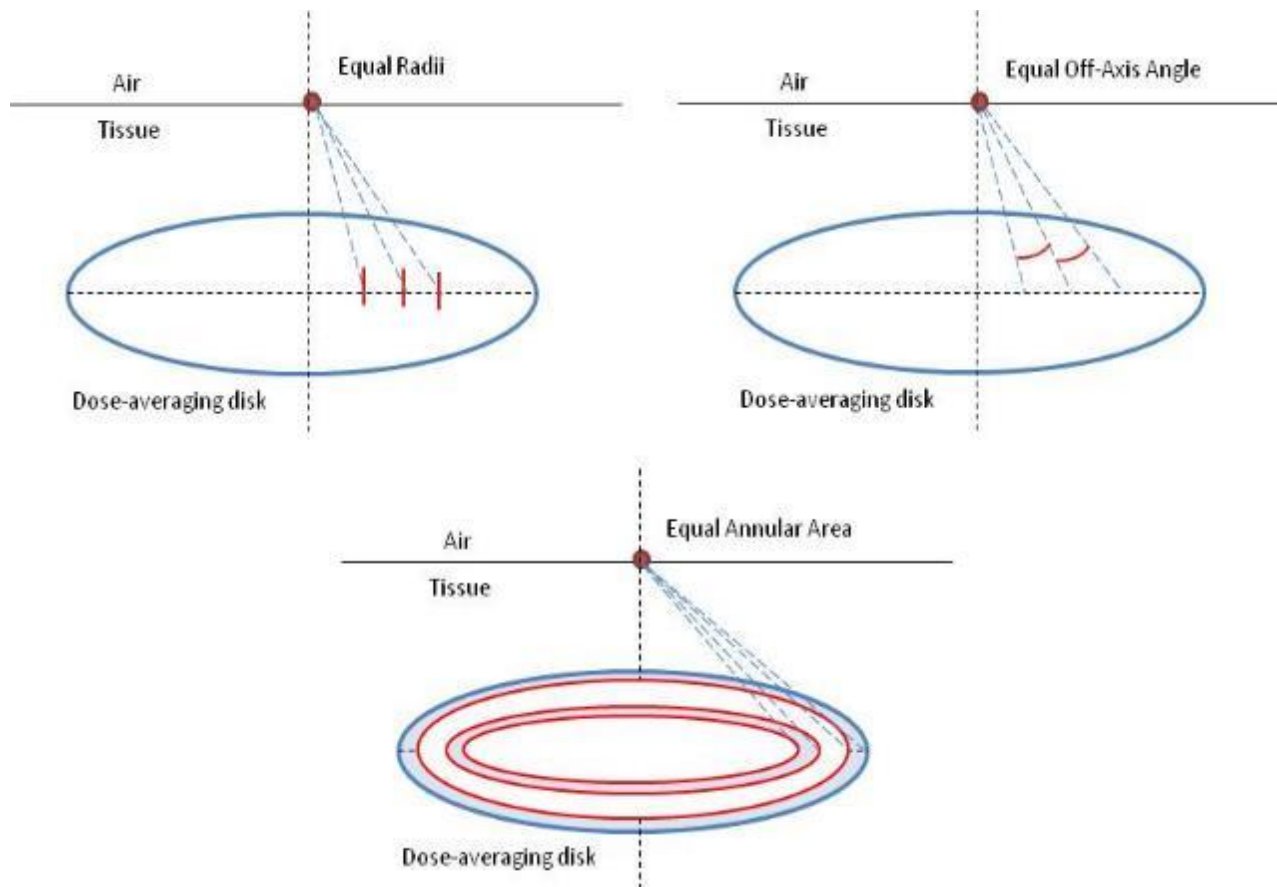
Numerical Integration Method

- Numerical integration provides
 - Average of point kernel dose over combination of photon emission locations
 - Within volume of source, and
 - Dose point locations
- Within infinitely thin disk of tissue
 - Depth h from the surface

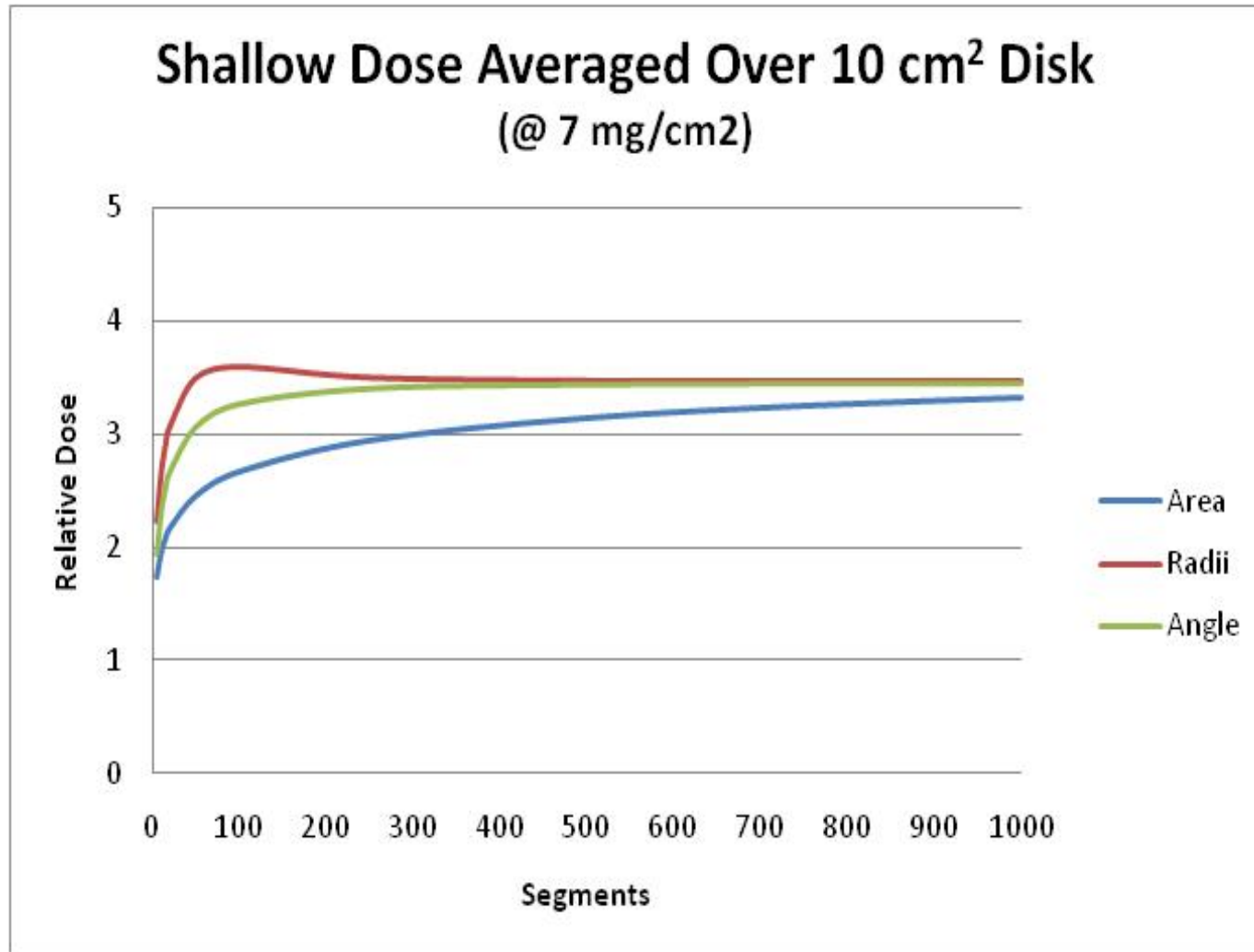
Approach to calculation

- Convergence studies conducted
- Dose averaging disk divided into segments
- Three segmenting methods examined
 - equal radii (quickest)
 - equal off-axis angle
 - equal annular area (slowest)

Methods used to select integration method



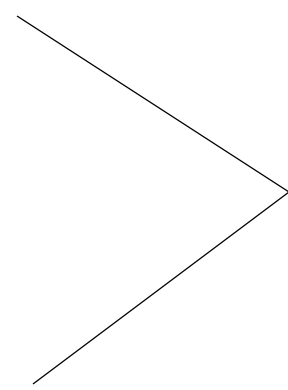
Relative dose as a function of the number of segments in a numerical integration (iterations), by method



VARSKIN 4 numerical integration utilizes 300 segments along the radius for the averaging disk. Convergence achieved with fewer segments for smaller disk

VARSKIN 4/5/6 exposure geometries

•Source Geometries

- Point ← Offset Particle Model
 - Disk
 - Cylinder
 - Sphere
 - Slab
 - Syringe
- ← Distributed Source Option
- ← Geometry eliminated
- 

VARSKIN 4/5/6 exposure options

- User specifies:
 - Source & Geometry
 - Dose depth
 - Dose averaging area
 - Volume averaging option
 - Air and cover thicknesses
- Multiple cover calculator
- Option to turn off photon dose calculations
- “Reset” feature to re-initialize parameters

Varskin 6.0

File Help

Source Geometry

☐ Point ☒ Sphere
☒ Disk ☐ Slab
☐ Cylinder

Special Options

☐ Exclude Photon Dose
☐ Exclude Electron Dose
☐ Perform Volume Averaging
☒ Offset Particle Model

Skin Averaging Area

10 cm²

Exposure Time

60 min

Radionuclide Library [Zeff]

C-14 [7.42] 38
Ce-144 [7.42] 107
Ce-144 [7.42] 107D
Ce-144 [7.42] 38
Ce-144 [7.42] 38D
Co-60 [25.5] 38
Pr-144 [7.42] 107
Pr-144 [7.42] 38
Pr-144m [7.42] 38
Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

Point Source Irradiation Geometry

Skin Thickness or Skin Density Thickness: 7 mg/cm²

Air Gap Thickness: 0 mm

Cover Thickness: 0 mm

Cover Density: 0 g/cm³

Multiple Cover Calculator

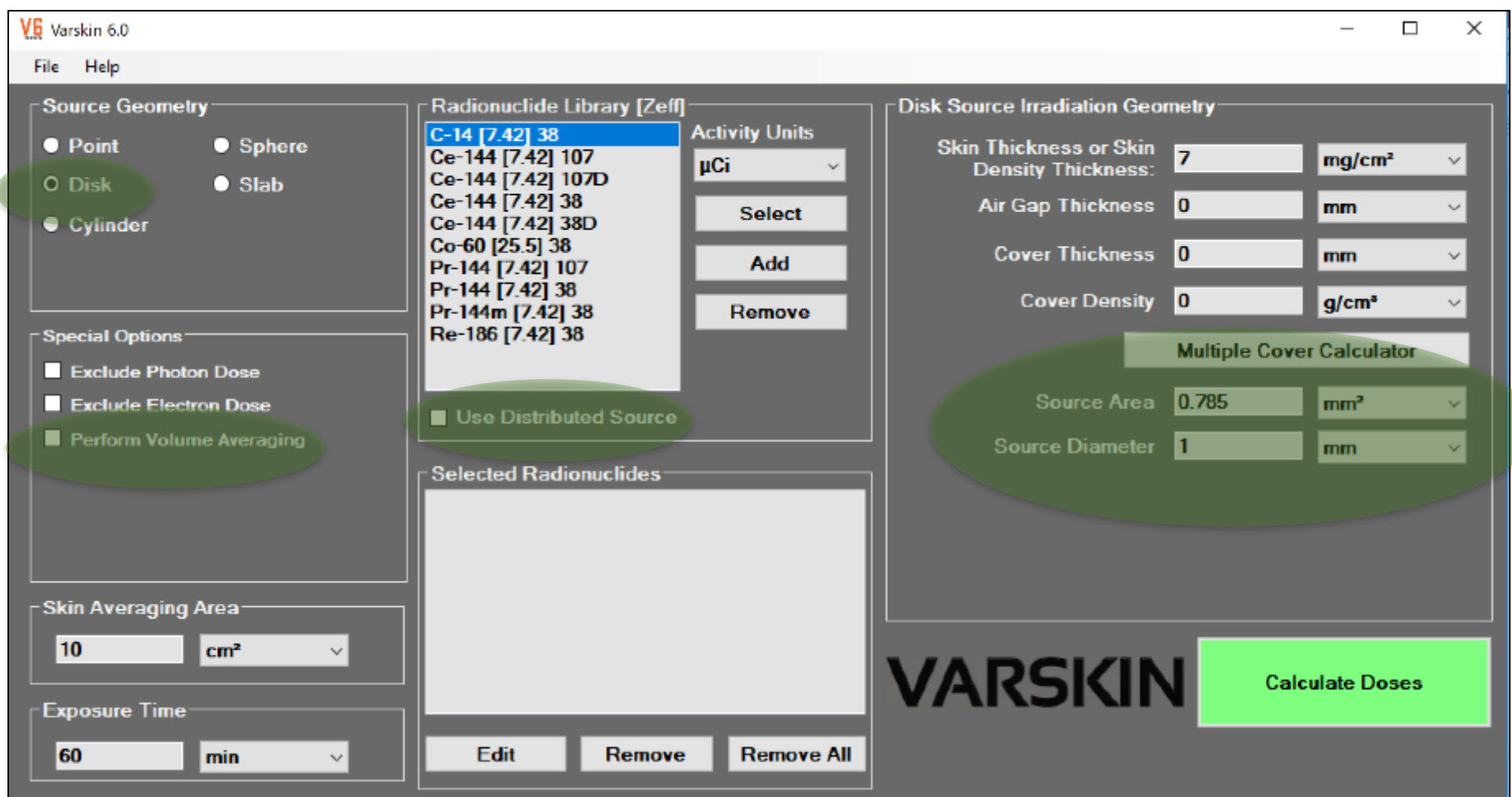
Selected Radionuclides

Edit Remove Remove All

VARSKIN

Calculate Doses

air gap (5 cm max) is always adjacent to the skin



Source Geometry

- ☐ Point ☐ Sphere
☐ Disk ☐ Slab
☒ Cylinder

Special Options

- ☐ Exclude Photon Dose
☐ Exclude Electron Dose
☐ Perform Volume Averaging

Skin Averaging Area

10 cm²

Exposure Time

60 min

Radionuclide Library [Zeff]

C-14 [7.42] 38
Ce-144 [7.42] 107
Ce-144 [7.42] 107D
Ce-144 [7.42] 38
Ce-144 [7.42] 38D
Co-60 [25.5] 38
Pr-144 [7.42] 107
Pr-144 [7.42] 38
Pr-144m [7.42] 38
Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

☐ Use Distributed Source

Selected Radionuclides

Edit

Remove

Remove All

Cylinder Source Irradiation Geometry

Skin Thickness or Skin Density Thickness: 7 mg/cm²

Air Gap Thickness 0 mm

Cover Thickness 0 mm

Cover Density 0 g/cm³

Multiple Cover Calculator

Source Diameter 1 mm

Source Thickness 1 μm

Source Density 1 g/cm³

VARSKIN

Calculate Doses

Varskin 6.0

FileHelp

Source Geometry

☐ Point

☒ Sphere

☐ Disk

☐ Slab

☐ Cylinder

Special Options

☐ Exclude Photon Dose

☐ Exclude Electron Dose

☐ Perform Volume Averaging

Skin Averaging Area

10

cm²

Exposure Time

60

min

Radionuclide Library [Zeff]

C-14 [7.42] 38

Ce-144 [7.42] 107

Ce-144 [7.42] 107D

Ce-144 [7.42] 38

Ce-144 [7.42] 38D

Co-60 [25.5] 38

Pr-144 [7.42] 107

Pr-144 [7.42] 38

Pr-144m [7.42] 38

Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

☐ Use Distributed Source

Selected Radionuclides

Edit

Remove

Remove All

Sphere Source Irradiation Geometry

Skin Thickness or Skin Density Thickness:

7

mg/cm²

Air Gap Thickness

0

mm

Cover Thickness

0

mm

Cover Density

0

g/cm³

Multiple Cover Calculator

Source Diameter

1

mm

Source Density

1

g/cm³

VARSKIN

Calculate Doses

Source Geometry

- ☐ Point ☐ Sphere
☐ Disk ☒ Slab
☐ Cylinder

Special Options

- ☐ Exclude Photon Dose
☐ Exclude Electron Dose
☐ Perform Volume Averaging

Skin Averaging Area

10 cm²

Exposure Time

60 min

Radionuclide Library [Zeff]

C-14 [7.42] 38
Ce-144 [7.42] 107
Ce-144 [7.42] 107D
Ce-144 [7.42] 38
Ce-144 [7.42] 38D
Co-60 [25.5] 38
Pr-144 [7.42] 107
Pr-144 [7.42] 38
Pr-144m [7.42] 38
Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

☐ Use Distributed Source

Selected Radionuclides

Edit

Remove

Remove All

Slab Source Irradiation Geometry

Skin Thickness or Skin Density Thickness: 7 mg/cm²

Air Gap Thickness 0 mm

Cover Thickness 0 mm

Cover Density 0 g/cm³

Multiple Cover Calculator

X-Side Length 1 μm

Y-Side Length 1 μm

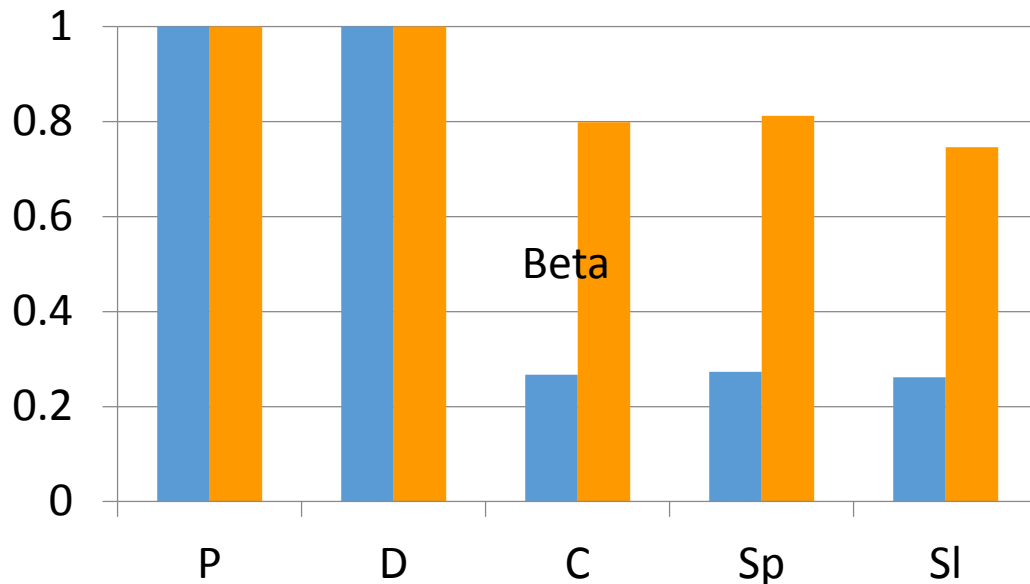
Source Thickness 1 μm

Source Density 1 g/cm³

VARSKIN

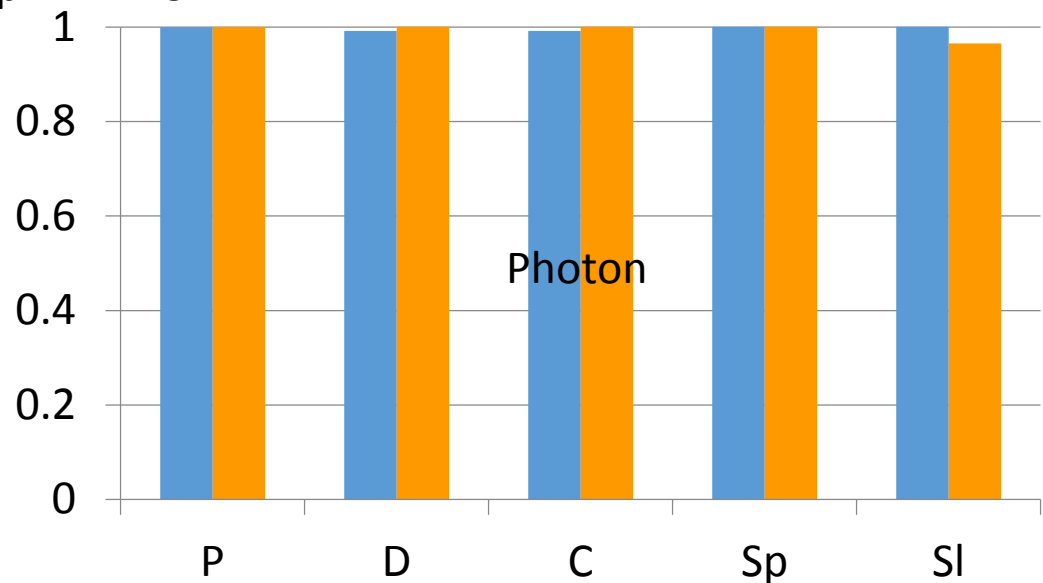
Calculate Doses

Impact of Source Geometry

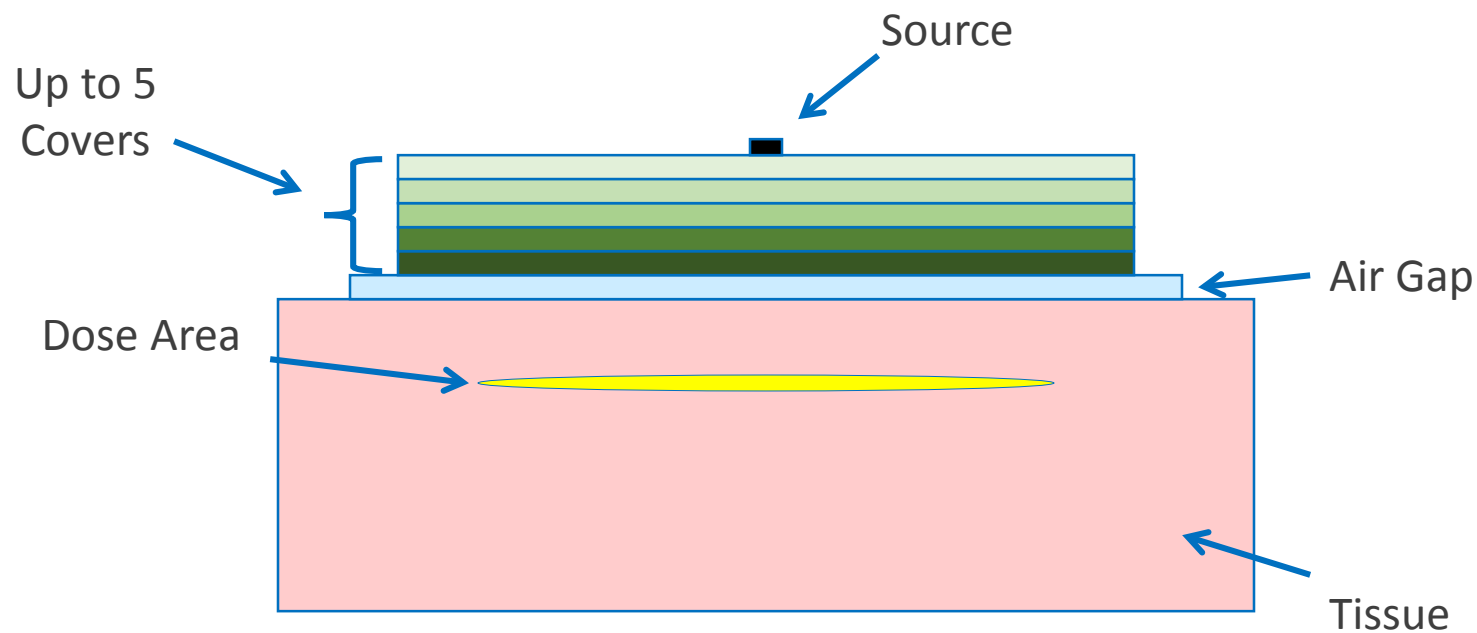


^{60}Co (0.318; 1.25)
 ^{106}Rh (3.54; 0.512)

Dose relative to point geometry
1 mm dimensions
10 cm² area
Shallow dose



Cover model



Cover Materials

- Up to 5 layers above the skin are allowed (air next to skin, if present)
- Attenuation in cover materials is considered

For Photons...

- The presence of cover materials
 - disrupts CPE, adds depth, and alters off-axis geometry
- Material layers are restricted to “cotton” or “latex”
- Cotton or latex attenuation is energy dependent
 - if $\rho > 1.25 \text{ g/cm}^2$ (cotton assumed)
 - if $\rho < 1.25 \text{ g/cm}^2$ (latex assumed)
- For photon attenuation, the cover material is assumed to be air
 - insignificant for very small volumetric sources and for photon energies above $\sim 50 \text{ keV}$

Air-Gap Model

- The presence of air between source and skin
 - disrupts charged-particle buildup
 - adds depth to dose calculation
 - alters off-axis geometry
- The air layer can be model only as being in contact with the skin surface
- Attenuation in air is considered

Special Options

- Exclude Photon Dose (off)
- Exclude Electron Dose (off)
- Perform Volume Averaging (off)
 - errors possible with large values
- Offset Particle Model (off)
 - available only for point source geometry and only for photon dosimetry

Source Geometry

- ☐ Point ☒ Sphere
☐ Disk ☐ Slab
☐ Cylinder

Special Options

- ☐ Exclude Photon Dose
☐ Exclude Electron Dose
☐ Perform Volume Averaging
☐ Offset Particle Model

Skin Averaging Area

10 cm²

Exposure Time

60 min

Radionuclide Library [Zeff]

C-14 [7.42] 38
Ce-144 [7.42] 107
Ce-144 [7.42] 107D
Ce-144 [7.42] 38
Ce-144 [7.42] 38D
Co-60 [25.5] 38
Pr-144 [7.42] 107
Pr-144 [7.42] 38
Pr-144m [7.42] 38
Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

Selected Radionuclides

Edit

Remove

Remove All

Point Source Irradiation Geometry

Skin Thickness or Skin Density Thickness: 7 mg/cm²

Air Gap Thickness 0 mm

Cover Thickness 0 mm

Cover Density 0 g/cm³

Multiple Cover Calculator

VARSKIN

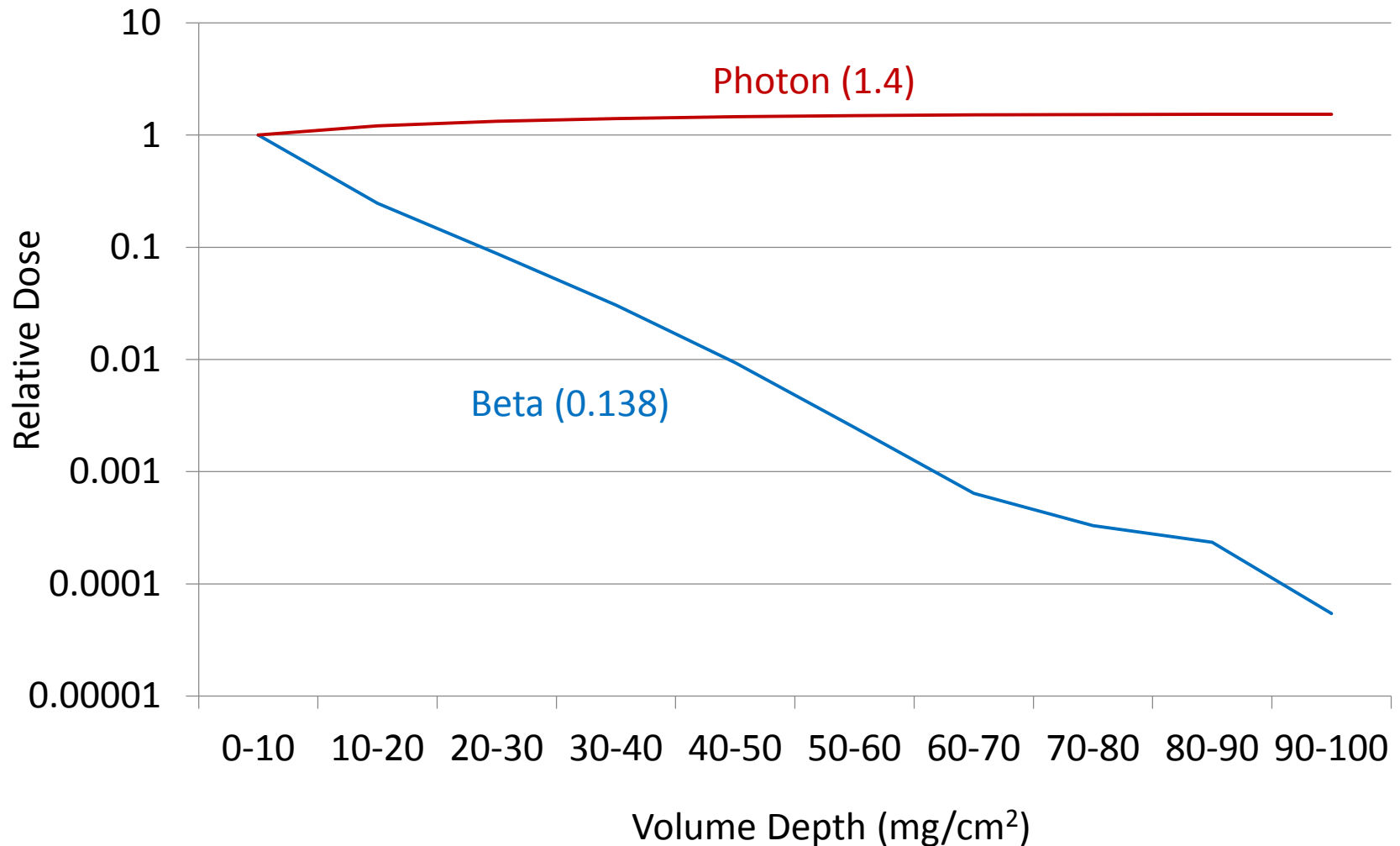
Calculate Doses

Volume Averaging

- Averaging cell is a cylinder defined laterally by the skin averaging area, with a user-specified top and bottom
- As defaults, the “top” of the cell is assumed to be the skin surface (0 mg/cm²) and the “bottom” is assumed to be equal to the range of the maximum energy electron for the chosen radionuclide (not to exceed 1500 mg/cm²)

Volume Averaging

^{60}Co ; point source; 10 cm^2 ; (0-100 mg/cm^2)



Varskin 6.0

File Help

Source Geometry

☐ Point

☐ Sphere

☐ Disk

☐ Slab

☐ Cylinder

Special Options

☐ Exclude Photon Dose

☐ Exclude Electron Dose

☐ Perform Volume Averaging

☒ Offset Particle Model

Offset Value:

0

cm

Skin Averaging Area

10

cm²

Exposure Time

60

min

Radionuclide Library [Zeff]

C-14 [7.42] 38

Ce-144 [7.42] 107

Ce-144 [7.42] 107D

Ce-144 [7.42] 38

Ce-144 [7.42] 38D

Co-60 [25.5] 38

Pr-144 [7.42] 107

Pr-144 [7.42] 38

Pr-144m [7.42] 38

Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

Selected Radionuclides

Edit

Remove

Remove All

Point Source Irradiation Geometry

Skin Thickness or Skin Density Thickness:

7

mg/cm²

Air Gap Thickness

0

mm

Cover Thickness

0

mm

Cover Density

0

g/cm³

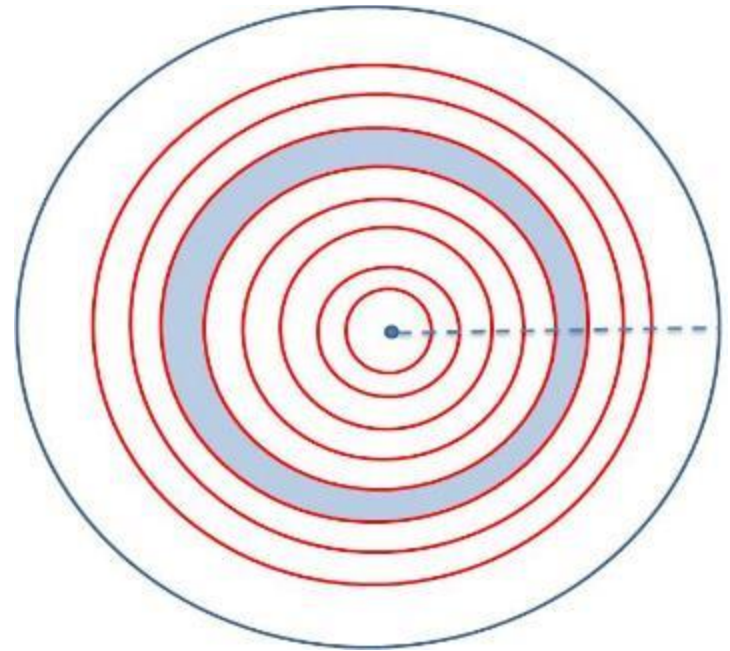
Multiple Cover Calculator

VARSKIN

Calculate Doses

On-Axis Calculation of Dose

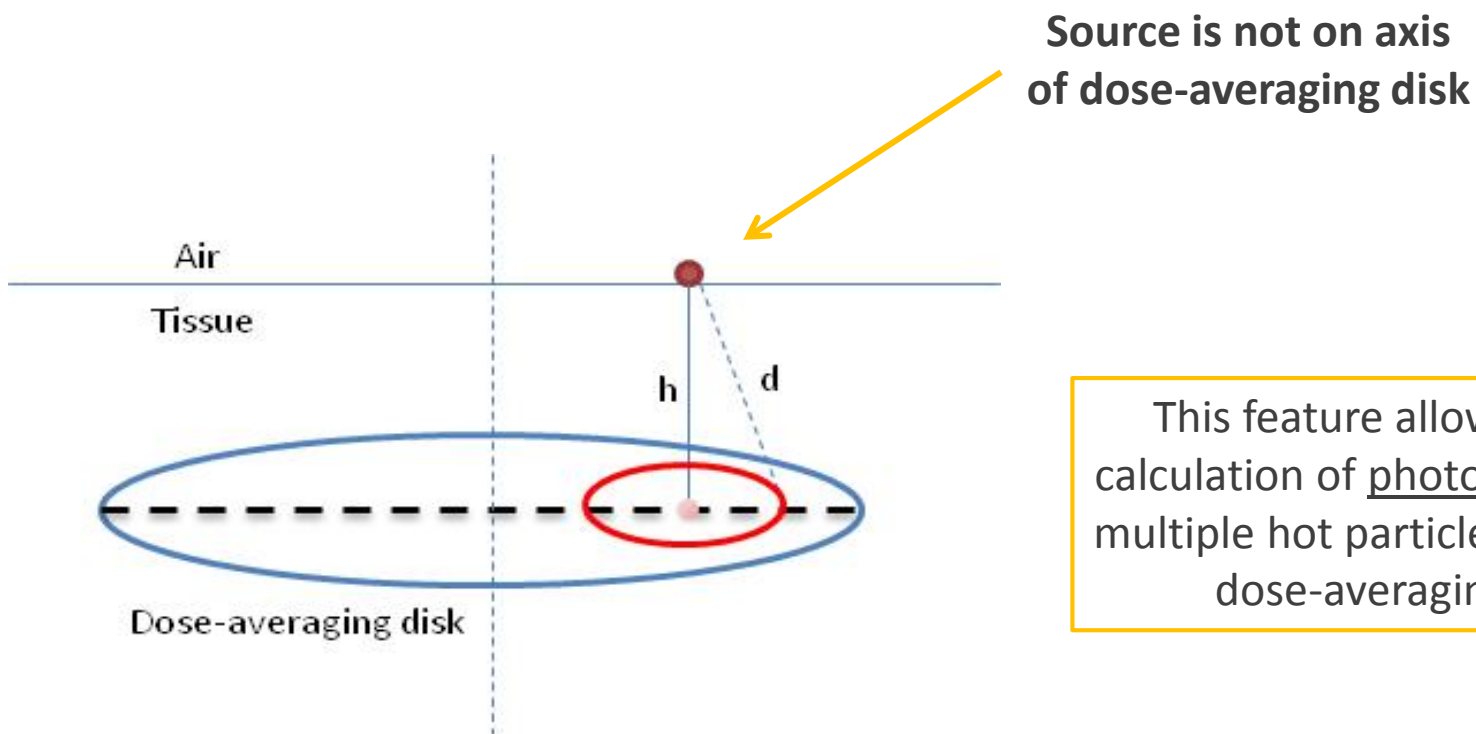
- Varskin 3 calculated dose at 60 locations around the dose-averaging disk
 - Method tends to weight the average such that it provides an over-estimation
- For VARSKIN 4, we assumed the following:
 - Point source is located directly above and on-axis with the averaging disk
 - Presumes symmetry in calculations along a radius of the dose-averaging disk
 - Weighted by the fractional area of each annulus
 - Provides a better estimate of average dose to the entire disk



Offset Particle Model

- For point source, photon dosimetry
- To estimate the greatest dose to a single averaging area beneath multiple sources
- Used when two (or more) hot particles are in proximity to each other (when separation is less than the diameter of the averaging area)
- On selection, user must enter the Offset Value (0 cm)

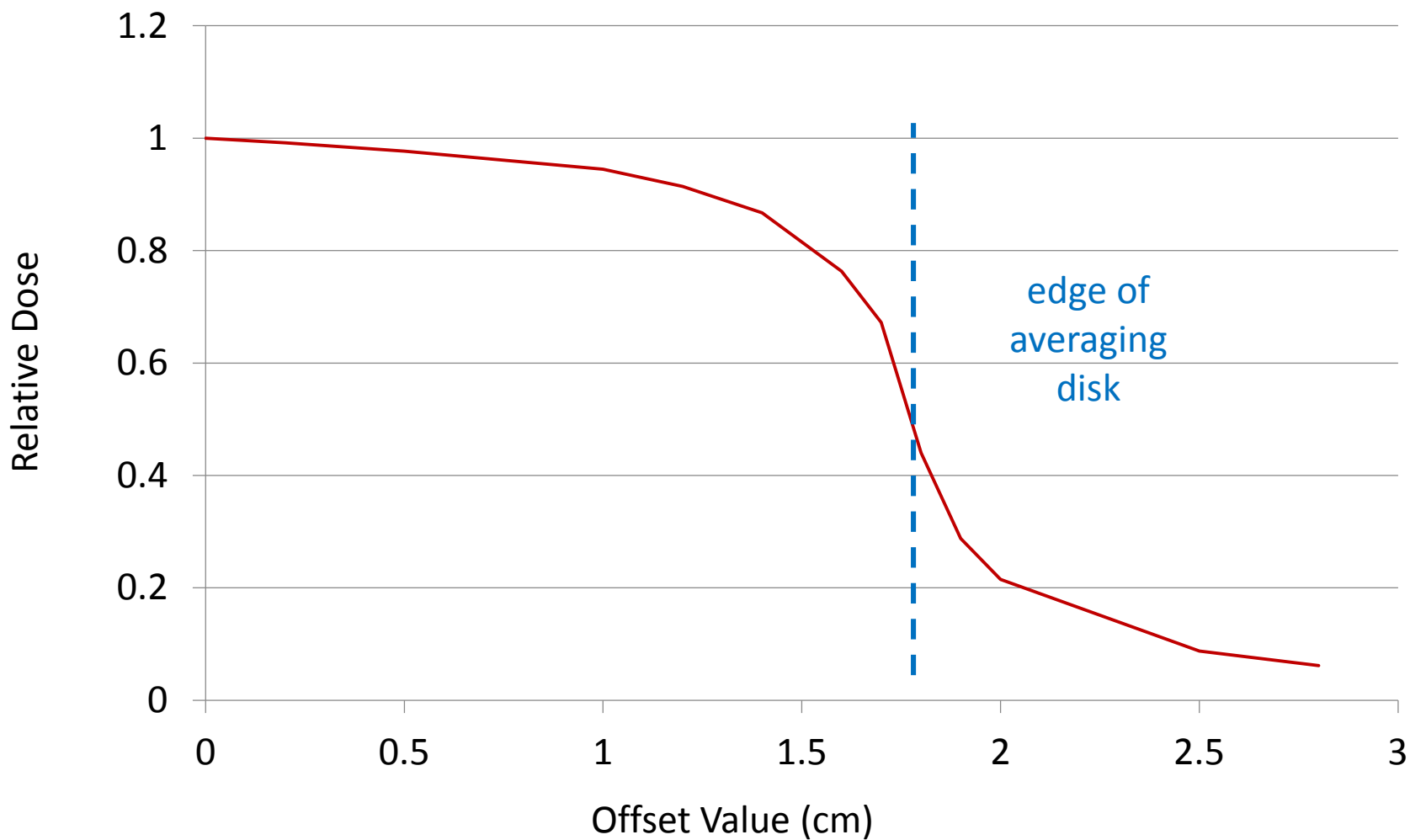
Offset-particle model



This feature allows for the calculation of photon dose from multiple hot particles to a single dose-averaging disk

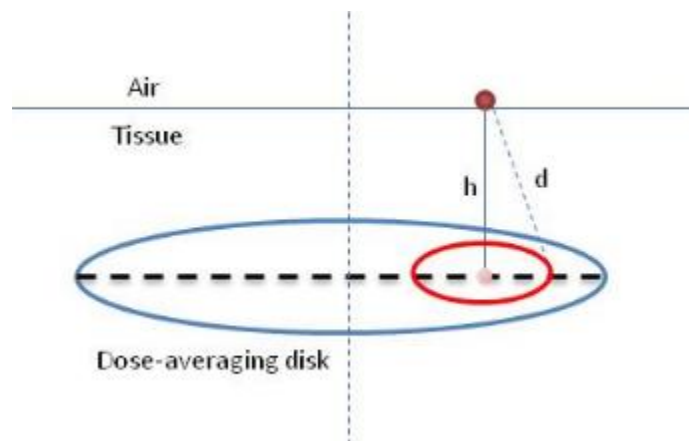
Offset Particle

^{60}Co ; point source; photon dosimetry only; 10 cm^2 ; 7 mg/cm^2



Dose Calculation for Offset Particles

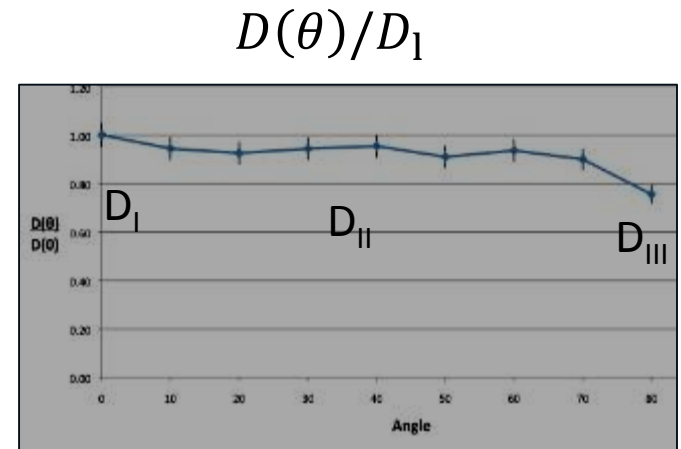
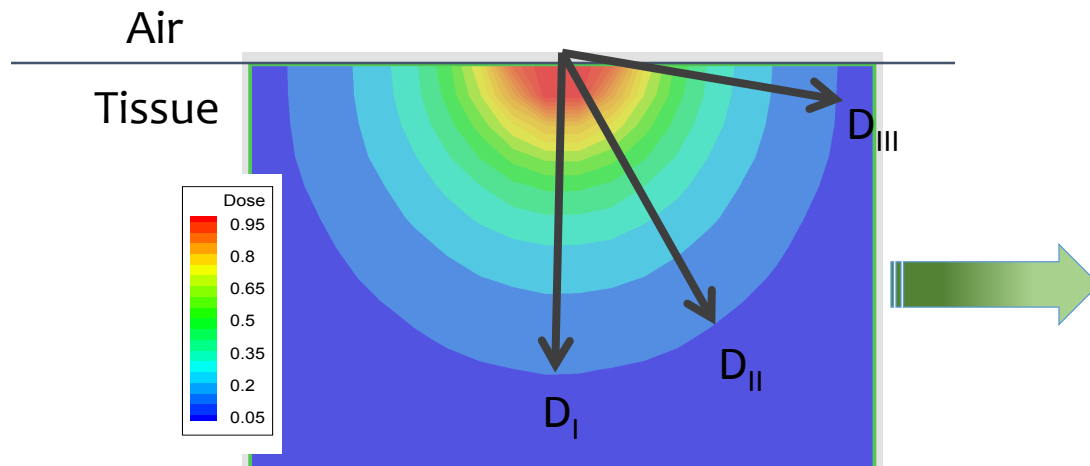
- Also, necessary for volumetric sources
 - essentially all of source volume will be offset
 - 15 x 15 x 15 source points
 - 300 dose points along the symmetric diameter
 - weighted by the fractional area of each annulus (red circle) that resides within the averaging disk



Offset (10 cm ²) r = 1.78 cm	Relative Dose Rate
0.0 cm	1.28
0.1	1.28
0.2	1.27
0.3	1.27
0.5	1.25
0.7	1.25
0.9	1.23
1.1	1.19
1.3	1.13
1.5	1.06
1.7	0.86
1.8	0.56
1.9	0.37

Off-Axis Correction

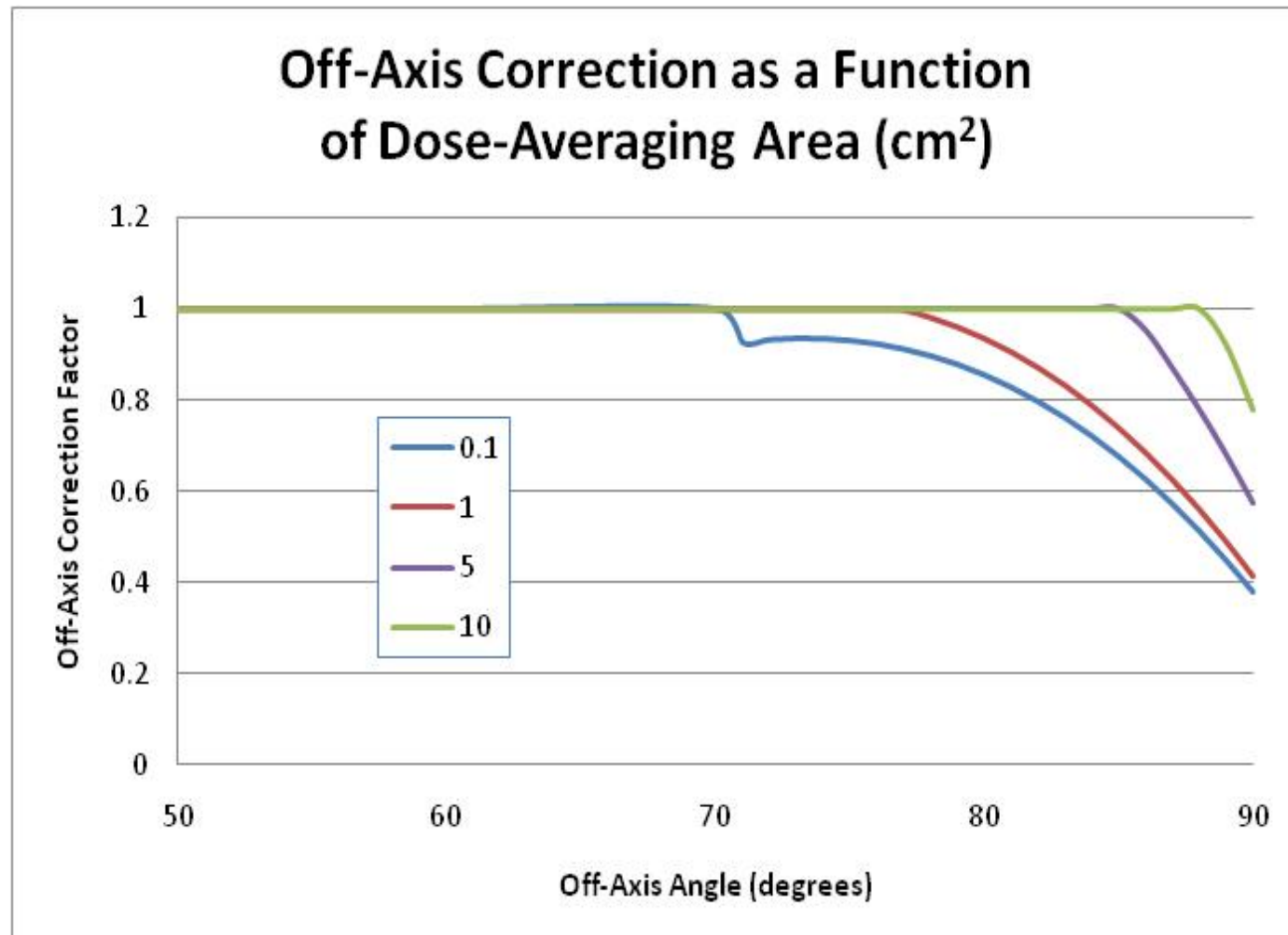
- CPE factors were determined at various depths on-axis in an infinite medium
 - thus, photon/electron loss at tissue-air interface is not considered
- Previous calculations assumed $D_I = D_{II} = D_{III}$
 - additional simulations performed to consider electron loss
- Ratio of off-axis dose to perpendicular dose at depth is plotted



$E = 662 \text{ keV}$

Off-Axis Correction Factors

Implemented for 4 Dose Averaging Areas



Elements of the dose calculation

- So, this leaves us with a point-kernel photon dosimetry model that contains these elements:

The diagram shows the equation for the dose rate $\dot{D}(d)$ in a point-kernel photon dosimetry model, with various components labeled and color-coded:

$$\dot{D}(d) = \left[E_0 \cdot \frac{S}{4\pi d^2} e^{-\mu d} \cdot \frac{\mu_{tr}}{\rho} \right] \cdot f_{cpe}(d, E) \cdot F_{oa}(\theta, E)$$

- Source Strength** (green arrow) points to S .
- Photon Energy** (red arrow) points to E_0 .
- Geometric Attenuation** (purple arrow) points to $\frac{1}{4\pi d^2}$.
- Material Attenuation** (red arrow) points to $e^{-\mu d}$.
- Energy Transfer Probability** (brown arrow) points to $\frac{\mu_{tr}}{\rho}$.
- Buildup Correction** (light blue arrow) points to $f_{cpe}(d, E)$.
- Off-Axis Correction** (blue arrow) points to $F_{oa}(\theta, E)$.

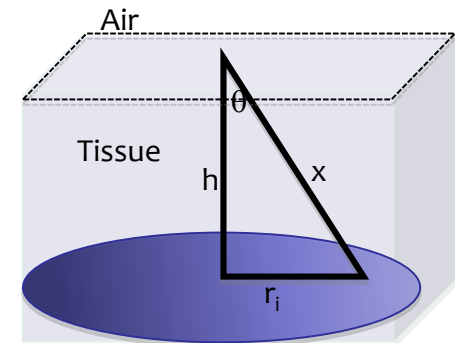
SUMMARIZING the Model

Effort to improve accuracy, simplify, and provide continuity

$$D_{disc}(h, A) = \frac{\int f_{CPE}(x) \cdot K(x) \cdot F_{oa} \cdot e^{-\mu\sqrt{h^2+r^2}} dA}{\int dA}$$

Model Components

- Attenuation Coefficient
 - improve accuracy
- Buildup Region – f_{cpe}
 - improve accuracy
 - simplify –function of E
- Off-Axis Factors – F_{oa}
 - analytical fit



Source Geometry

- ☐ Point ☒ Sphere
☐ Disk ☐ Slab
☐ Cylinder

Special Options

- ☐ Exclude Photon Dose
☐ Exclude Electron Dose
☐ Perform Volume Averaging
☐ Offset Particle Model

Skin Averaging Area

10 cm²

Exposure Time

60 min

Radionuclide Library [Zeff]

C-14 [7.42] 38
Ce-144 [7.42] 107
Ce-144 [7.42] 107D
Ce-144 [7.42] 38
Ce-144 [7.42] 38D
Co-60 [25.5] 38
Pr-144 [7.42] 107
Pr-144 [7.42] 38
Pr-144m [7.42] 38
Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

Selected Radionuclides

Edit

Remove

Remove All

Point Source Irradiation Geometry

Skin Thickness or Skin
Density Thickness: 7 mg/cm²

Air Gap Thickness 0 mm

Cover Thickness 0 mm

Cover Density 0 g/cm³

Multiple Cover Calculator

VARSKIN

Calculate Doses

Source Geometry

- ☐ Point ☒ Sphere
☐ Disk ☐ Slab
☐ Cylinder

Special Options

- ☐ Exclude Photon Dose
☐ Exclude Electron Dose
☐ Perform Volume Averaging
☐ Offset Particle Model

Skin Averaging Area

10 cm²

Exposure Time

60 min

Radionuclide Library [Zeff]

C-14 [7.42] 38
Ce-144 [7.42] 107
Ce-144 [7.42] 107D
Ce-144 [7.42] 38
Ce-144 [7.42] 38D
Co-60 [25.5] 38
Pr-144 [7.42] 107
Pr-144 [7.42] 38
Pr-144m [7.42] 38
Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

Selected Radionuclides

Edit

Remove

Remove All

Point Source Irradiation Geometry

Skin Thickness or Skin Density Thickness: 7 mg/cm²

Air Gap Thickness 0 mm

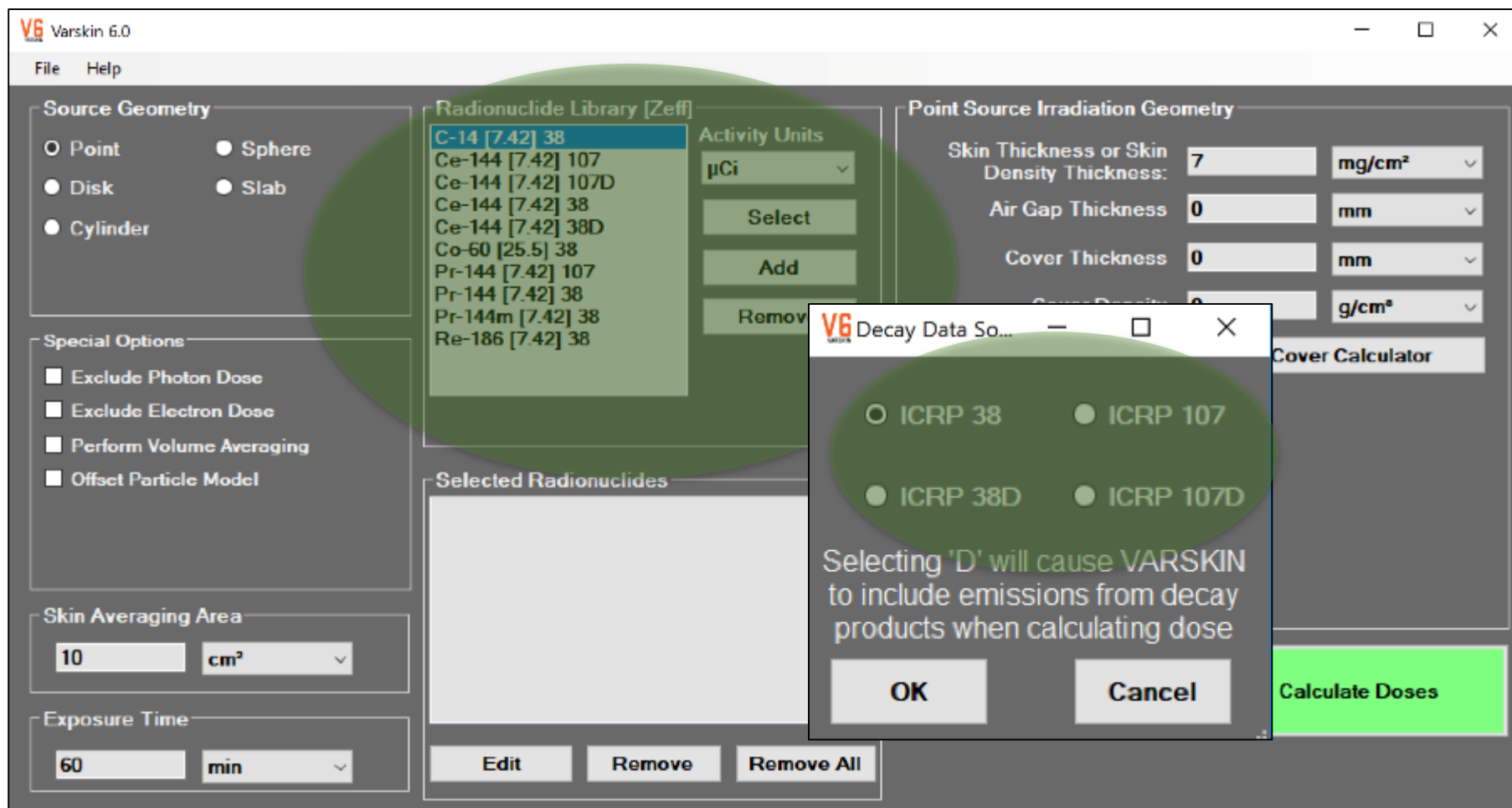
Cover Thickness 0 mm

Cover Density 0 g/cm³

Multiple Cover Calculator

VARSKIN

Calculate Doses



Radionuclides Available to Add

Ac-223	Ag-108	Am-240	As-69	At-217	Ba-128	Bi-200	Bi-214
Ac-224	Ag-108m	Am-241	As-70	At-218	Ba-131	Bi-201	Bk-245
Ac-225	Ag-109m	Am-242	As-71	Au-193	Ba-131m	Bi-202	Bk-246
Ac-226	Ag-110	Am-242m	As-72	Au-194	Ba-133	Bi-203	Bk-247
Ac-227	Ag-110m	Am-243	As-73	Au-195	Ba-133m	Bi-204	Bk-249
Ac-228	Ag-111	Am-244	As-74	Au-195m	Ba-135m	Bi-205	Bk-250
Ag-102	Ag-112	Am-244m	As-76	Au-198	Ba-137m	Bi-206	Br-74
Ag-103	Ag-115	Am-245	As-77	Au-198m	Ba-139	Bi-207	Br-74m
Ag-104	Al-26	Am-246	As-78	Au-199	Ba-140	Bi-210	Br-75
Ag-104m	Al-28	Am-246m	At-207	Au-200	Ba-141	Bi-210m	Br-76
Ag-105	Am-237	Ar-37	At-211	Au-200m	Ba-142	Bi-211	Br-77
Ag-106	Am-238	Ar-39	At-215	Au-201	Be-10	Bi-212	Br-80
Ag-106m	Am-239	Ar-41	At-216	Ba-126	Be-7	Bi-213	Br-80m

<

>

Atomic Number of
Source Material (Z)

7.42

Add
Radionuclide

Cancel

Radionuclides Available to Add

Cd-115	Ce-135	Cf-250	Cm-239	Co-54m	Cr-51	Cs-130m	Cu-57
Cd-115m	Ce-137	Cf-251	Cm-240	Co-55	Cr-55	Cs-131	Cu-59
Cd-117	Ce-137m	Cf-252	Cm-241	Co-56	Cr-56	Cs-132	Cu-60
Cd-117m	Ce-139	Cf-253	Cm-242	Co-57	Cs-121	Cs-134	Cu-61
Cd-118	Ce-141	Cf-254	Cm-243	Co-58	Cs-121m	Cs-134m	Cu-62
Cd-119	Ce-143	Cf-255	Cm-244	Co-58m	Cs-123	Cs-135	Cu-64
Cd-119m	Ce-144	Cl-34	Cm-245	Co-60	Cs-124	Cs-135m	Cu-66
Ce-130	Ce-145	Cl-34m	Cm-246	Co-60m	Cs-125	Cs-136	Cu-67
Ce-131	Cf-244	Cl-36	Cm-247	Co-61	Cs-126	Cs-137	Cu-69
Ce-132	Cf-246	Cl-38	Cm-248	Co-62	Cs-127	Cs-138	Dy-148
Ce-133	Cf-247	Cl-39	Cm-249	Co-62m	Cs-128	Cs-138m	Dy-149
Ce-133m	Cf-248	Cl-40	Cm-250	Cr-48	Cs-129	Cs-139	Dy-150
Ce-134	Cf-249	Cm-238	Cm-251	Cr-49	Cs-130	Cs-140	Dy-151

<

>

Calculating for Cs-137...

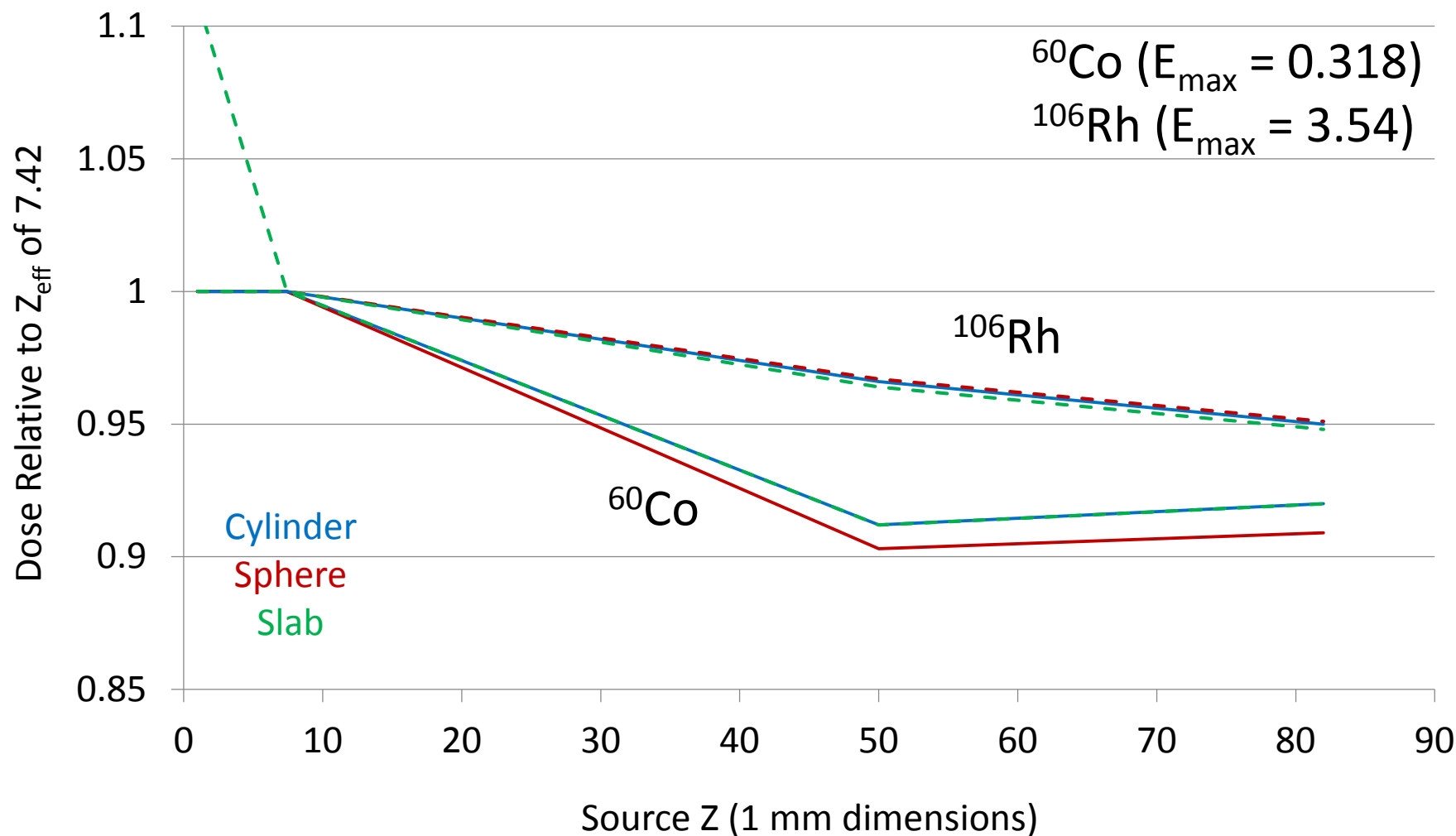
Atomic Number of
Source Material (Z)

Add
Radionuclide

7.42

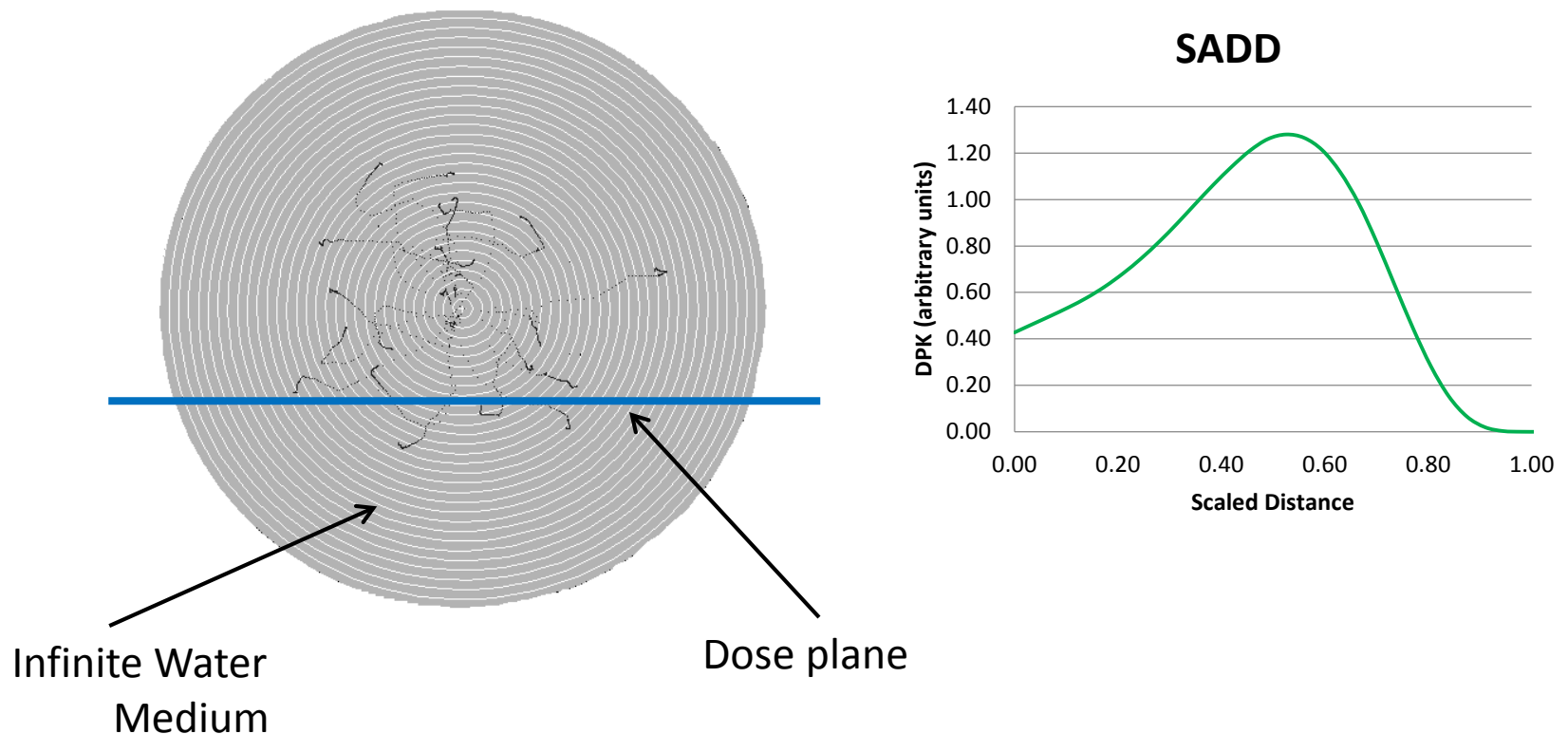
Why do I need the source atomic number?

Volumetric Beta Dose vs Source Z



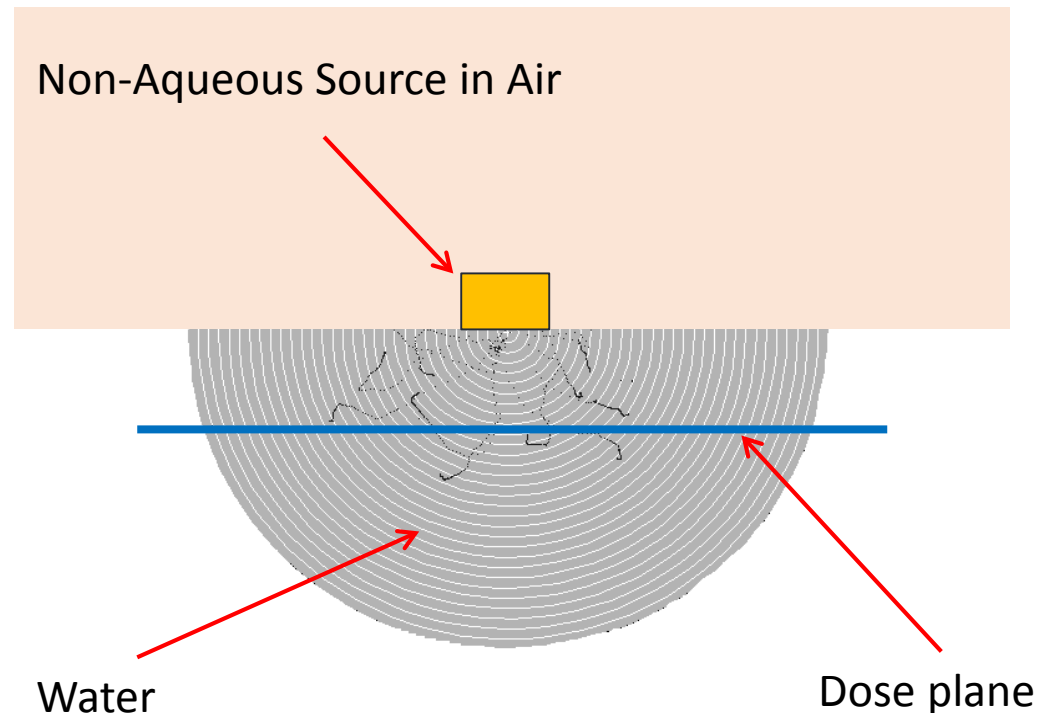
Corrections to Dose-Point Kernel

- Spatial distribution of energy absorption from electron emission sources is the basic physical information required for electron dosimetry



Corrections to Dose-Point Kernels

- Develop an electron energy-absorption scaling model for source materials with $7.42 < Z \leq 94$
- Develop a volumetric backscatter model for typical hot particle geometries
 - to predict dose perturbations due to both source and atmospheric backscattering

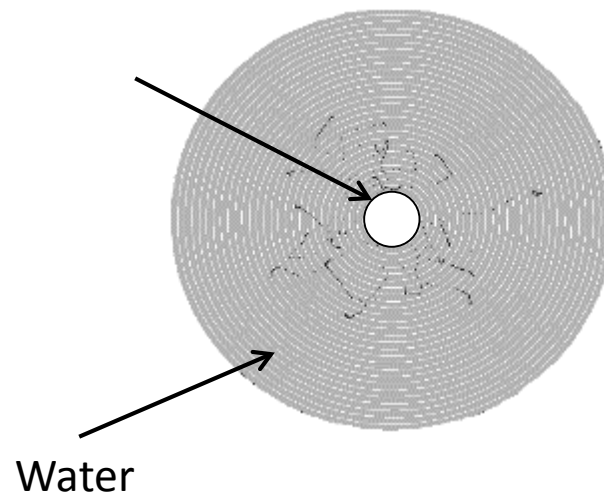


the handling of
kinetic energy loss (SADD)

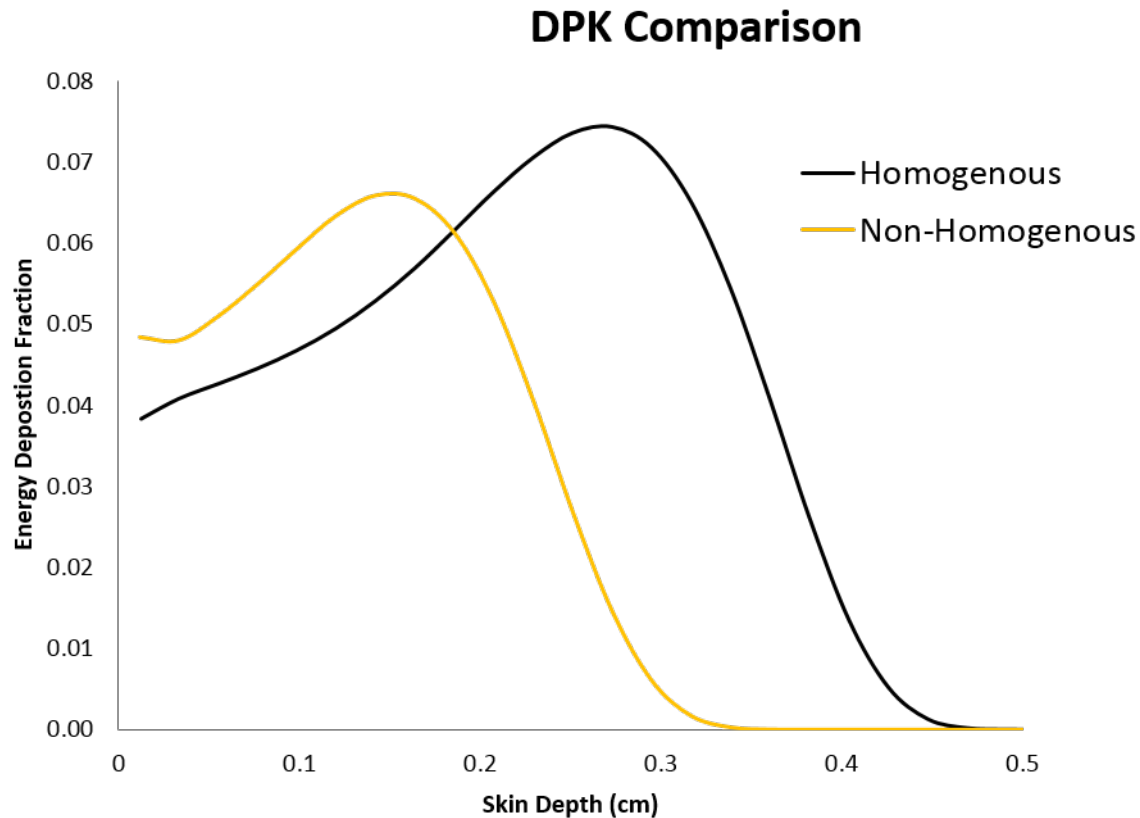
Methods: Scaling Model

- Using EGSnrc Monte Carlo simulations:
 - Homogeneous point-source DPK's for water at $0.01 \text{ MeV} \leq E \leq 8 \text{ MeV}$ (30 energies)
 - Non-homogeneous point-source DPK's for $7.42 < Z \leq 94$ (18 solid elements) at $0.01 \text{ MeV} \leq E \leq 8 \text{ MeV}$
 - water absorption sphere
 - radii varied between 5% to 110% of the X_{90} value

Absorption Sphere

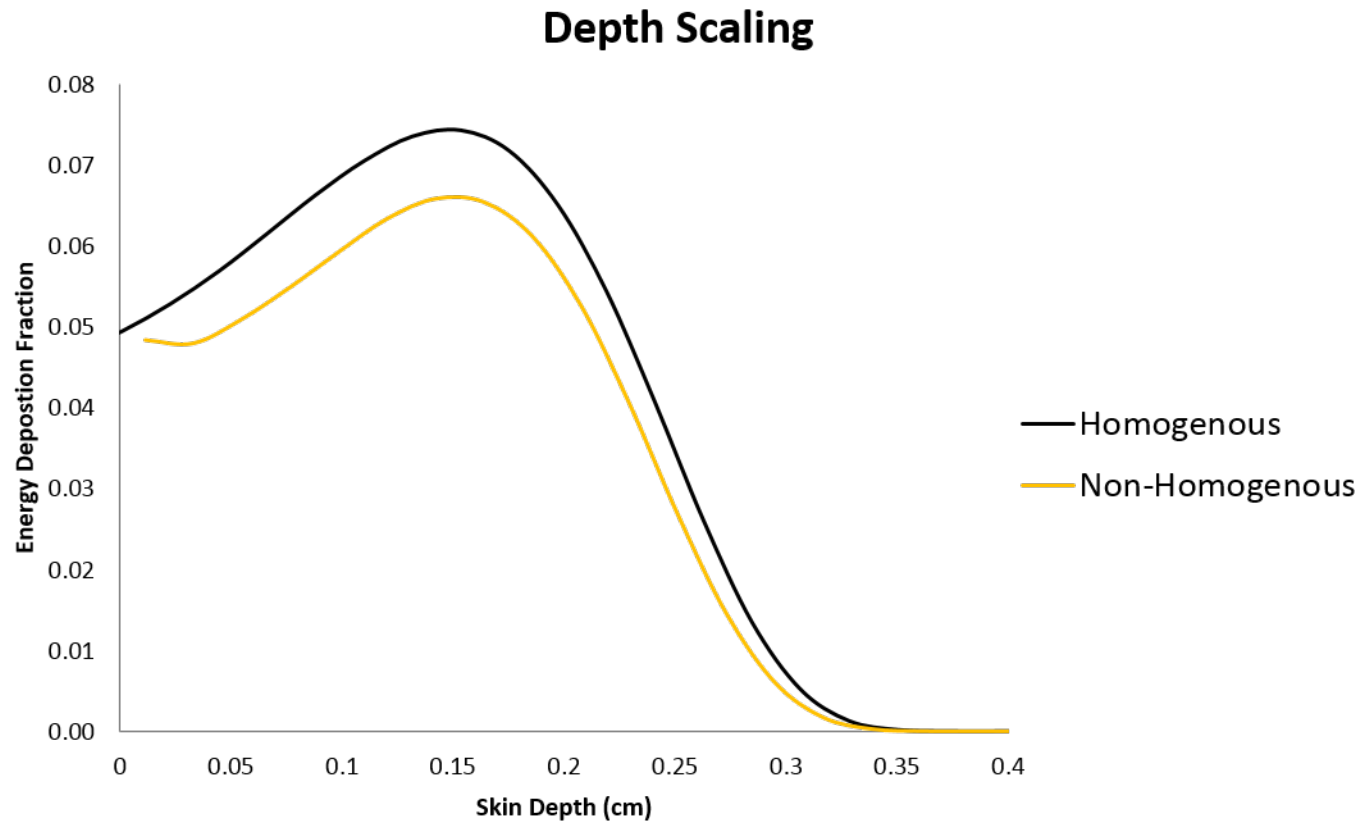


Scaling Model



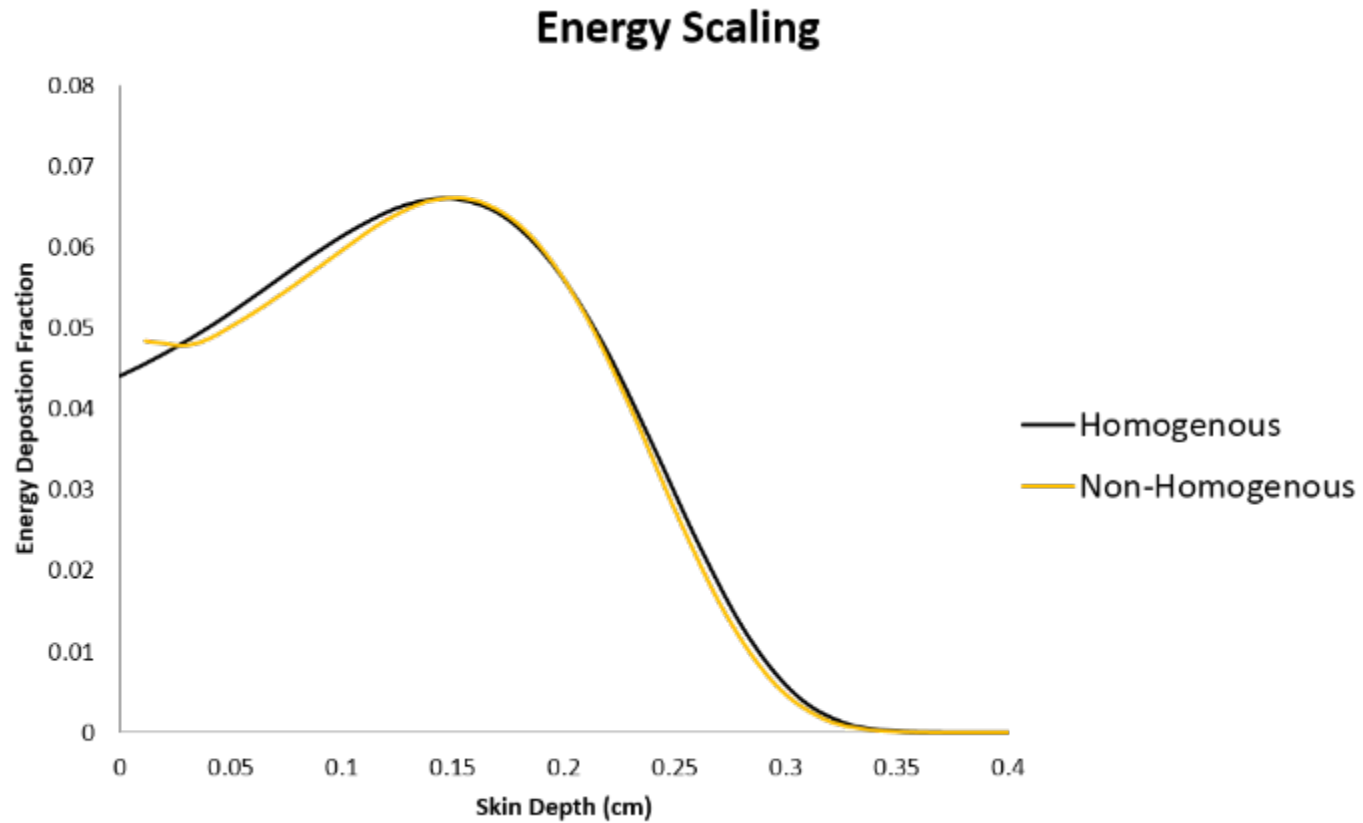
- 1 MeV electron DPK's for the case of a homogenous medium (water) and the case of a non-homogeneous medium (for example, air over the skin with a source material of iron)

Scaling Model



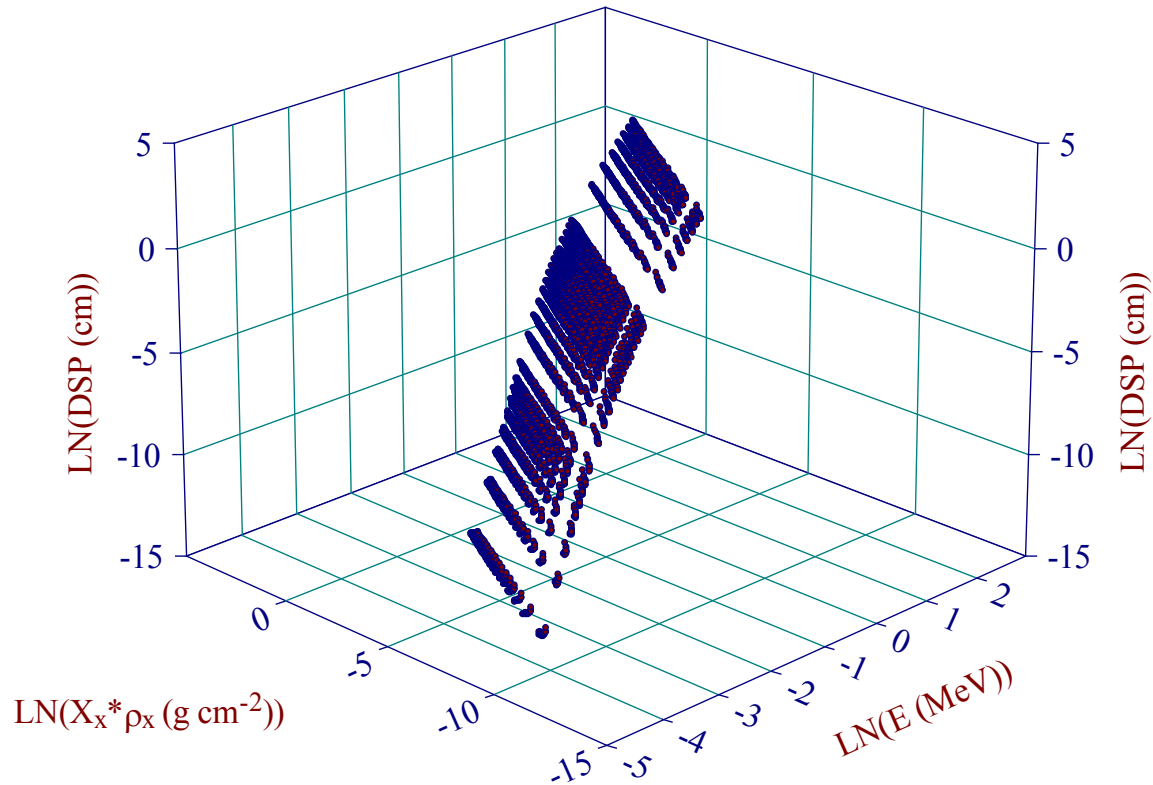
- 1 MeV electron DPK's for the case of a homogenous medium (water) and the case of a non-homogeneous medium (for example, air over the skin with a source material of iron)

Scaling Model



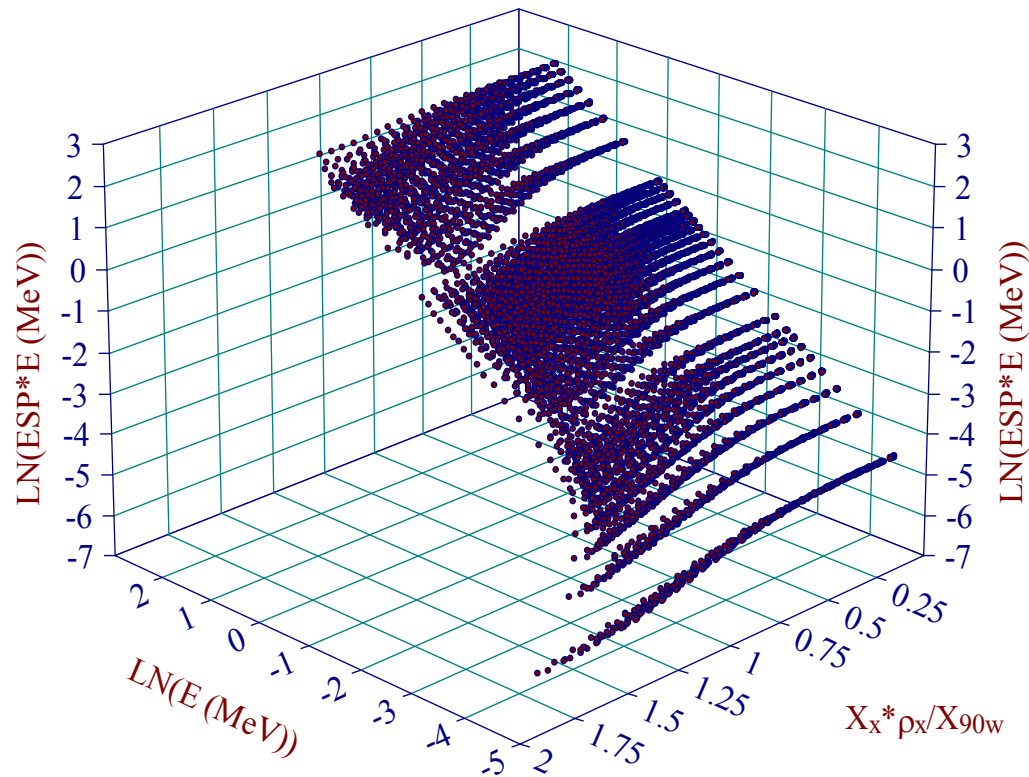
Scaling Results

Depth Scaling for All Materials



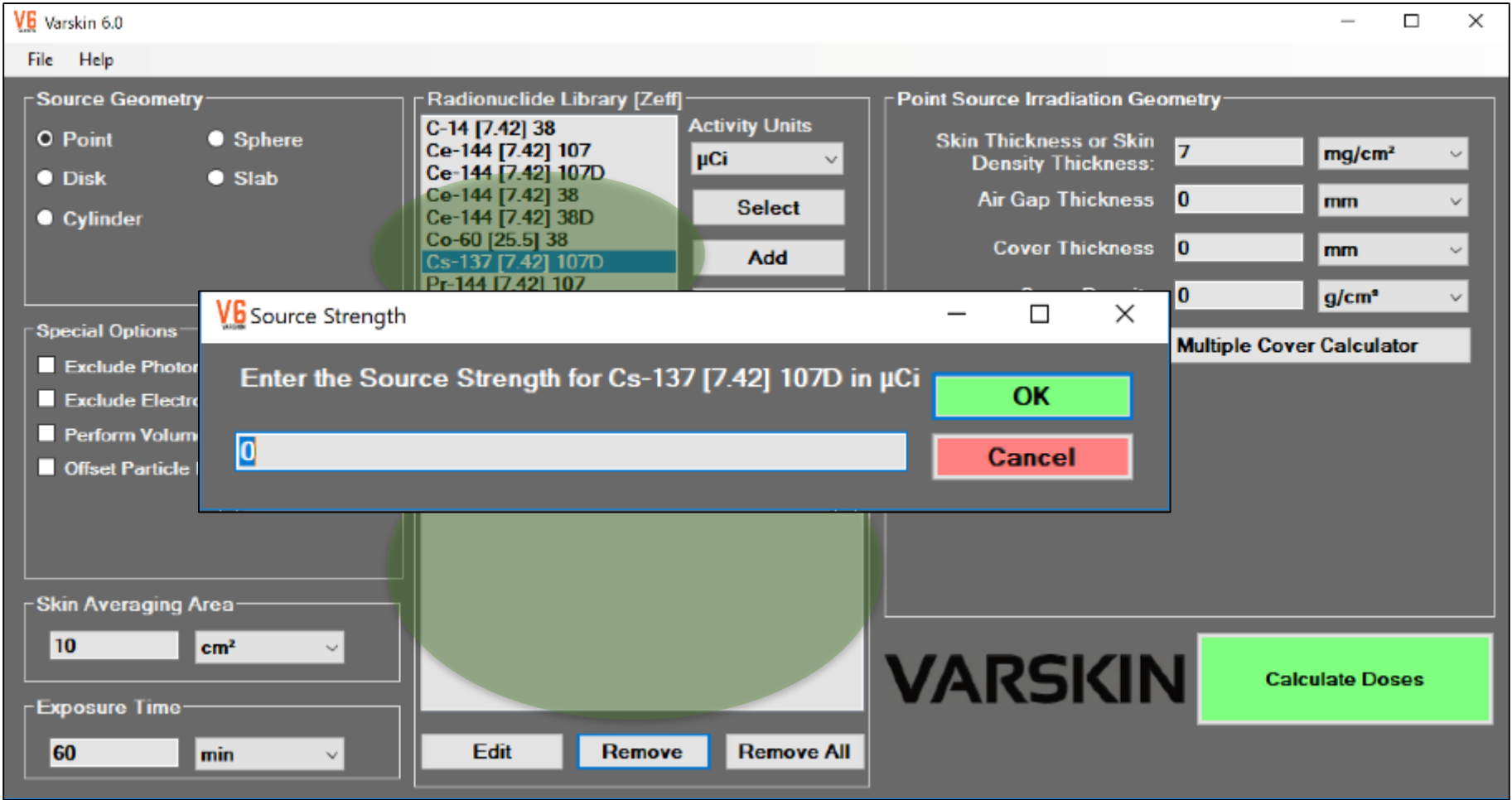
Scaling Results

Energy Scaling for All Materials



Radionuclide Library

- Current database taken from ICRP 38
- Contains > 800 radionuclides
- Parent/daughter relationships **NOT** incorporated
- Emissions include:
 - photons (gamma; X-ray; annihilation)
 - electrons (beta; positron; conversion; Auger)
- Source atomic number (Z) affects electron energy loss prior to skin entry



Source Geometry

- ☐ Point ☒ Sphere
☐ Disk ☐ Slab
☐ Cylinder

Special Options

- ☐ Exclude Photon Dose
☐ Exclude Electron Dose
☐ Perform Volume Averaging
☐ Offset Particle Model

Skin Averaging Area

10 cm²

Exposure Time

60 min

Radionuclide Library [Zeff]

C-14 [7.42] 38
Ce-144 [7.42] 107
Ce-144 [7.42] 107D
Ce-144 [7.42] 38
Ce-144 [7.42] 38D
Co-60 [25.5] 38
Cs-137 [7.42] 107D
Pr-144 [7.42] 107
Pr-144 [7.42] 38
Pr-144m [7.42] 38
Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

Selected Radionuclides

Cs-137 [7.42] 107D: 1.00E+00 μCi

Edit

Remove

Remove All

Point Source Irradiation Geometry

Skin Thickness or Skin Density Thickness: 7 mg/cm²

Air Gap Thickness 0 mm

Cover Thickness 0 mm

Cover Density 0 g/cm³

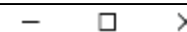
Multiple Cover Calculator

VARSKIN

Calculate Doses



Varskin 6.0



File Help

Source Geometry

- ☒ Point ☐ Sphere
☐ Disk ☐ Slab
☐ Cylinder

Special Options

- ☐ Exclude Photon Dose
☐ Exclude Electron Dose
☐ Perform Volume Averaging

Skin Averaging Area

10 cm²

Exposure Time

60 min

Radionuclide Library [Zeff]

C-14 [7.42] 38
Ce-144 [7.42] 107
Ce-144 [7.42] 107D
Ce-144 [7.42] 38
Ce-144 [7.42] 38D
Co-60 [25.5] 38
Cs-137 [7.42] 107D
Pr-144 [7.42] 107
Pr-144 [7.42] 38
Pr-144m [7.42] 38
Re-186 [7.42] 38

Activity Units

 $\mu\text{Ci}/\text{cm}^2$

Select

Add

Remove

☒ Use Distributed Source

Selected Radionuclides

Cs-137 [7.42] 107D: 1.00E+00 $\mu\text{Ci}/\text{cm}^2$

Edit

Remove

Remove All

Disk Source Irradiation Geometry

Skin Thickness or Skin Density Thickness: 7 mg/cm²

Air Gap Thickness 0 mm

Cover Thickness 0 mm

Cover Density 0 g/cm³

Multiple Cover Calculator

Source Area 0.785 mm²

Source Diameter 1 mm

VARSKIN

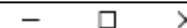
Calculate Doses

Distributed Source

- For all geometries except point
- The selected radionuclide is always distributed throughout the source area or volume
- This option simply gives the user the ability to enter the volumetric equivalent of activity, as opposed to total activity
- On selection:
 - source units change from activity to activity per unit area ($\mu\text{Ci}/\text{cm}^2$) or volume ($\mu\text{Ci}/\text{cm}^3$)
 - user must remove and re-select radionuclide(s)



Varskin 6.0



File Help

Source Geometry

- ☐ Point ☐ Sphere
☐ Disk ☐ Slab
☐ Cylinder

Special Options

- ☐ Exclude Photon Dose
☐ Exclude Electron Dose
☐ Perform Volume Averaging

Skin Averaging Area

10 cm²

Exposure Time

60 min

Radionuclide Library [Zeff]

C-14 [7.42] 38
Ce-144 [7.42] 107
Ce-144 [7.42] 107D
Ce-144 [7.42] 38
Ce-144 [7.42] 38D
Co-60 [25.5] 38
Cs-137 [7.42] 107D
Pr-144 [7.42] 107
Pr-144 [7.42] 38
Pr-144m [7.42] 38
Re-186 [7.42] 38

Activity Units

μCi/cm²

Select

Add

Remove

☒ Use Distributed Source

Selected Radionuclides

Cs-137 [7.42] 107D: 1.00E+00 μCi/cm²

Edit

Remove

Remove All

Disk Source Irradiation Geometry

Skin Thickness or Skin Density Thickness: 7 mg/cm²

Air Gap Thickness 0 mm

Cover Thickness 0 mm

Cover Density 0 g/cm³

Multiple Cover Calculator

Source Area 0.785 mm²

Source Diameter 1 mm

VARSKIN

Calculate Doses

Multiple Cover Calculator

- For each cover material, user enters two of:
 - density (g/cm^3)
 - thickness (mm)
 - density thickness (mg/cm^2)
- Then, total thickness and effective density are used as inputs describing the total cover:

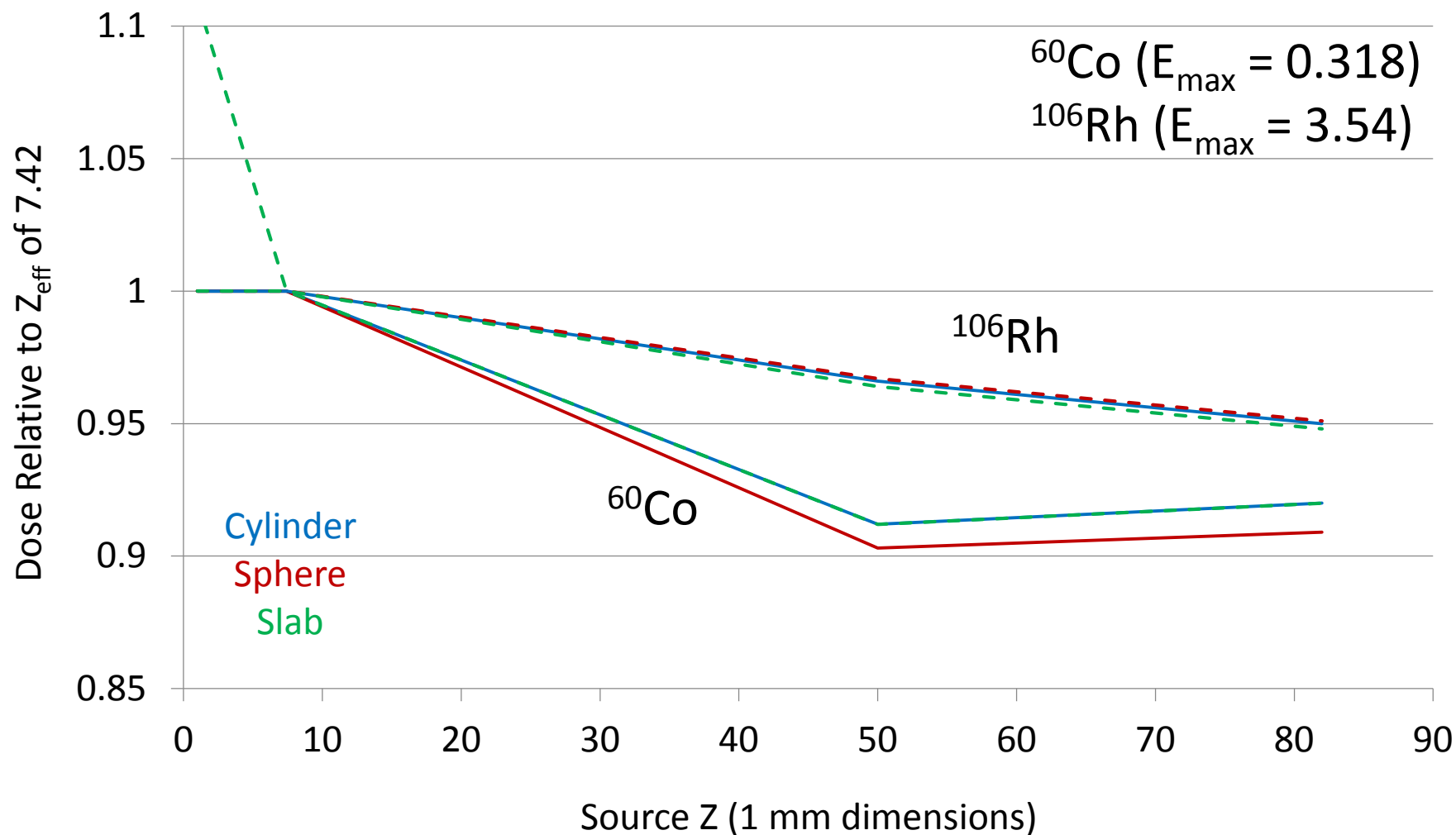
$$\rho_{eff} \left(\frac{\text{g}}{\text{cm}^3} \right) = \frac{\sum \rho x \left(\frac{\text{g}}{\text{cm}^2} \right)}{\sum x (\text{cm})}$$

	Density		Thickness		Density Thickness	
Cover 1	1.50E+00	g/cm ³ ▾	0.002	cm ▾		mg/cm ² ▾
Cover 2	4	g/cm ³ ▾	0.05	cm ▾		mg/cm ² ▾
Cover 3		g/cm ³ ▾		mm ▾		mg/cm ² ▾
Cover 4		g/cm ³ ▾		mm ▾		mg/cm ² ▾
Cover 5		g/cm ³ ▾		mm ▾		mg/cm ² ▾
Total	3.90E+00	g/cm ³ ▾	5.20E-02	cm ▾	2.03E-01	g/cm ² ▾

Calculate

Cancel

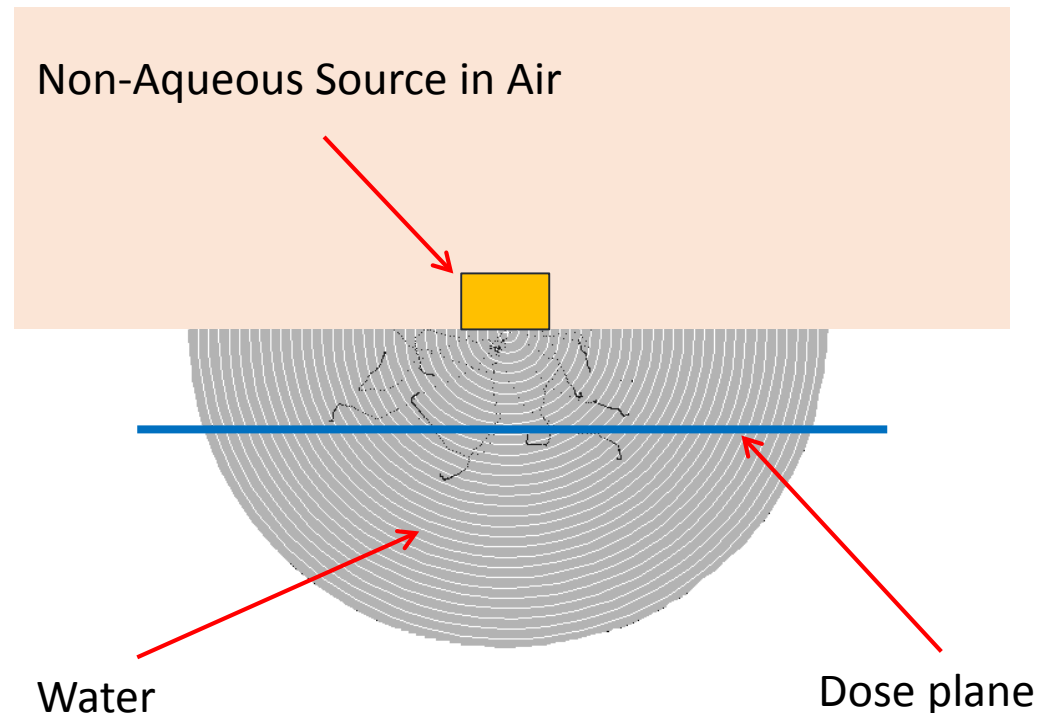
Volumetric Beta Dose vs Source Z



Why would dose increase as Z increases >50 ?

Corrections to Dose-Point Kernels

- Develop an electron energy-absorption scaling model for source materials with $7.42 < Z \leq 94$
- Develop a volumetric backscatter model for typical hot particle geometries
 - to predict dose perturbations due to both source and atmospheric backscattering

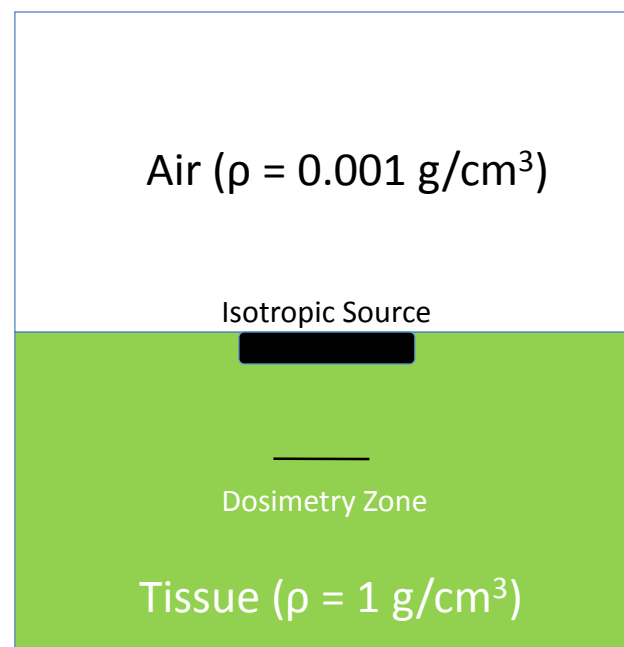
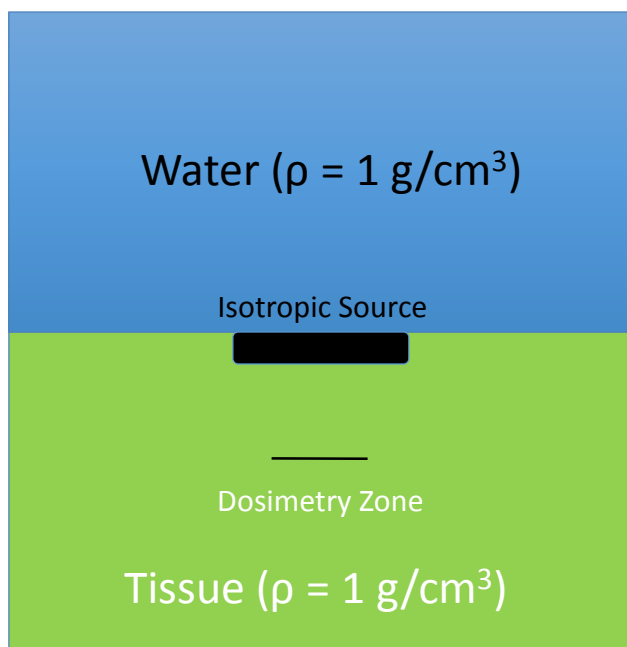


backscatter correction

Backscatter Correction

- Cross (1991b, 1992c) developed atmospheric point-source factors
- Source material point-source factors for medical physics by Buffa (2004), Cho (1999), and Lee (2004)
- Durham (2006) developed backscatter factors for volumetric sources with dimensions $<$ beta-particle range
 - accounts only for atmospheric scattering above the source

Original Backscatter Determination

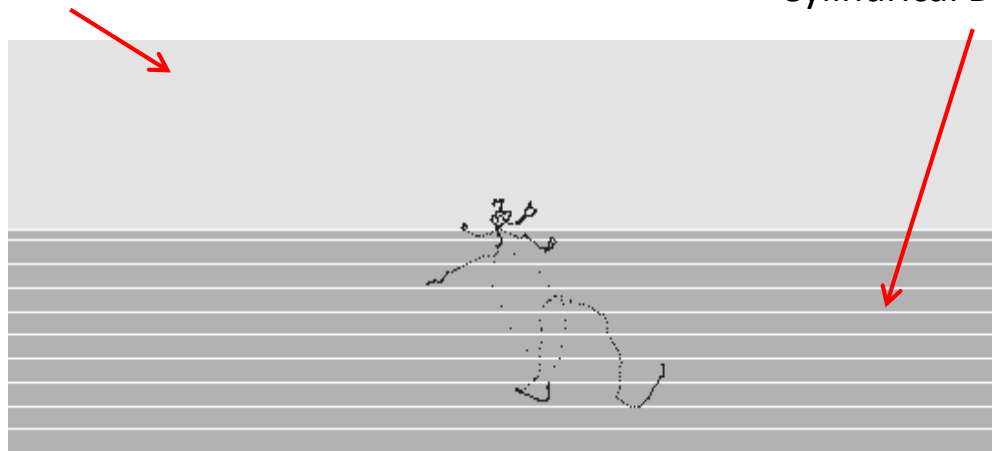


New Backscatter Model

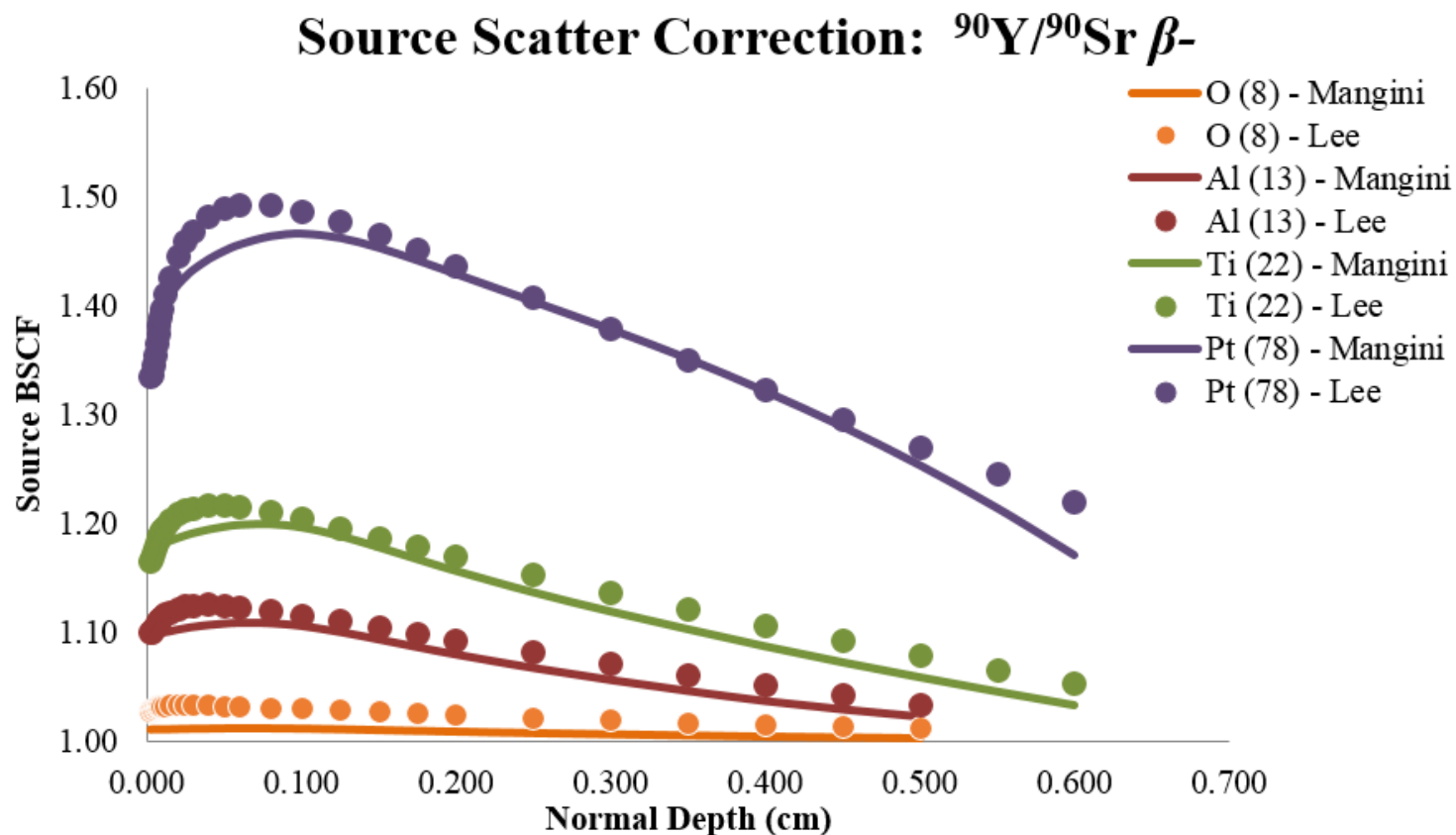
- Point-source planar dose profiles for water, air, and $7.42 < Z \leq 94$ scattering media at $0.01 \text{ MeV} \leq E \leq 8 \text{ MeV}$ using EGSnrc Monte Carlo simulations
- Dose averaging areas of 1 and 10 cm^2
- Normal depths every 1 mg cm^{-2} (up to 1000 mg cm^{-2})

Scattering Medium (“infinite” thickness)

Cylindrical Dose Planes

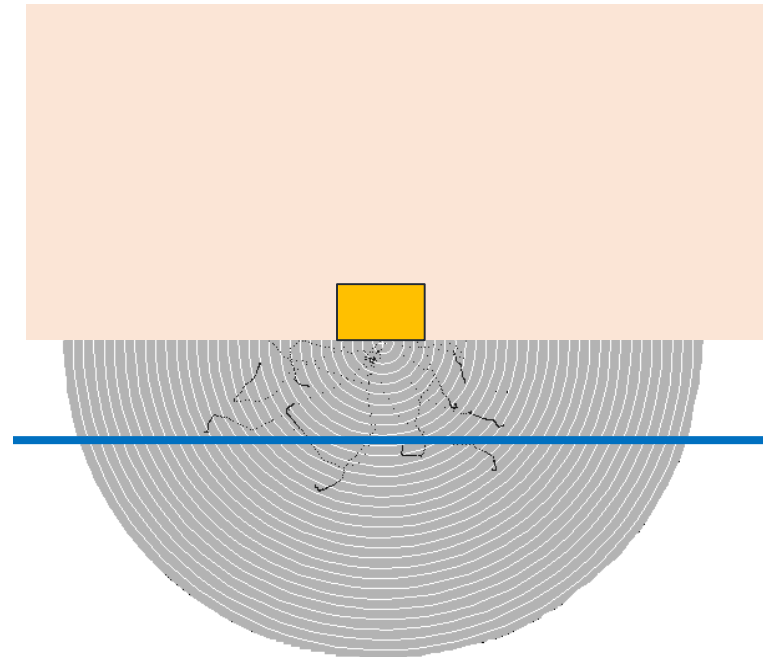


Point-Source BSCF

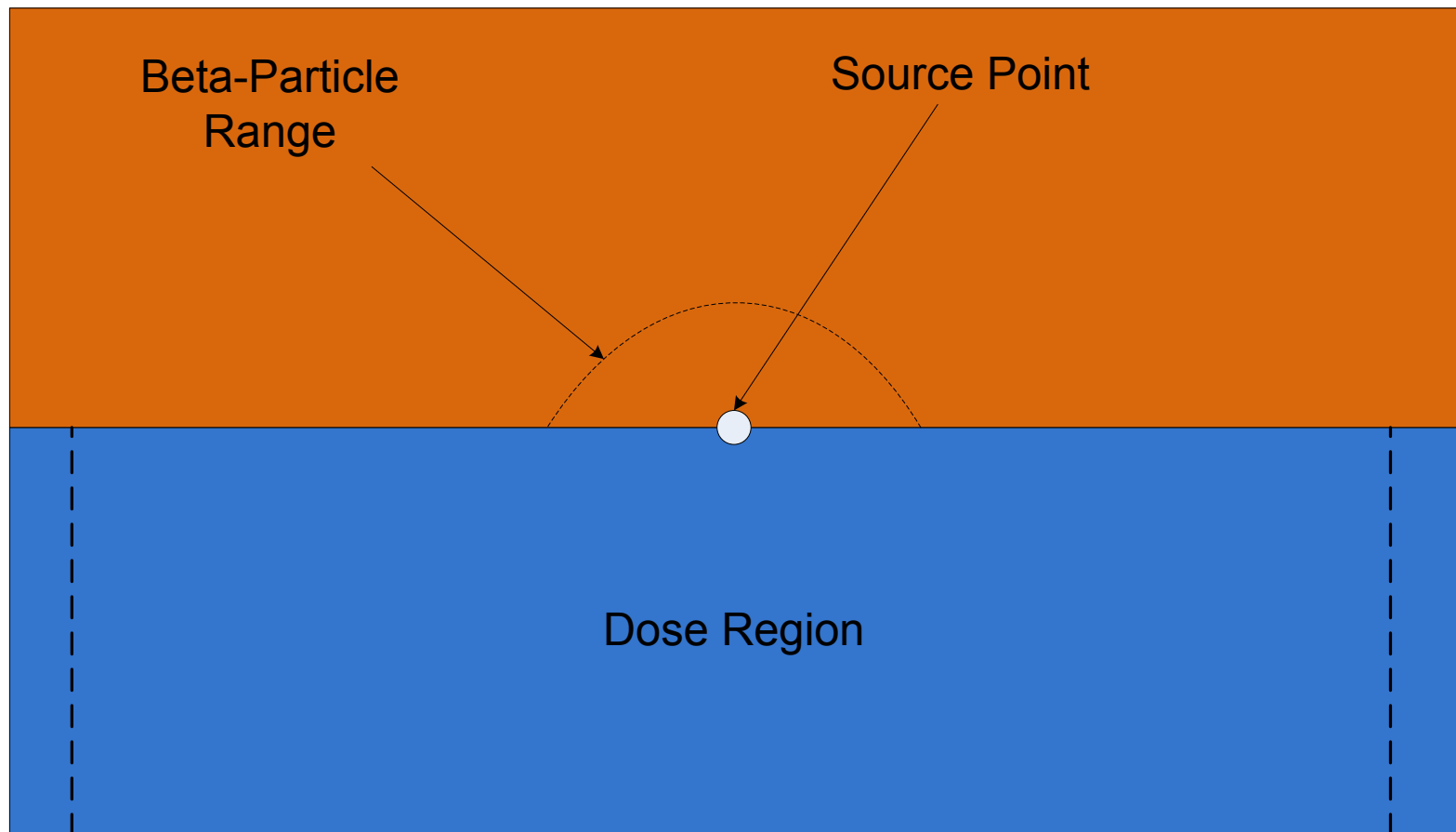


Scatter Scenarios

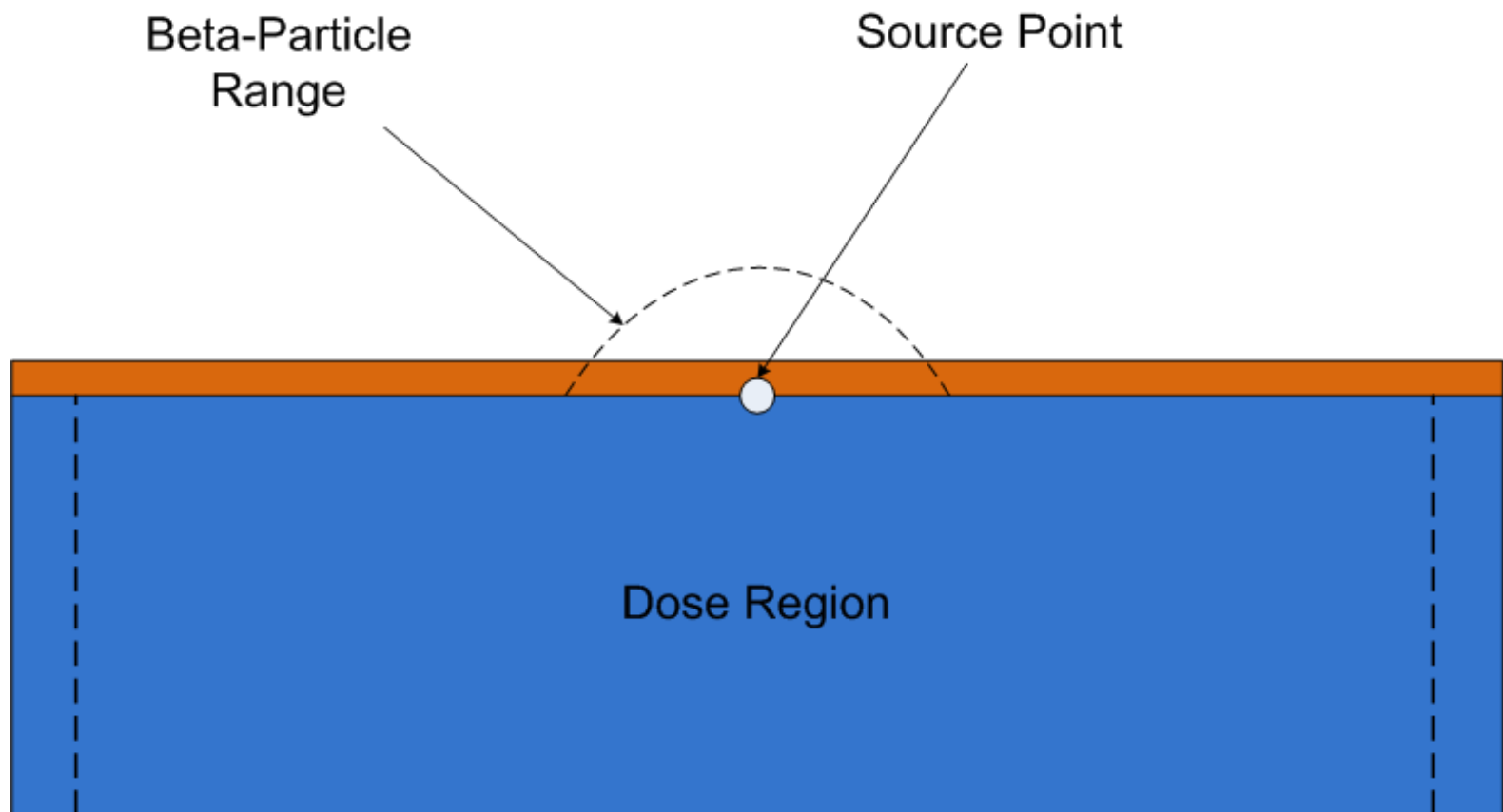
- Source scatter for top/bottom of source
- Source scatter for sides of source
- Air scatter for top/sides of source



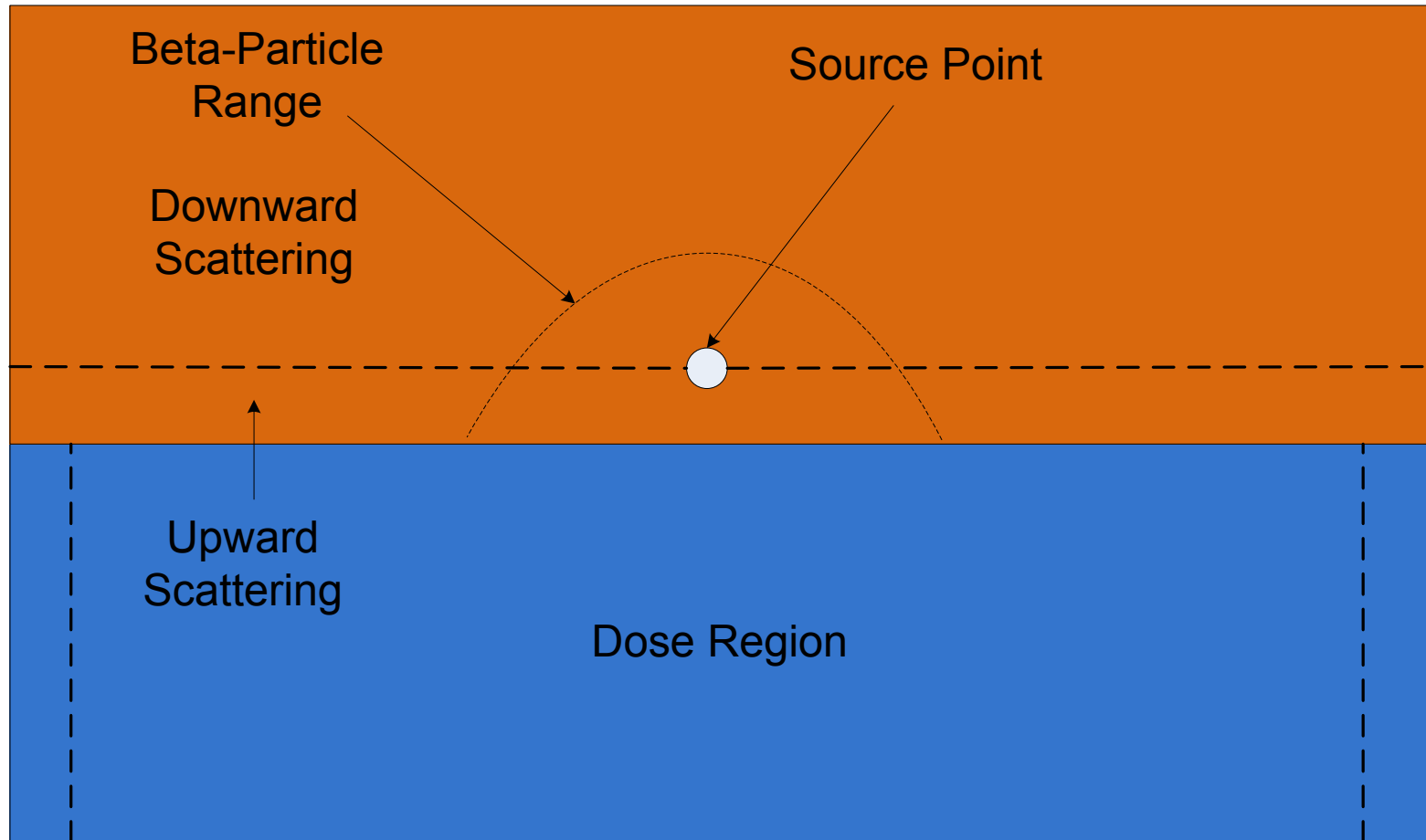
Scatter for Top/Bottom of Source



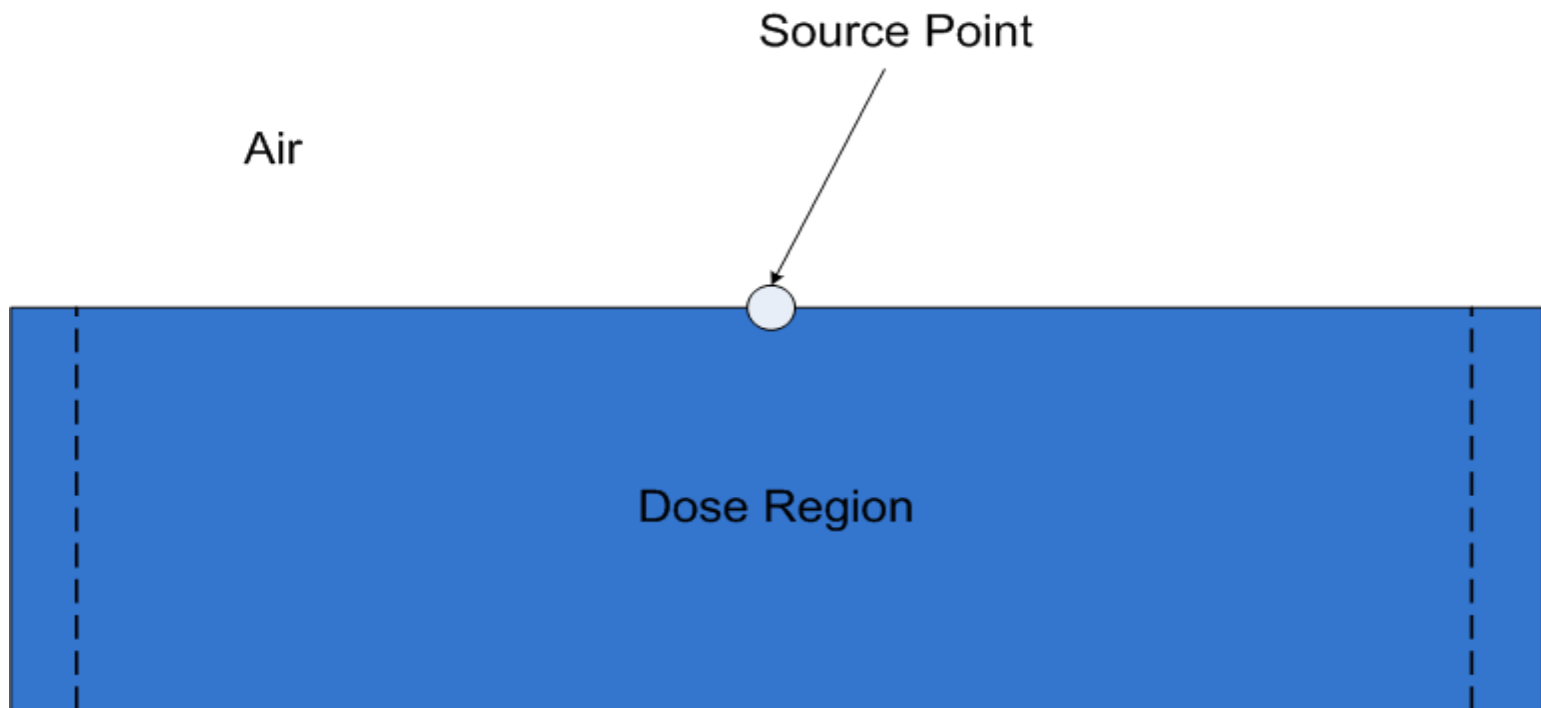
Scatter for Top/Bottom of Source



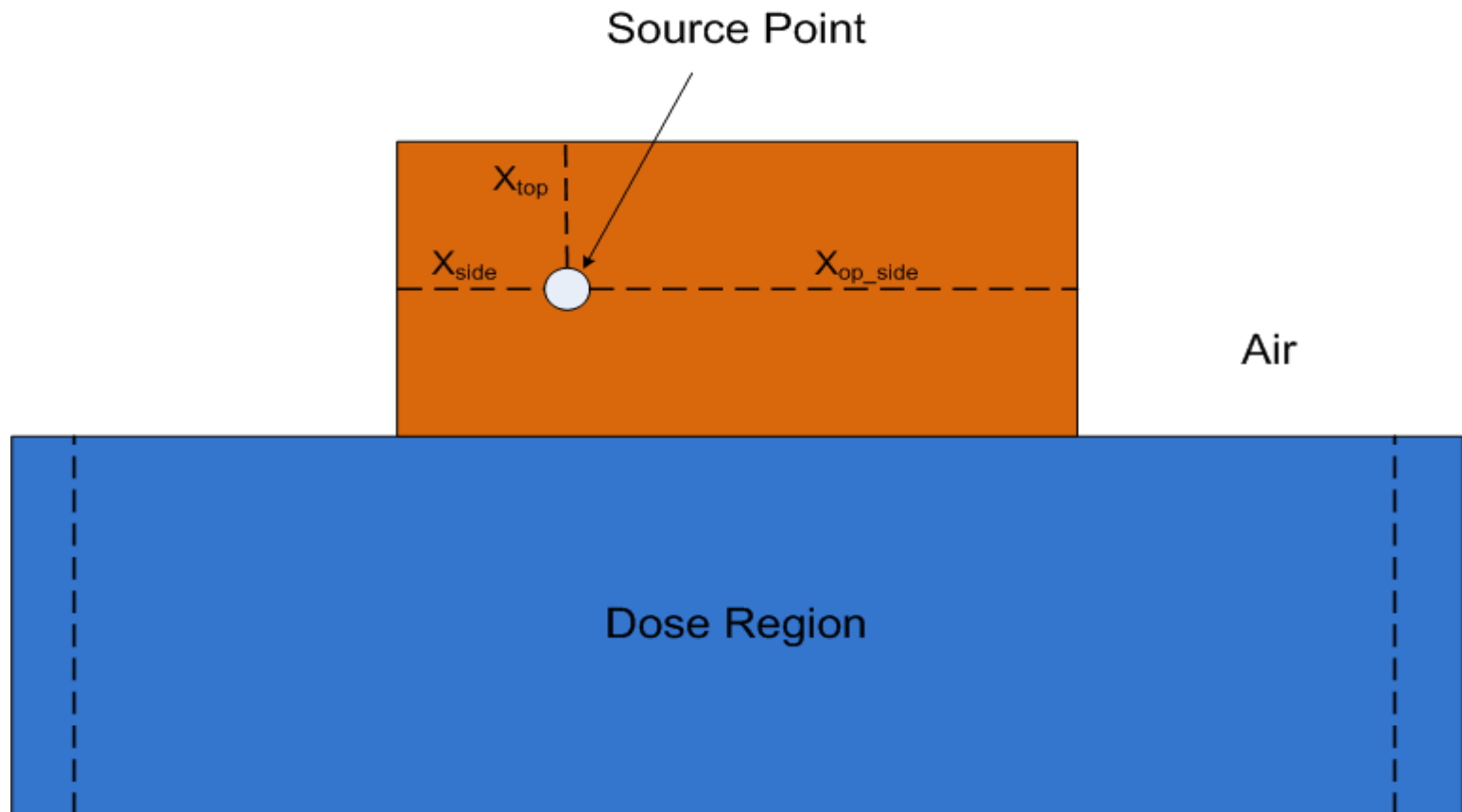
Scatter for Top/Bottom of Source



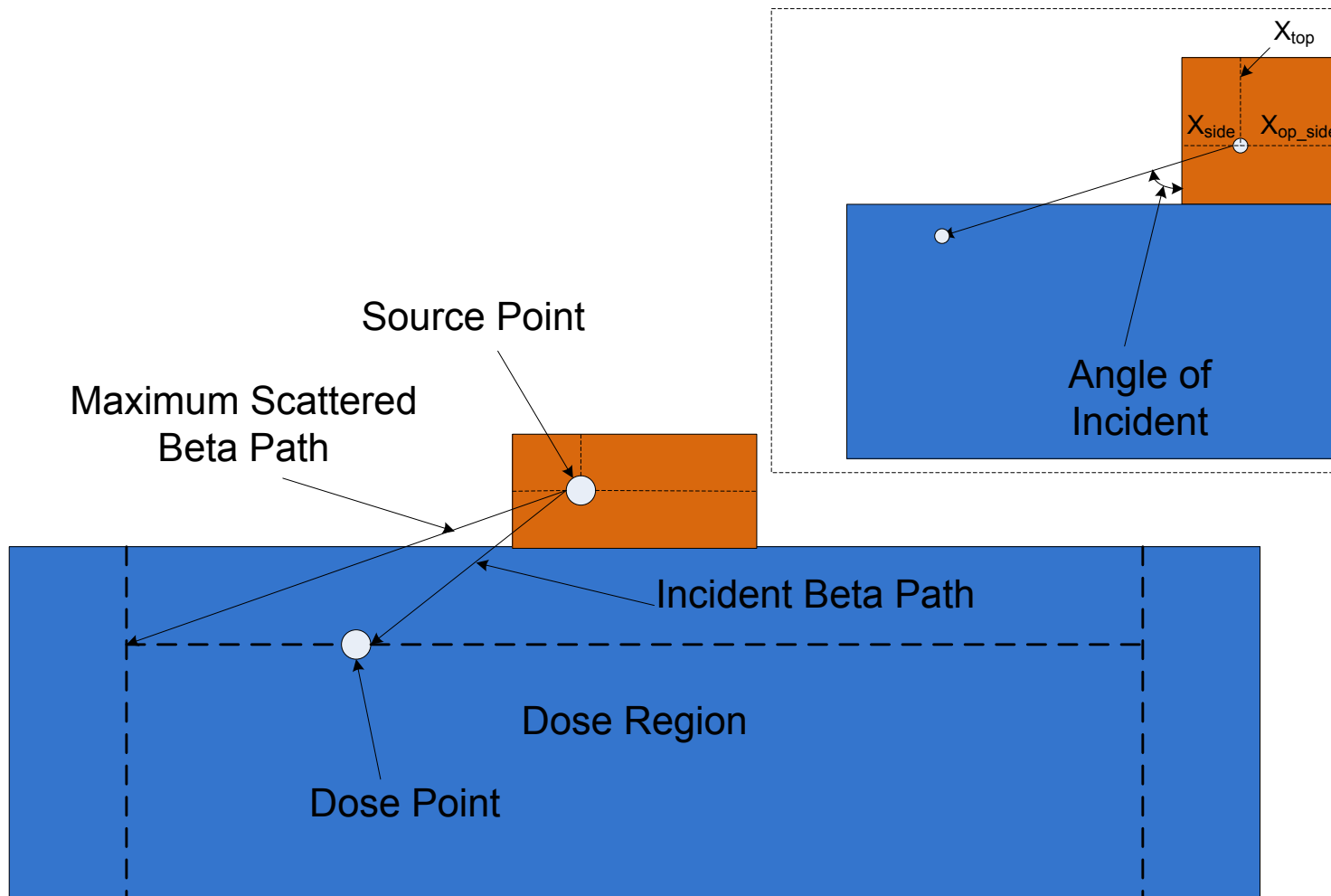
Air Scatter for Top/Sides of Source



Air Scatter for Top/Sides of Source



Scatter for Sides of Source



Selective Integration

- Source Scatter for Top/Bottom of Source

$$\text{Source } BSCF_{top/bottom} = SW (SE_{top} - SE_{bottom})$$

- Source Scatter for Sides of Source

$$\text{Source } BSCF_{side} = SA \frac{X_{top}}{0.5} (X_{op_side} - X_{side})$$

SW = source/water scatter correction for point sources

SE = scattering effectiveness (i.e., finite backscatter factor)

SA = source/air scatter correction for point sources

AW = air/water scatter correction for point sources

X = distance dimension

Selective Integration

- Air Scatter for Top/Sides of Source

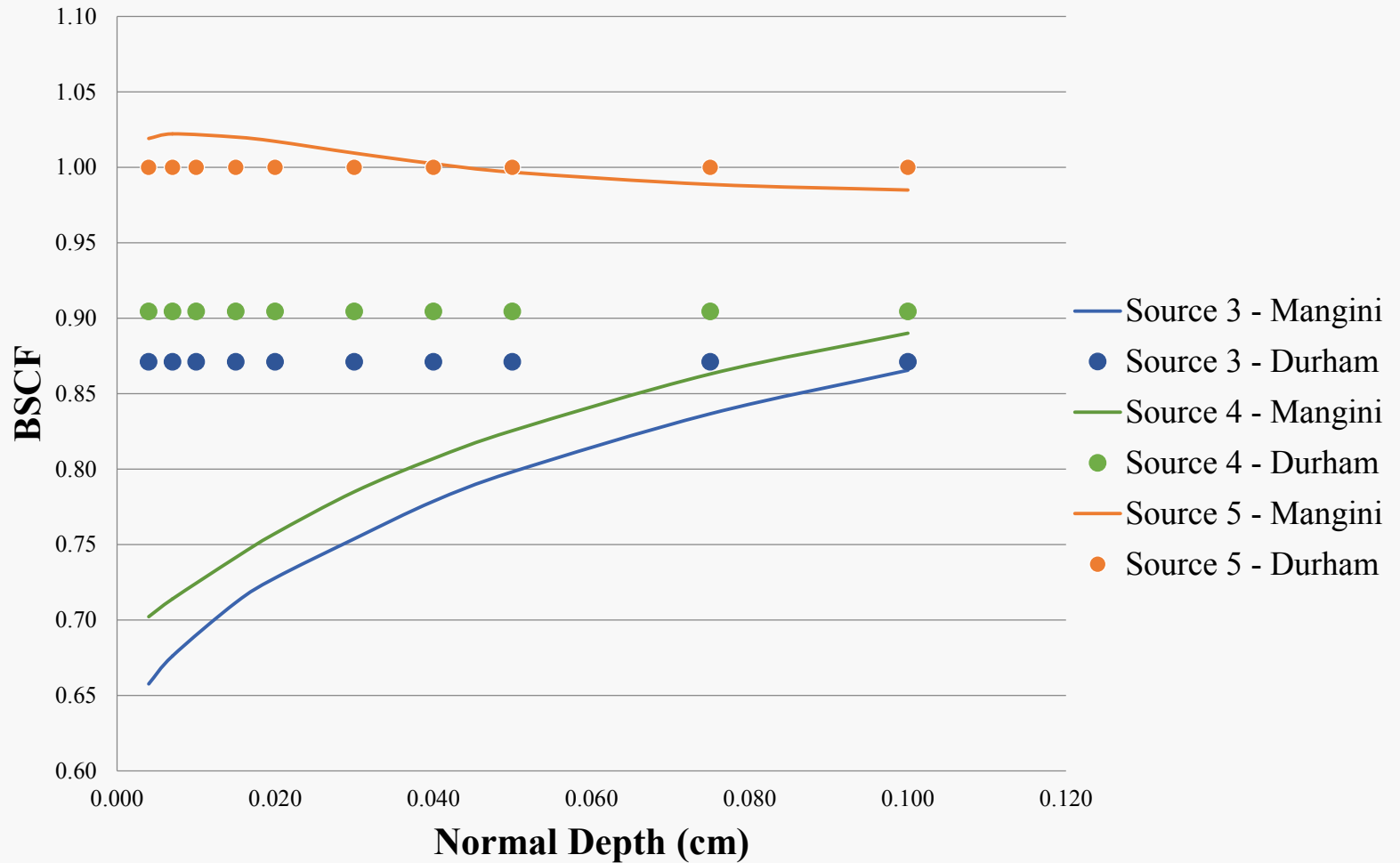
$$Air\ BSCF_{top} = AW \frac{1.8 - X_{top}}{1.8} 0.5$$

$$Air\ BSCF_{side} = AW \frac{1.8 - X_{side}}{1.8} 0.25$$

$$Air\ BSCF_{op_side} = AW \frac{1.8 - X_{op_side}}{1.8} 0.25$$

Volumetric BSCF

BSCF's for Uranium Oxide Slabs: ^{32}P β -



One other important improvement...

Electron Energy Distribution

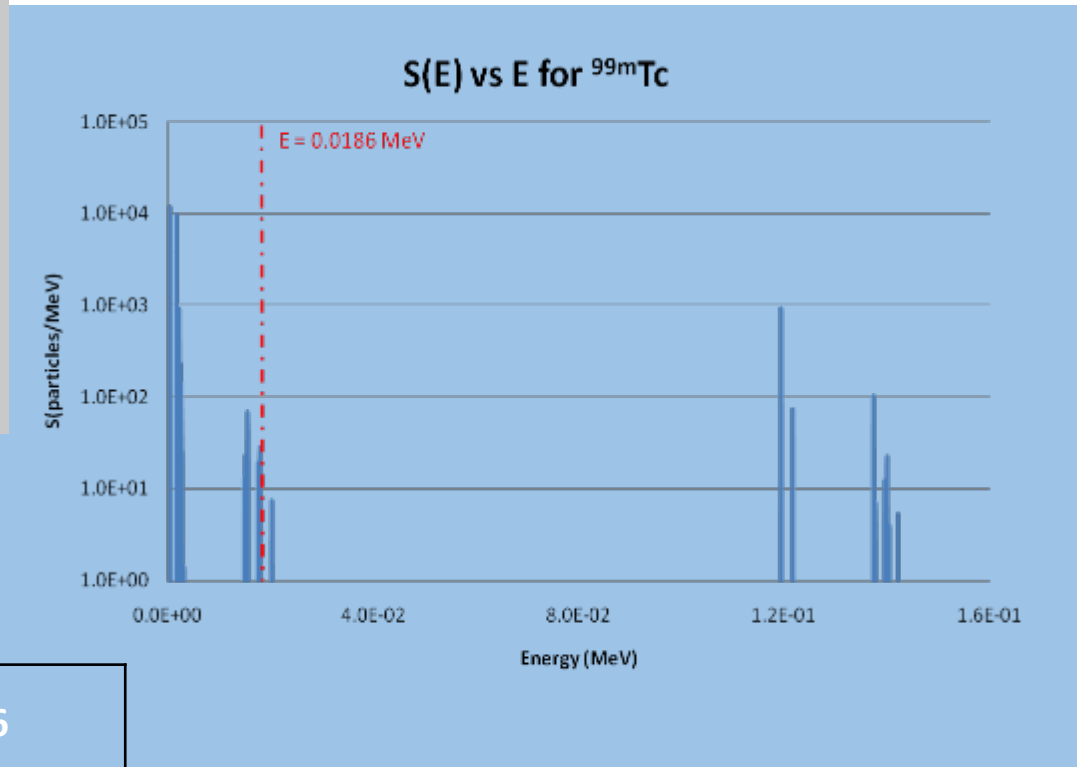
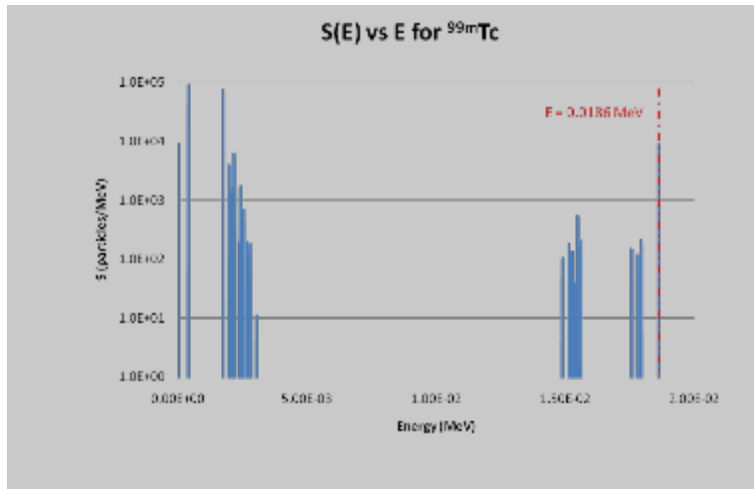
- Nuclides were first processed in SADCALC.f
 - calculation of the SADD when adding a radionuclide to the User library
 - electron emission data imported from ICRP38.BET
- For beta emitters:
 - an energy distribution, $S(E)$, was developed by interpolating 1500 points from 0.0 to E_{max}
 - average energy of $S(E)$ calculated
 - conversion/Auger electrons added to $S(E)$
 - but, if $S(E)_e > S(E_{max})$ then $S(E)_e$ was added to $S(E_{max})$
- For non-beta emitters:
 - electron yields were added to a “dummy” ^3H spectrum with a yield of 0.1%, with $E_{max} = 0.0186 \text{ MeV}$
- This resulted in errors depending on max electron energy

Electron Energy Distribution

- The new SADCALC routine constructs $S(E)$ from the original beta emission spectrum
- ... and, includes conversion electrons and Auger electrons at their proper energy
- Results in a more appropriate average electron energy incident on the skin

ELECTRON ENERGY – V3/4 vs V5/6

^{99m}Tc as the example



VARSKIN 3/4		VARSKIN 5/6	
X_{90} (mm)	E_{avg} (keV)	X_{90} (mm)	E_{avg} (keV)
0.0055	1.99	0.15	6.67

VARSKIN 5/6 Electron Model

- Integrated dose point-kernel over source and dose volumes
- Improved handling of electron energy distribution
- Modified energy loss (SADD) functions, (F_β)
 - relative to the X_{90} range
- New backscatter characteristics (BSCF)

$$\dot{D}_\beta \left[\frac{Gy}{sec} \right] = \frac{A \left[\frac{dis}{sec} \right] \cdot Y \bar{E} \left[\frac{J}{dis} \right] \cdot F_\beta}{4\pi\rho \left[\frac{kg}{cm^3} \right] \cdot x^2 [cm^2] \cdot X_{90} [cm] \cdot BSCF}$$

Comparison with literature

- “Beta and Electron Dose Calculations to Skin Due to Contamination by Common Nuclear Medicine Radionuclides.”
 - McGuire and Dalrymple, *Health Physics*, 1990
- “Electron dose-rate conversion factors for external exposure of the skin from uniformly deposited activity on the body surface.”
 - Kocher, D. C.; Eckerman, K. F., *Health Physics*, 1987
- ^{99m}Tc , ^{51}Cr , ^{57}Co , ^{67}Ga , ^{111}In , ^{123}I , ^{131}I , and ^{201}Tl
- $1 \mu\text{Ci cm}^{-2}$ source uniform contamination, averaged over a 1 cm^2
- 0.004 cm to 0.010 cm skin depths

Depth dose comparisons

Depth in Tissue, cm												
	0.004				0.005				0.007			
Nuclide	V5/6	V4	M	K	V5/6	V4	M	K	V5/6	V4	M	K
Co-57(EC)					0.32	0.00	0.36	0.32	0.27	0.00	0.29	0.29
Ga-67(EC)	2.97	0.00	3.34	3.21					1.14	0.00	1.19	1.09
Tc-99m(γ)	0.99	0.00	1.25	1.22	0.92	0.00	1.12	1.14	0.78	0.00	0.90	0.89
In-111(EC)									1.10	0.00	1.36	1.39
I-123(EC)									1.13	0.00	1.33	1.35
I-131(β)									4.87	5.10	6.30	6.33
Tl-201(EC)	2.01	0.00	2.20	2.24					0.90	0.00	1.27	0.97

Note: Dose rates in rad/hr. (M) McGuire and Dalrymple, and (K) Kocher.

McGuire; Dalrymple. Beta and electron dose calculations to skin due to contamination by common nuclear medicine radionuclides. Health Phys. 1990.

Kocher, D. C.; Eckerman, K. F. Electron dose-rate conversion factors for external exposure of the skin from uniformly deposited activity on the body surface. Health Phys. 53:135-141: 1987

... continued

	0.008				0.01			
Nuclide	V5/6	V4	M	K	V5/6	V4	M	K
Co-57					0.18	0.00	0.19	0.17
Ga-67	0.62	0.00	0.53	0.59				
Tc-99m	0.70	0.00	0.79	0.76	0.54	0.00	0.58	0.63
In-111								
I-123								
I-131								
Tl-201	0.62	0.00	0.97	0.68				

Note: Dose rates in rad/hr. (M) McGuire and Dalrymple, and (K) Kocher.

McGuire; Dalrymple. Beta and electron dose calculations to skin due to contamination by common nuclear medicine radionuclides. Health Phys. 1990.

Kocher, D. C.; Eckerman, K. F. Electron dose-rate conversion factors for external exposure of the skin from uniformly deposited activity on the body surface. Health Phys. 53:135-141: 1987

Water Sphere

Averaging area: 1 cm ²		Nuclide: Co-60 0.05 cm water sphere	
Depth (μm)	MCNP5 Dose Rate (mGy/hr/MBq)	VARSKIN 5/6 Dose Rate (mGy/hr/MBq)	VARSKIN 4 Dose Rate (mGy/hr/MBq)
30	396	385	375
50	297	281	271
70	238	216	205
100	167	153	142
120	133	122	112
150	96.9	85.1	75.2
200	58.0	46.6	39.1
300	18.1	14.0	9.97
500	1.67	0.961	0.168
1000	0	0	0

Iron Sphere

Averaging area: 1 cm ²		Nuclide: Co-60 0.05 cm iron sphere	
Depth (μm)	MCNP5 Dose Rate (mGy/hr/MBq)	VARSKIN 5/6 Dose Rate (mGy/hr/MBq)	VARSKIN 4 Dose Rate (mGy/hr/MBq)
30	59.2	58.7	48.7
50	46.9	42.9	35.0
70	38.7	32.9	26.6
100	26.7	23.2	18.4
120	21.8	18.6	14.5
150	15.9	12.9	9.70
200	9.77	7.04	5.04
300	3.12	2.10	1.28
500	0.479	0.144	0.0213
1000	0	0.000008	0

SUMMARY

- Electron energy distribution
- Energy scaling model
- Range scaling model
- Backscatter correction factors
- Comparisons brought closer in line with literature

Varskin 6.0

File Help

Source Geometry

☐ Point

☐ Sphere

☐ Disk

☐ Slab

☐ Cylinder

Special Options

☐ Exclude Photon Dose

☐ Exclude Electron Dose

☐ Perform Volume Averaging

☐ Offset Particle Model

Skin Averaging Area

10

cm²

Exposure Time

60

min

Radionuclide Library [Zeff]

C-14 [7.42] 38

Ce-144 [7.42] 107

Ce-144 [7.42] 107D

Ce-144 [7.42] 38

Ce-144 [7.42] 38D

Co-60 [25.5] 38

Cs-137 [7.42] 107D

Pr-144 [7.42] 107

Pr-144 [7.42] 38

Pr-144m [7.42] 38

Re-186 [7.42] 38

Activity Units

μCi

Select

Add

Remove

Selected Radionuclides

Cs-137 [7.42] 107D: 1.00E+00 μCi

Edit

Remove

Remove All

Point Source Irradiation Geometry

Skin Thickness or Skin Density Thickness:

7

mg/cm²

Air Gap Thickness

0

mm

Cover Thickness

0

mm

Cover Density

0

g/cm³

Multiple Cover Calculator

VARSKIN

Calculate Doses

VARSKIN Output

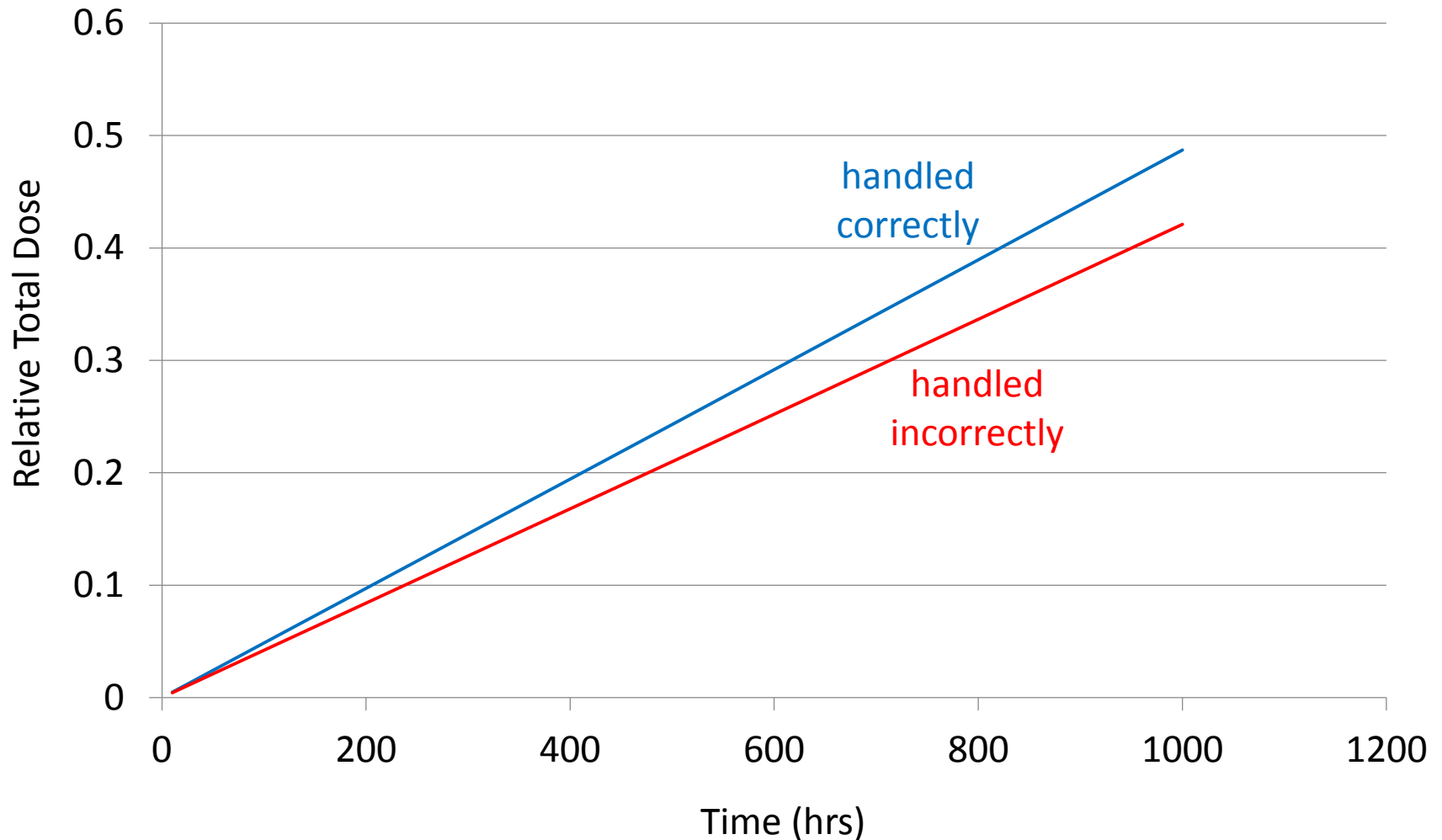
- English or SI units
- For each radionuclide (and total), the following doses are provided:
 - Beta, Photon & Total:
 - initial dose rate
 - dose (no decay)
 - decay-corrected dose
- Date/time
- Geometry summary
- Print option (to html file)

$$D = \dot{D}(0) \cdot t$$

$$D_{dc} = \int_0^t \dot{D}(t) dt = \dot{D}(0) \int_0^t e^{-\lambda t} dt$$

Decay-Corrected Dose

^{137}Cs and $^{137\text{m}}\text{Ba}$; point source; 10 cm^2 ; 7 mg/cm^2



Radionuclide: Activity

Cs-137 [7.42] 107D: 1.00E+00 µCi

All Radionuclides

Unit Selection

- ☐ English Units
- ☒ SI Units



	Initial Dose Rate	Dose (No Decay)	Decay-Corrected Dose
Electron	2.55E-03 rad/h	2.55E-03 rad	2.55E-03 rad
Photon	4.99E-03 rad/h	4.99E-03 rad	4.99E-03 rad
Total	7.54E-03 rad/h	7.54E-03 rad	7.54E-03 rad



	Initial Dose Rate	Dose (No Decay)	Decay-Corrected Dose
Electron	2.55E-03 rad/h	2.55E-03 rad	2.55E-03 rad
Photon	4.99E-03 rad/h	4.99E-03 rad	4.99E-03 rad
Total	7.54E-03 rad/h	7.54E-03 rad	7.54E-03 rad

Date/Time 3/19/18 11:29:50 AM

Source Geometry Disk Source

Source Diameter 1.00E+00 mm

Source Area 7.85E-01 mm²

Cover Thickness 5.20E-02 cm

Cover Density 3.90E+00 g/cm³

Air Gap Thickness 0.00E+00 mm

Irradiation Time 6.00E+01 min

Irradiation Area 1.00E+01 cm²

Print Results

Close